# Cortical Connectivity Changes Under Difficult Listening Conditions Revealed by Network Localized Granger Causality \*behrad@umd.edu



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#### Introduction

- Cortical connectivity may change under difficult listening conditions
- Connectivity characterized by the temporal predictability of activity across brain regions via Granger causality (GC)
- Challenges with M/EEG: the data are low-dimensional, noisy, and linearly-mixed versions of the true source activity
- · Conventional methods:



- Drawbacks: bias propagation, spatial leakage
- Goal: *directly* localize GC influences without an intermediate source localization step
- Method: Network Localized Granger Causality (NLGC)
- · Source dynamics as latent multivariate autoregressive model







#### Model

- **MEG observation model**   $\mathbf{y}_t = \mathbf{C}\mathbf{x}_t + \mathbf{n}_t, \quad t = 1, 2, \cdots, T$   $\mathbf{y}_t \in \mathbb{R}^M$  MEG sensor data,  $\mathbf{C} \in \mathbb{R}^{M \times N}$  Lead field matrix,  $\mathbf{x}_t \in \mathbb{R}^N$  Source activity,  $\mathbf{n}_t \in \mathbb{R}^M$  Measurement noise.
- Source dynamics model  $\mathbf{x}_t = \sum_{k=1}^{q} \mathbf{A}_k \mathbf{x}_{t-k} + \mathbf{w}_t, \quad t = 1, 2, \cdots, T$   $\mathbf{A}_k \in \mathbb{R}^{N \times N} \quad \begin{array}{c} \text{Coefficient matrix,} \\ \mathbf{w}_t \in \mathbb{R}^N & \text{Noise process.} \end{array}$

#### **Granger** Causality



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#### Parameter Estimation

· Objective: to estimate dynamic source model parameters

 $\boldsymbol{\theta} = (\mathbf{A}_k, k = 1, \cdots, q; \operatorname{diag}(\mathbf{Q}))$ 

- Challenge: source activities are unknown
- Solution: Expectation Maximization (EM)
- At the *l*-th iteration:



• Perform the EM parameter estimation for full/reduced model corresponding to every source pair

### Statistical Inference

• Test statistic, the *debiased deviance* for link  $(\tilde{i} \rightarrow i)$  [3]

 $\mathcal{D}_{(\tilde{i}\mapsto i)} = 2\big(\ell_i(\widehat{\boldsymbol{\theta}}_i^F) - \ell_i(\widehat{\boldsymbol{\theta}}_i^R)\big) - B(\widehat{\boldsymbol{\theta}}_i^F, \widehat{\boldsymbol{\theta}}_i^R)$ log-likelihood of the *i*-th source bias term full and reduced model parameters

Hypothesis test, distributional results [4]
Null: θ<sub>i</sub> = θ<sup>R</sup><sub>i</sub> (i.e., no GC influence); D<sub>(i→i</sub> → χ<sup>2</sup>(q)
Alternative: θ<sub>i</sub> = θ<sup>F</sup><sub>i</sub> (i.e., GC influence); D<sub>(i→i</sub> → χ<sup>2</sup>(q, ν<sub>(i→i)</sub>)

[1] Anderson, et al., "Optimal Filtering", 2012.

[4] Sheikhattar, et al., "Extracting neuronal functional network dynamics via adaptive Granger causality analysis", PNAS, 2018.

[5] Benjamini, et al., "The control of the false discovery rate in multiple testing under dependency", Ann. Stat., 2001.

- False discovery rate (FDR) control
- Reject null hypothesis at a confidence level and control FDR via BY procedure [5]
- Test strength characterization
- Calculate Youden's J-statistic for all links

$$J_{(\tilde{i}\to i)} = 1 - \alpha - F_{\chi^2(q,\hat{\nu}_{(\tilde{i}\to i)})}(F_{\chi^2(q)}^{-1}(1-\alpha))$$

- $\,J_{(\tilde{i} \rightarrow i)} \approx 1 \,\,(\approx 0)$  implies high (low) statistical confidence
- The GC map  $\Phi$ :  $[\Phi]_{i,\tilde{i}} = \begin{cases} J_{(\tilde{i} \to i)}, & i \neq \tilde{i} \\ 0, & \text{otherwise} \end{cases}$

#### Simulation Results

-100 sources, 50 sensors -FDR controlled at 2% -MNE procedure results in numerous spuriously detected links

Fig. 3. A. The GC network corresponding to sources {5, 6, ..., 10}. B. Ground truth GC map corresponding to 20 sources. C. Estimated GC map using the proposed method. D. Estimated GC map based on the two-stage procedure.





<sup>[2]</sup> Ba et al., "Convergence and stability of iteratively re-weighted least squares algorithms", IEEE TSP, 2013.

<sup>[3]</sup> Soleimani et al., "Granger Causal Inference from Indirect Low-Dimensional Measurements with Application to MEG Functional Connectivity Analysis", CISS, 2020.

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### **Difficult Listening Experiment**

• Task (see poster #71 [6]): 1-minute long speech segments from an audio book in two conditions:

-Clean: male/ female narration

-Mixed speech: two talker speech, male vs. female speaker

- · Mixed speech task: attend to pre-specified speaker
- · We analyzed the data from the first trials of these conditions

### **Model Specifications**

- Band-passed between 0.1 4.5 Hz (delta band)
- Head model: morph 'fsaverage' source space, Desican-Killiany atlas to identify 68 ROIs [6]
- Analyzed ROIs (in both hemispheres)

Temporal lobe 'superiortemporal', 'middletemporal', 'transversetemporal

#### Frontal lobe

 $'rostralmiddlefrontal', \, 'caudalmiddlefrontal', \, 'parsopercularis', \, 'parstriangularis'$ 

- We summarize the contribution of each ROI by the leading eigenvectors within the ROI
- The measurement noise covariance: empty room recordings
- 155 MEG sensors
- Model order q = 6 (to fully capture the delta band)
- Sampling frequency: 25 Hz

### Application to MEG Data

**Fig. 4.** NLGC estimates of neural connectivity for sites in the frontal and temporal lobes, during the last 40 s of each continuous speech listening trial, for either clean or masked speech (only significant links shown; arrows indicate direction of GC influence; N=4, FDR=1%).



While listening to clean speech, about half (48%) of the significant causal links are frontal→frontal and about a third (32%) are top- down frontal→temporal (out of 31 significant links).



 In contrast, while listening to masked speech, almost two thirds (65%) of the 17 significant causal links are now top-down frontal→temporal, and only 12% are frontal→frontal (out of 17 significant links).

[6] Poster #71: I.M. Dushyanthi Karunathilake, et al. "Effects of Aging on the Cortical Representation of Continuous Speech".

[7] Desikan, et al., "An Automated Labeling System for Subdividing the Human Cerebral Cortex on MRI Scans into Gyral based Regions of Interest", NeuroImage, 2006.