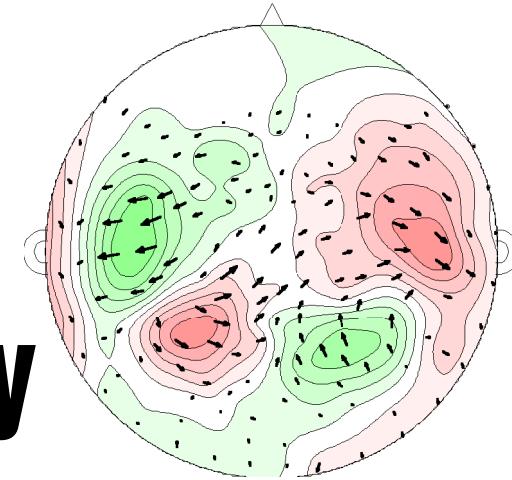


# Fully Complex Magnetoencephalography



Jonathan Z. Simon

*Biology / Electrical & Computer Engineering*

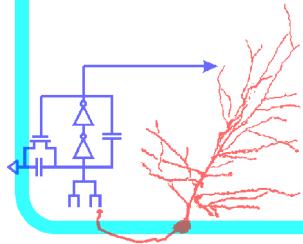
*Neuroscience and Cognitive Sciences*

*Bioengineering*

Yadong Wang

*Neuroscience and Cognitive Sciences*

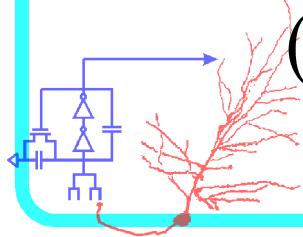
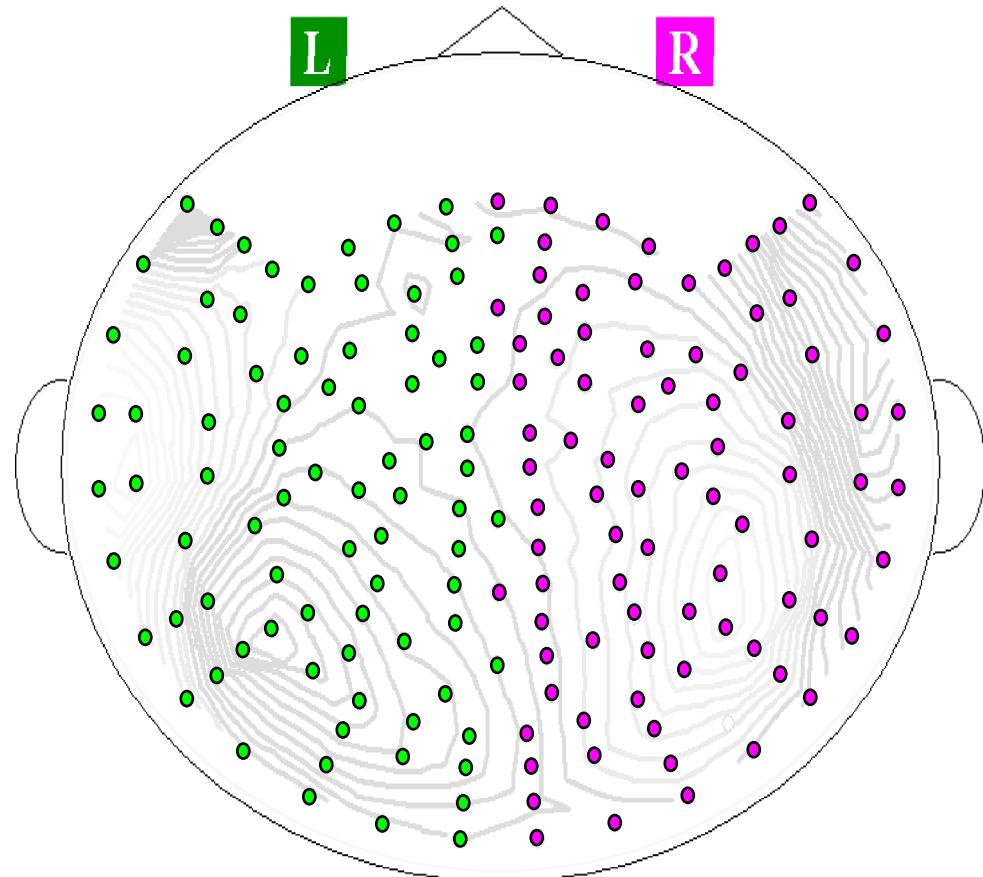
University of Maryland, College Park



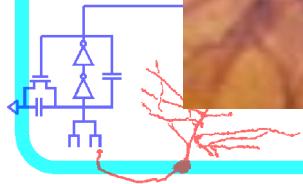
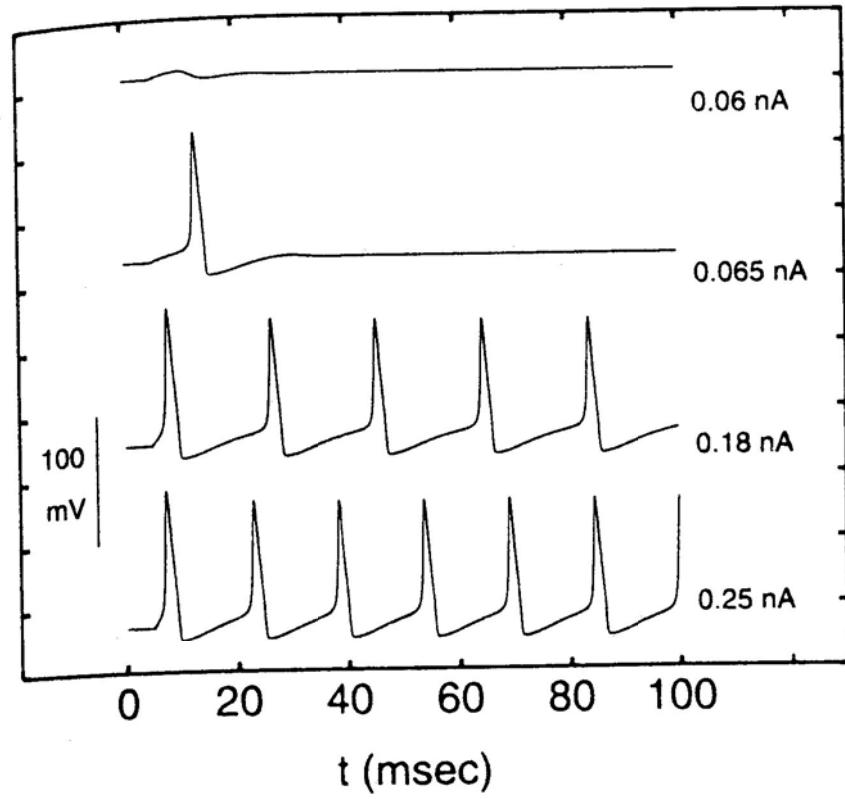
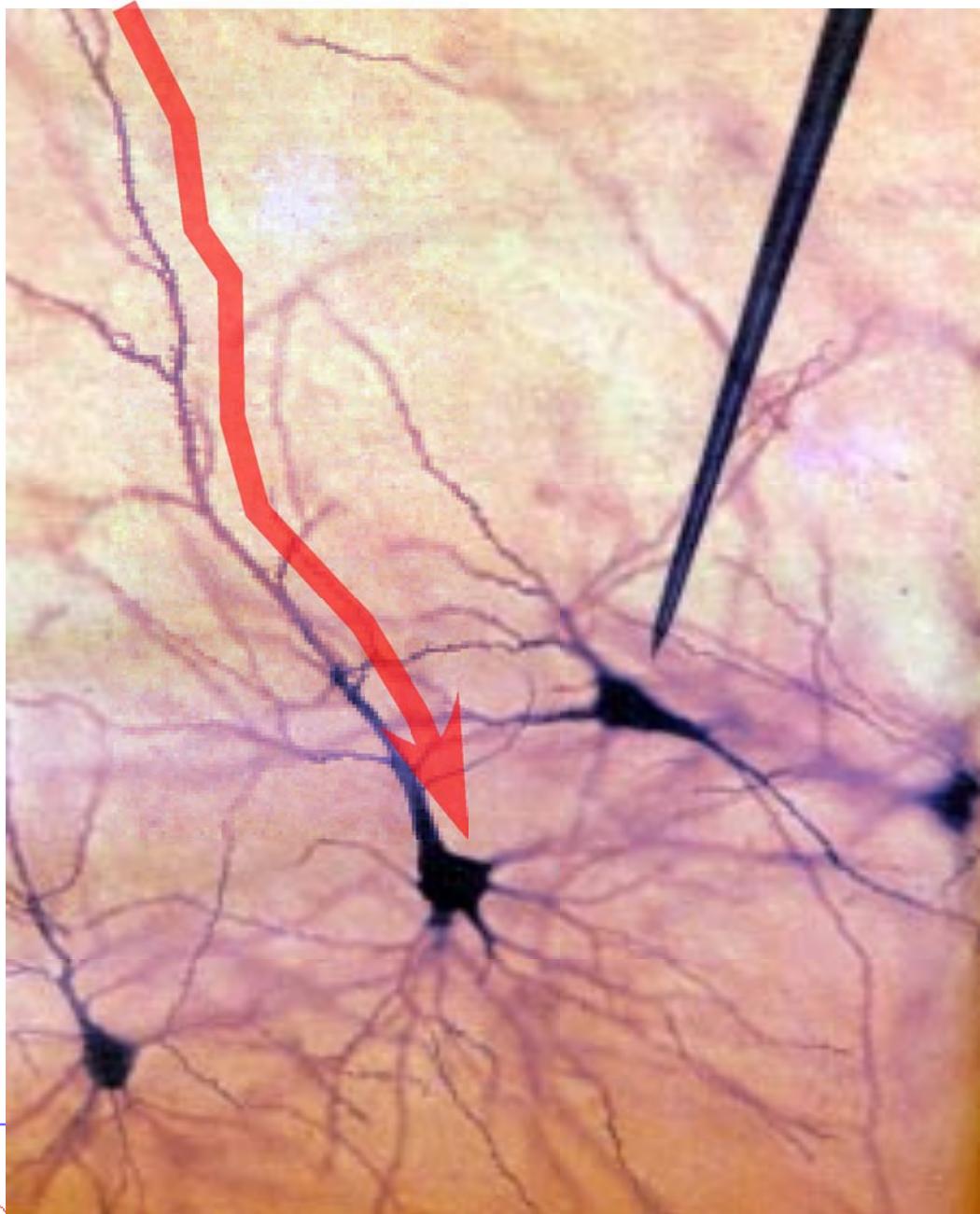
# MEG – Magnetoencephalography

- Non-invasive, Passive, Silent
- Simultaneous Whole Head recordings  
160 magnetic sensors (3 reference)
- Exquisitely Sensitive
  - ~ 100 fT ( $10^{-13}$  Tesla)
  - ~  $10^4$  neurons
- Temporal Resolution
  - ~ 1 ms

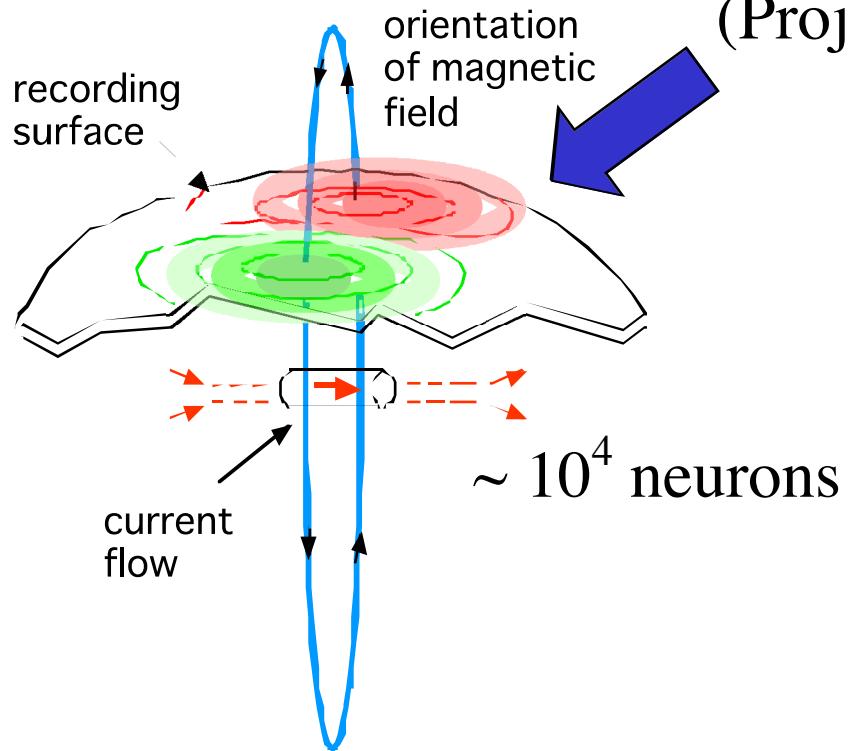
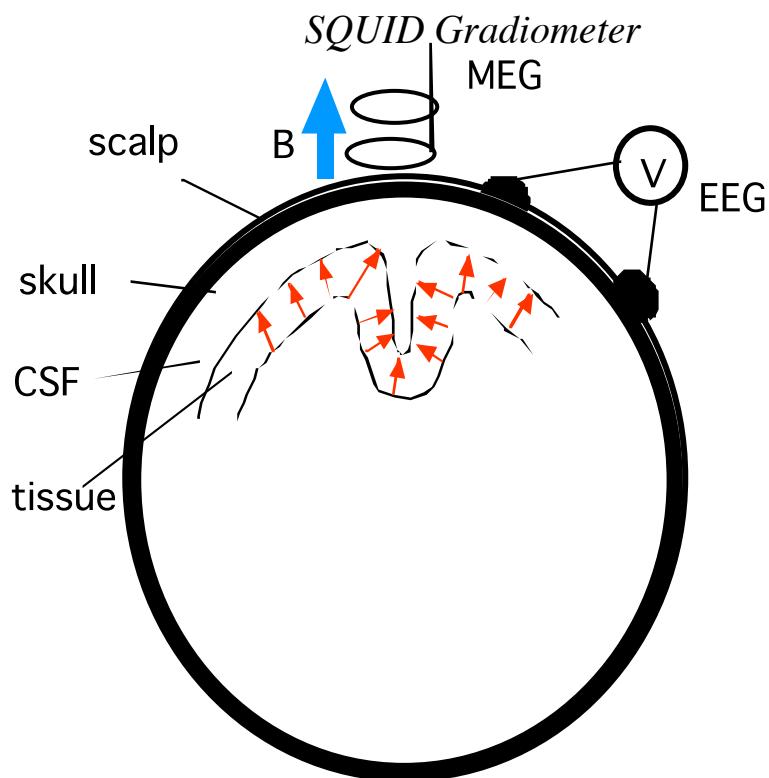
(c.f. fMRI: ~1 s)



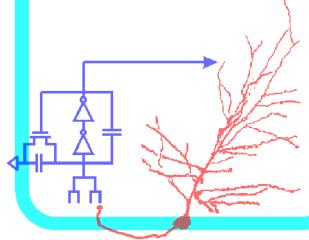
# Neural Activity = Neural Current



# MEG Magnetic Signal

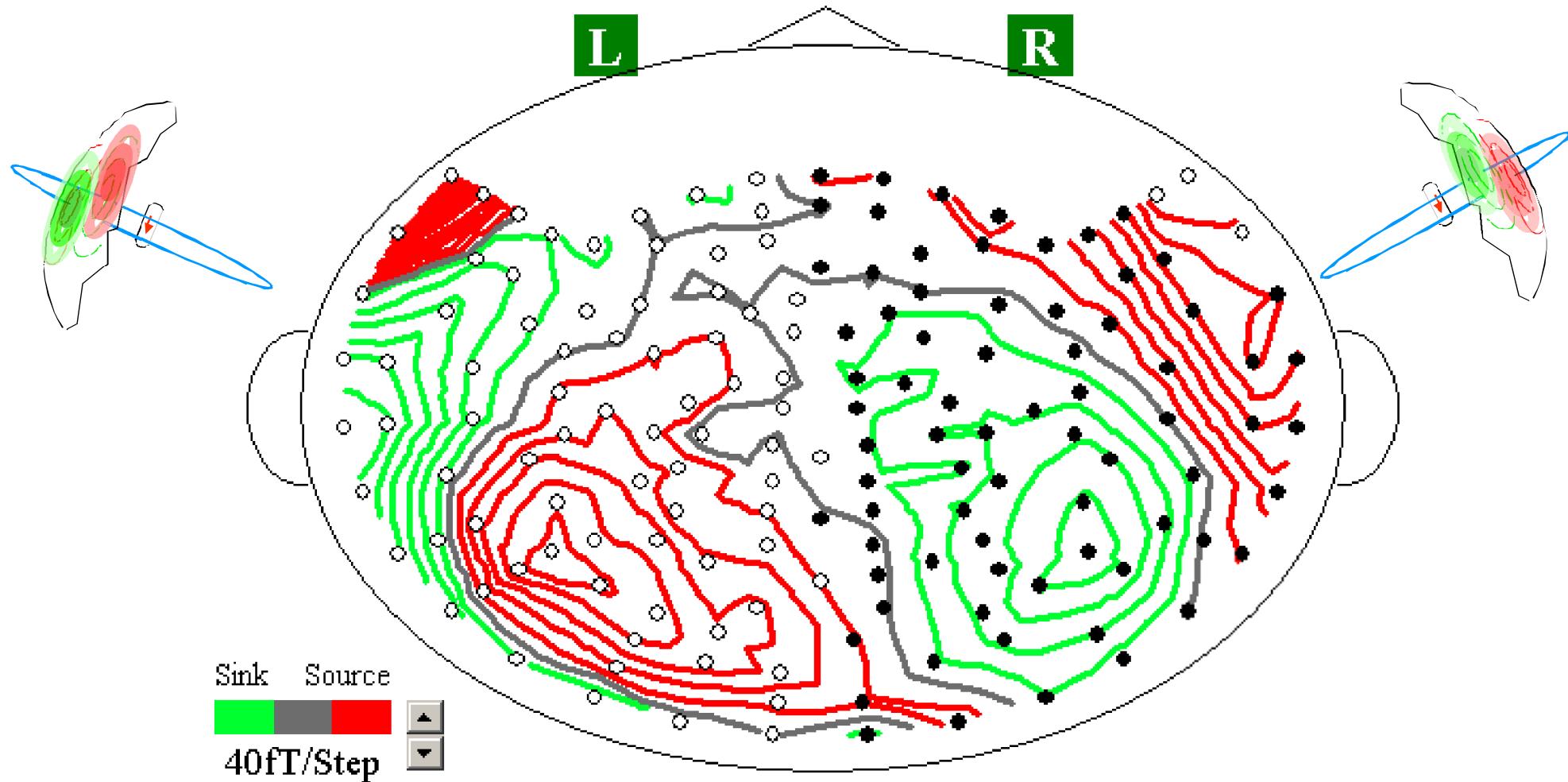


Non-invasive  
Direct electrophysiological  
measurement (not hemodynamic)



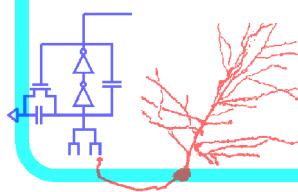
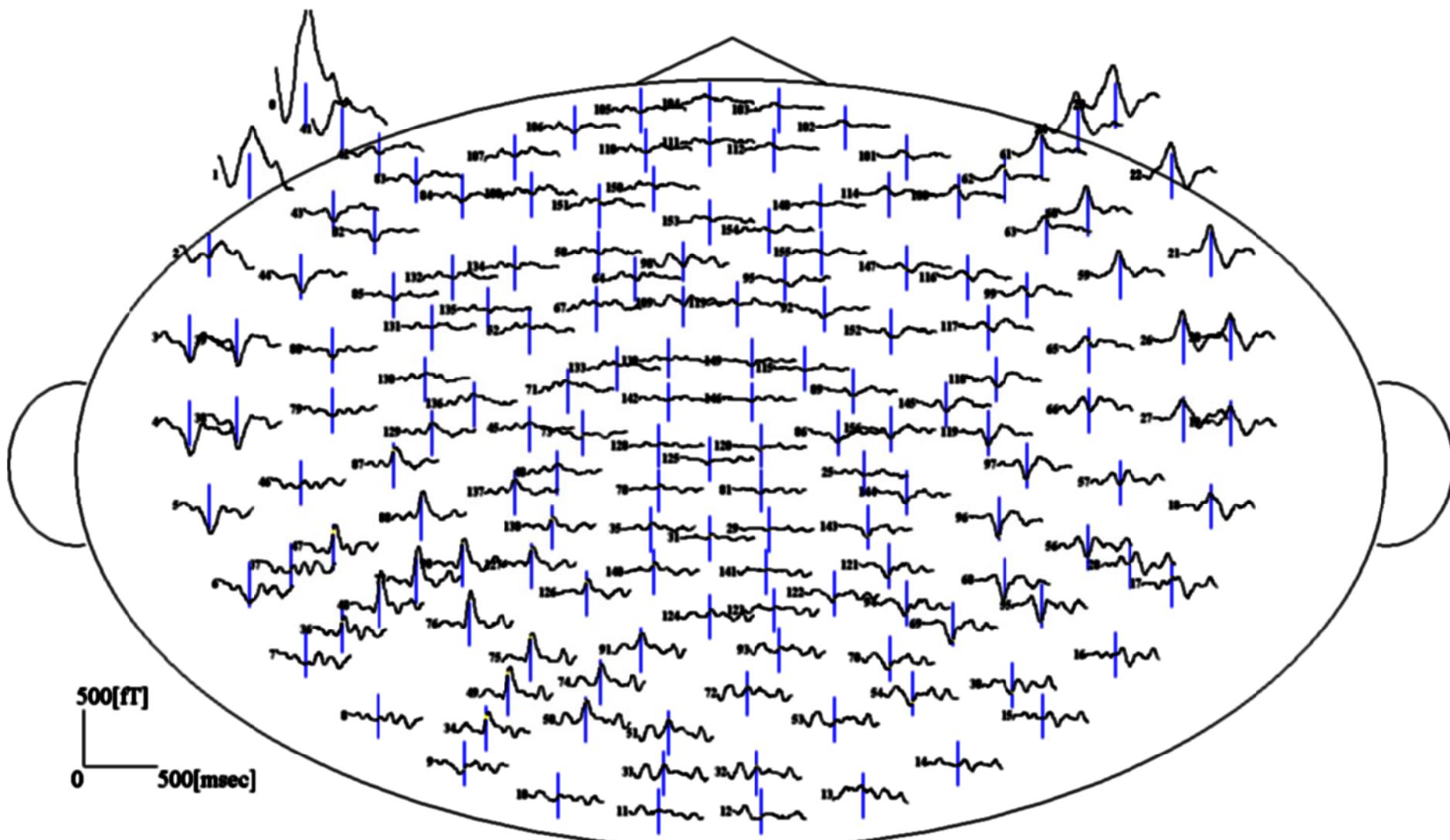
# MEG Response

Isofield Contour Map



Time = 98.00[msec]

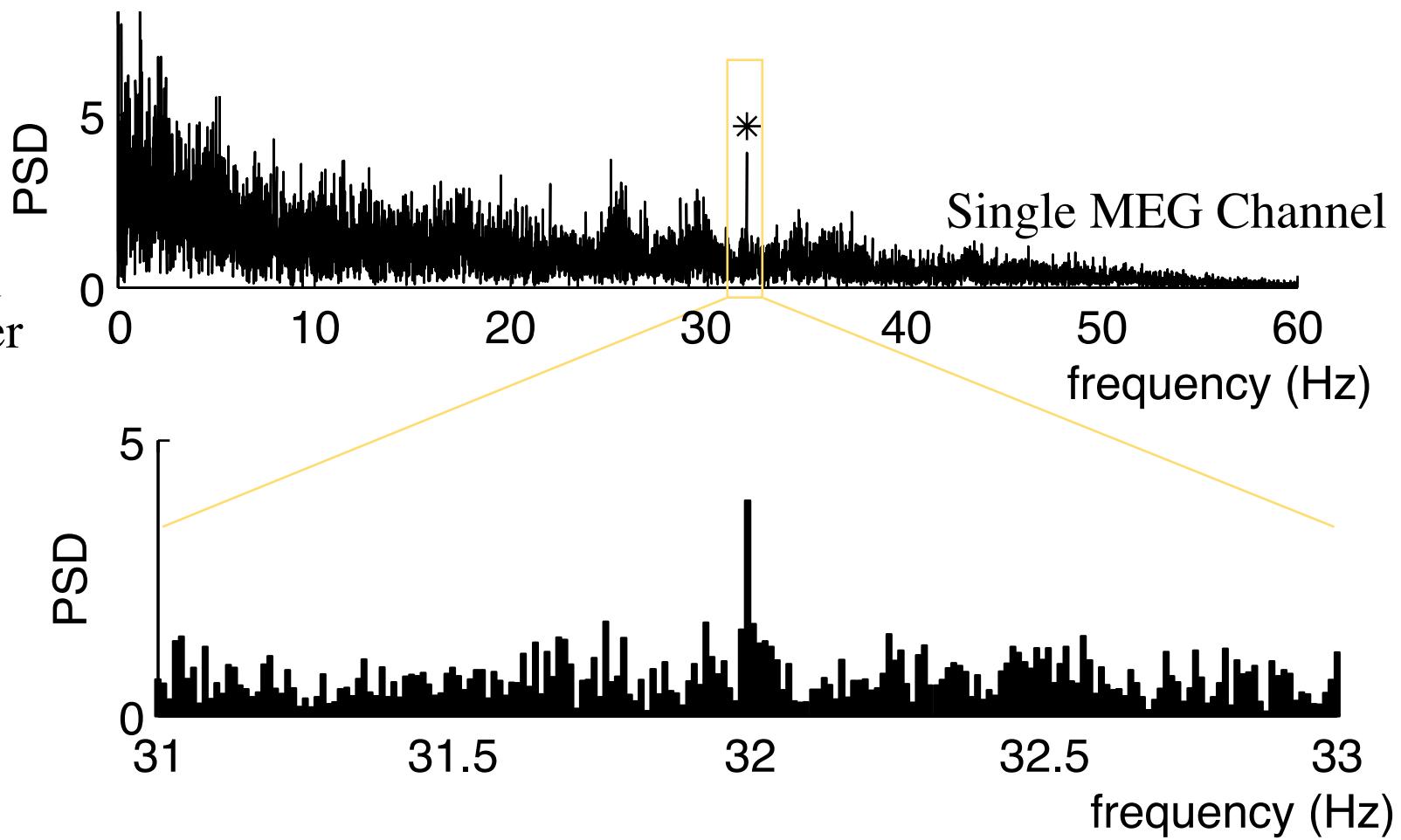
# MEG Response



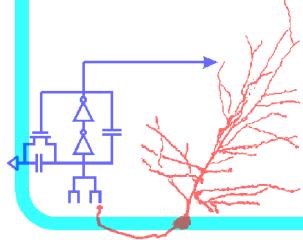
# Frequency Response

Stimulus Modulated at Single Frequency  $\rightarrow$  *Steady State Response* (SSR)

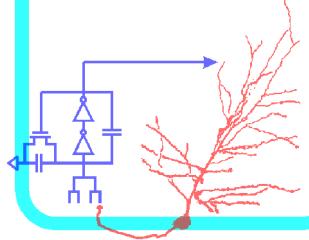
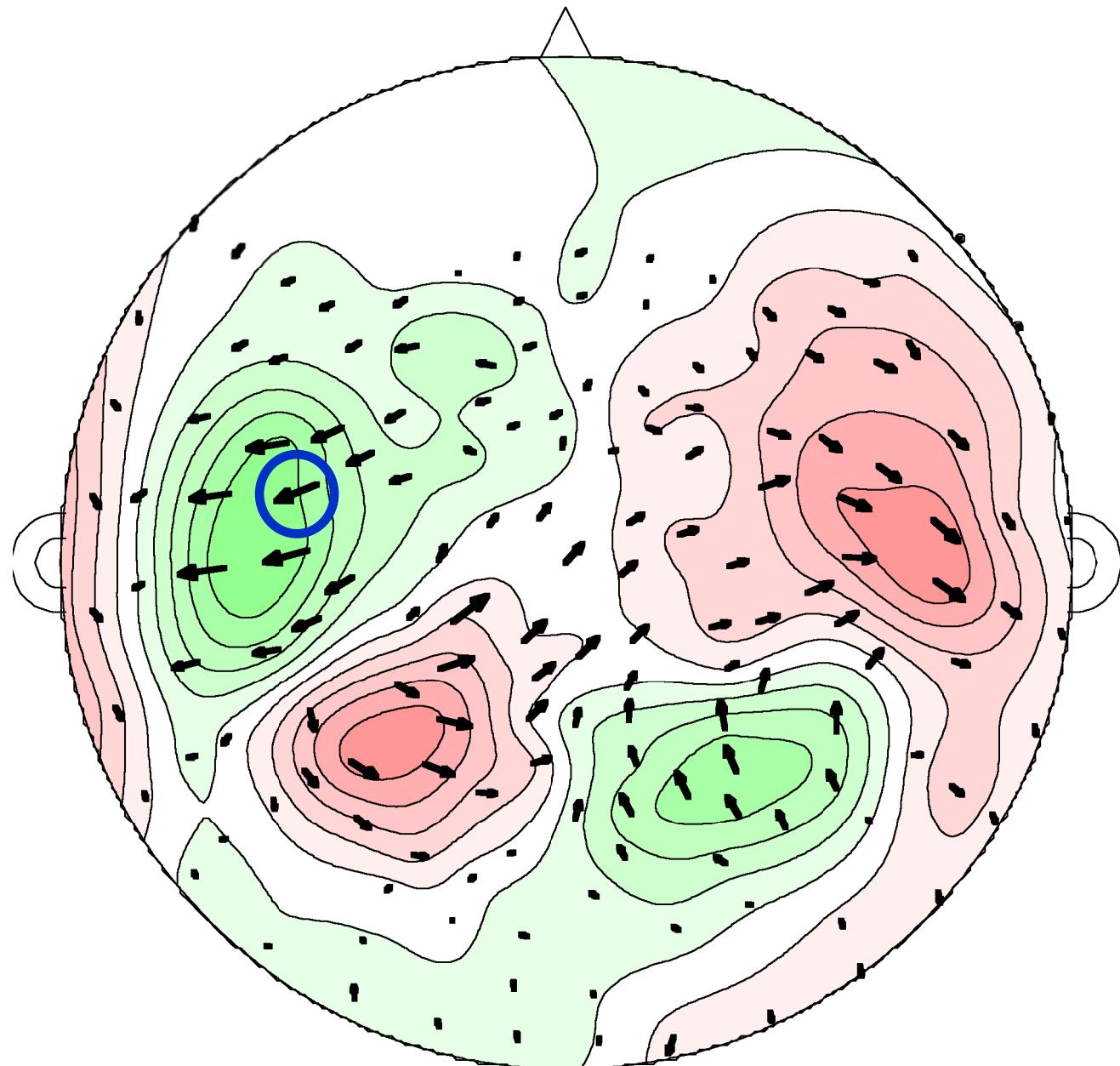
32 Hz Modulation  
400 Hz tone carrier  
100 trials @ 1 s  
(concatenated)



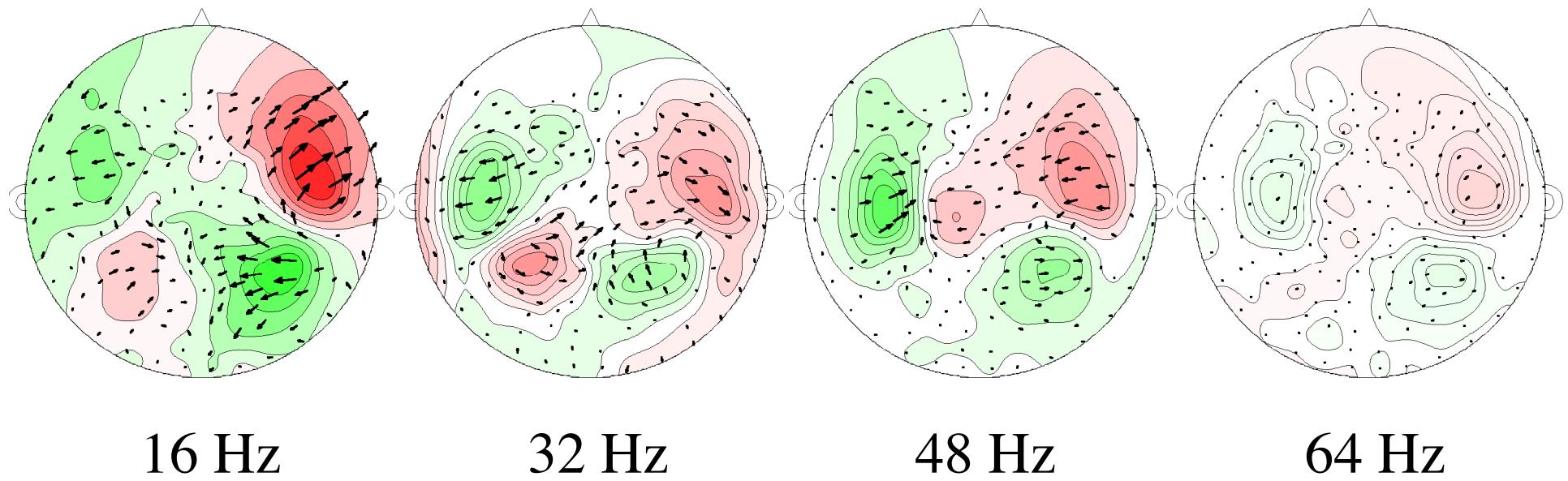
*Extremely Precise Phase-Locking: 0.01 Hz*  
No trial-to-trial jitter



# Whole Head Steady State Response



# Whole Head Transfer Function

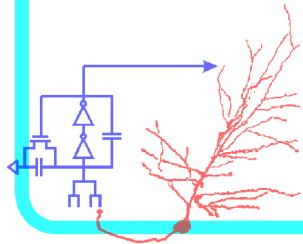


16 Hz

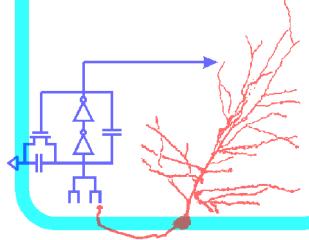
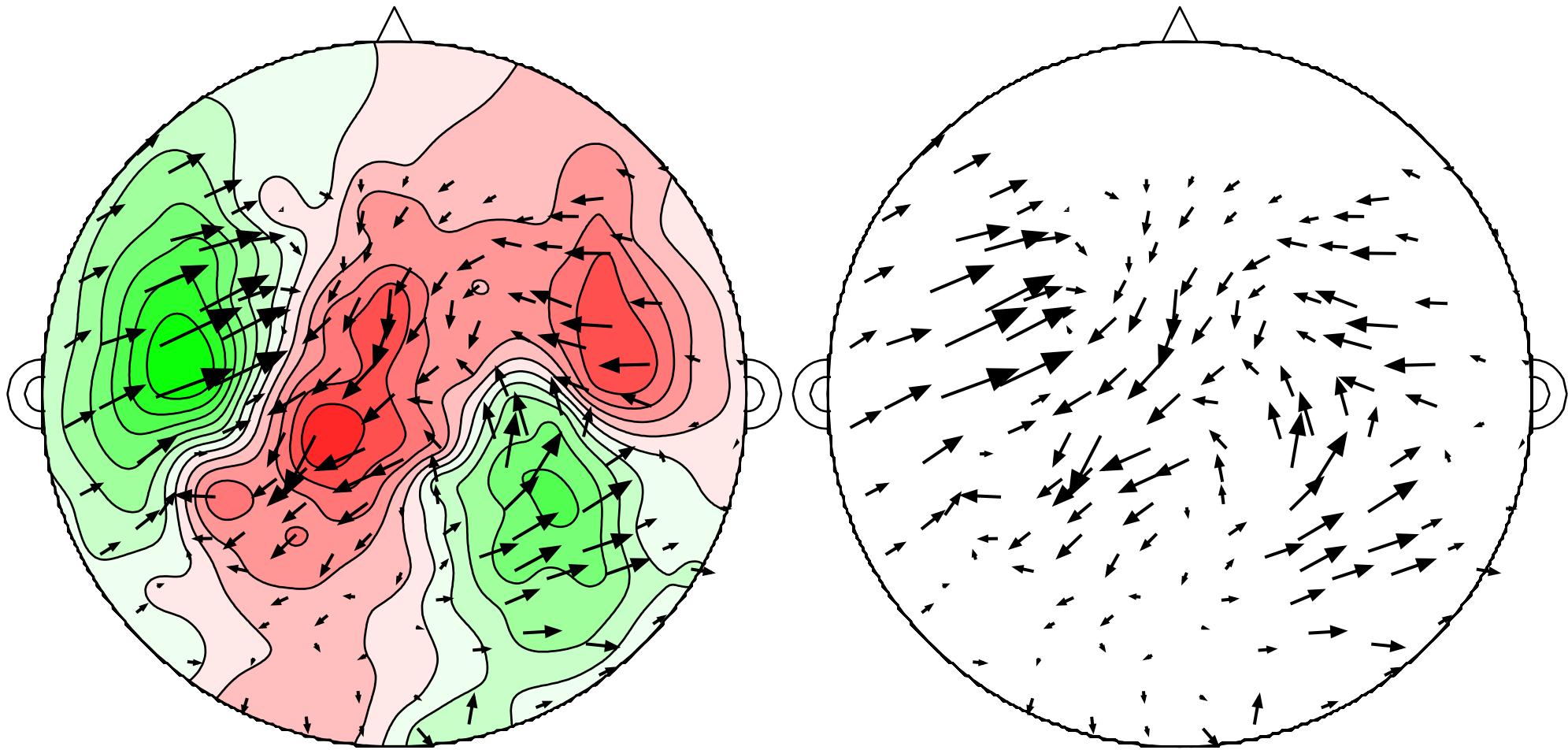
32 Hz

48 Hz

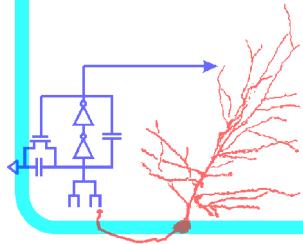
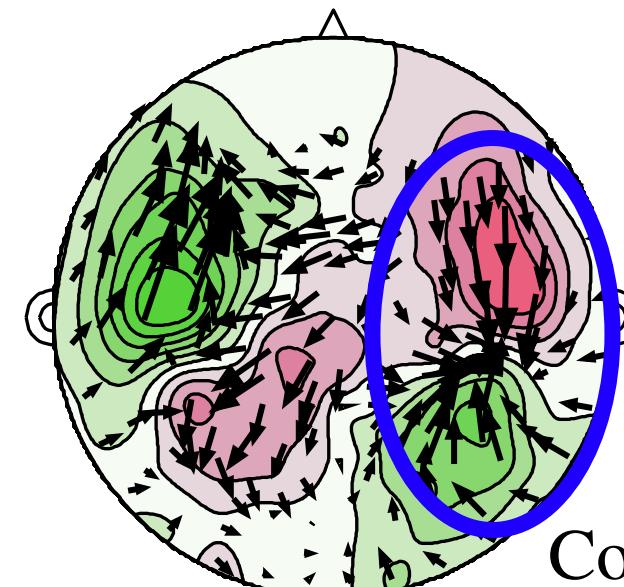
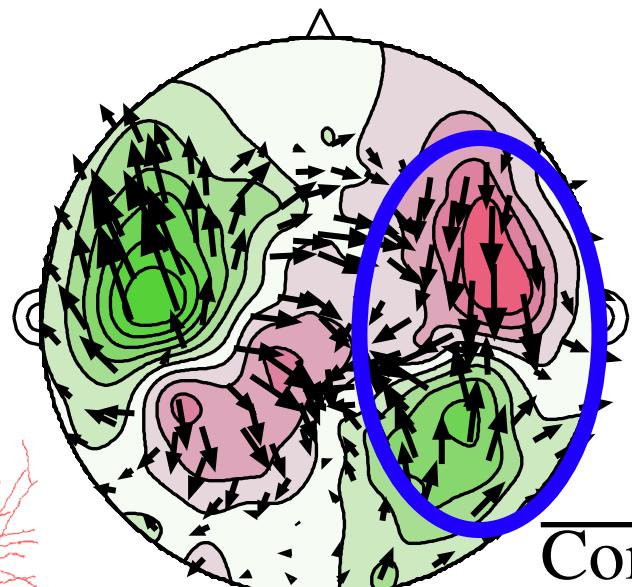
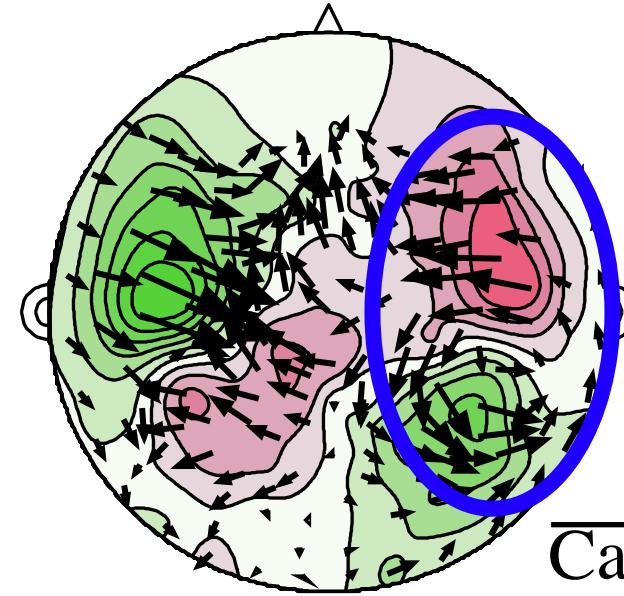
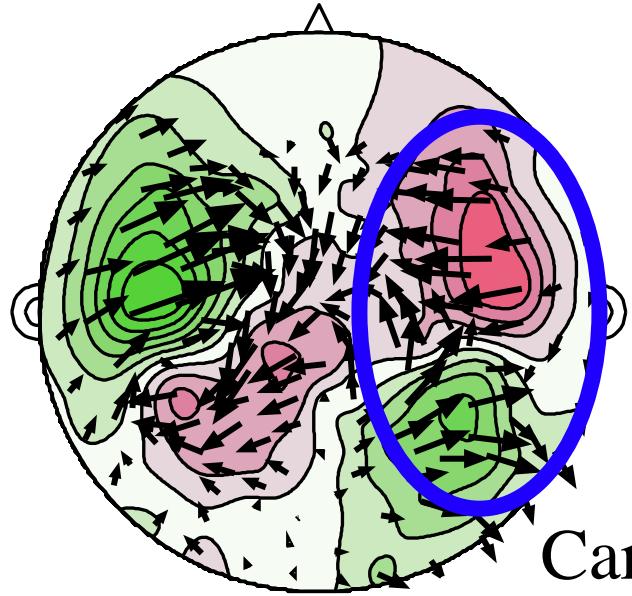
64 Hz



# Complex Magnetic Field

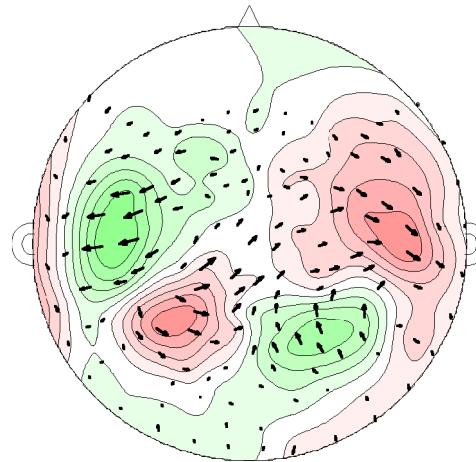


# Phase Conventions

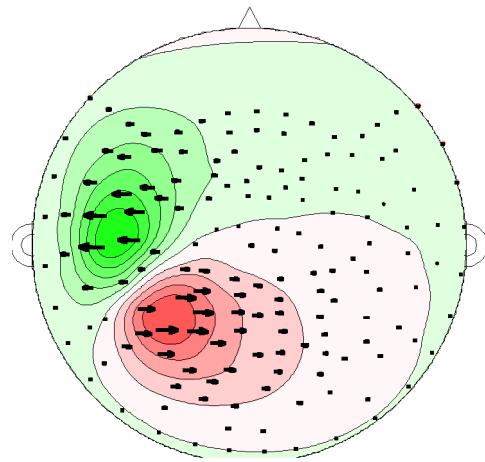


# Current-Equivalent Dipoles

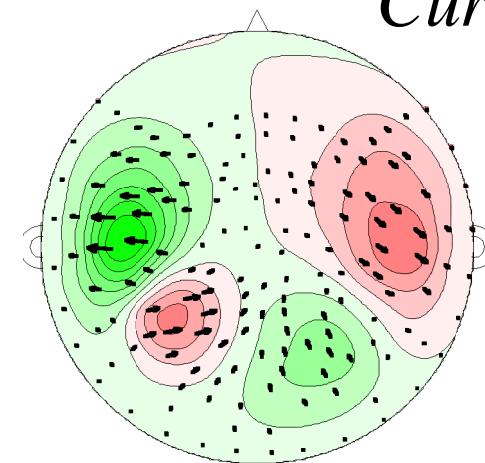
Raw Data



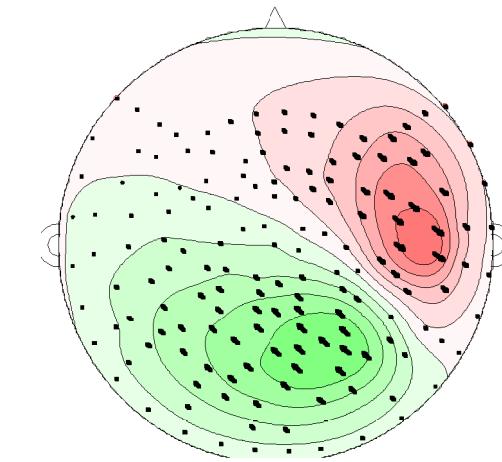
*Current Dipoles Complex Too!*



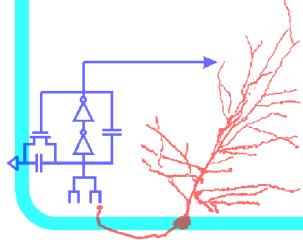
Two Dipole Fit



Left Dipole

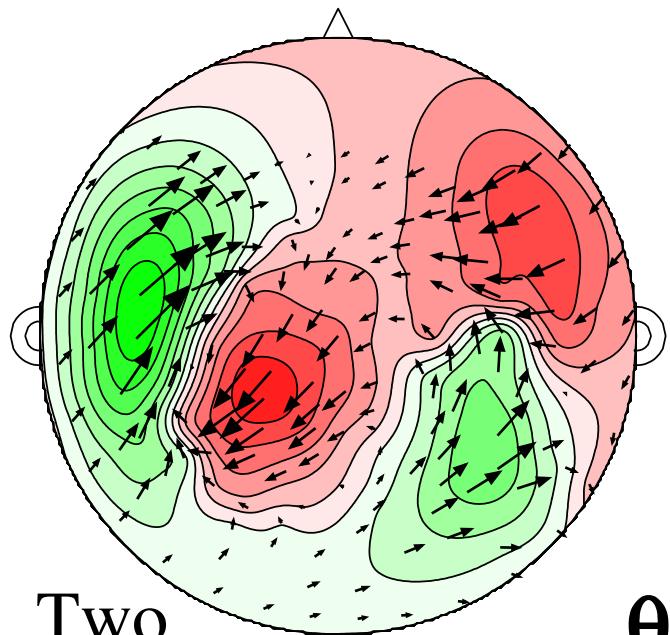


Right Dipole



32 Hz

# Complex Equivalent-Current Dipoles



Two  
Dipole  
Fit

$\theta_{\text{Max}}$   
“Phase”

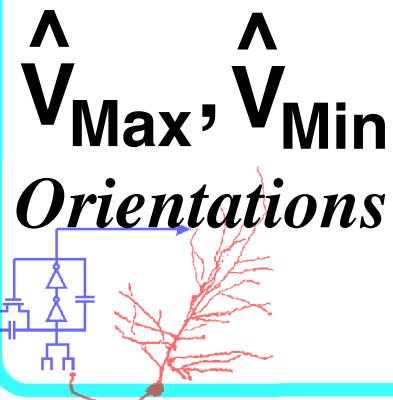
$V_{\text{Re}}$

$V_{\text{Max}}$   
“Strength”

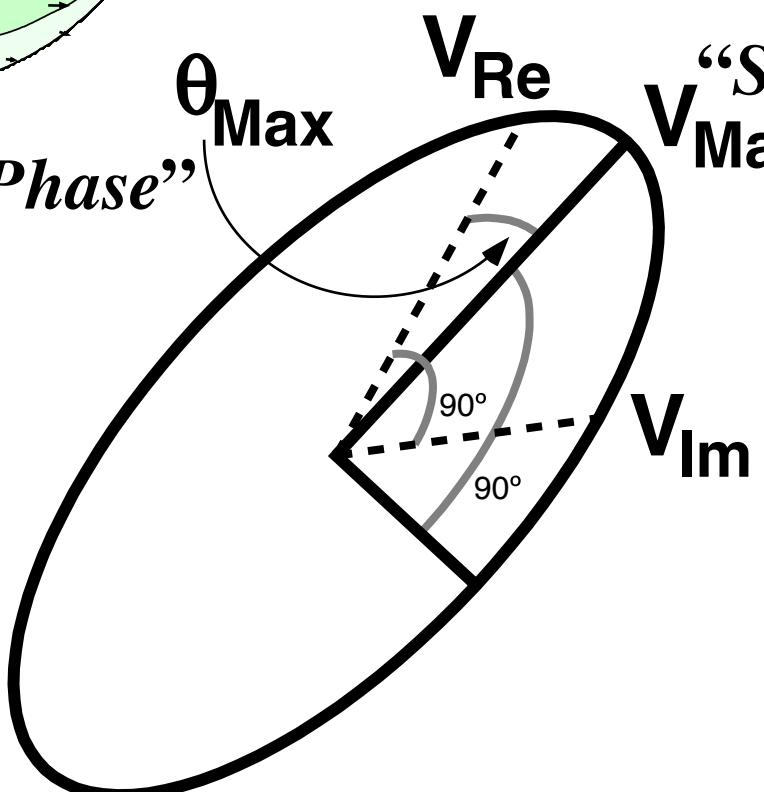
“Sharpness”

$$\eta = \frac{|V_{\text{Min}}|}{|V_{\text{Max}}|}$$

$$0 < \eta < 1$$



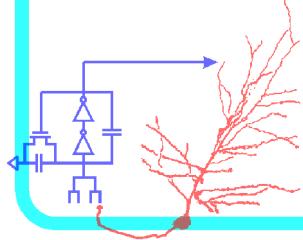
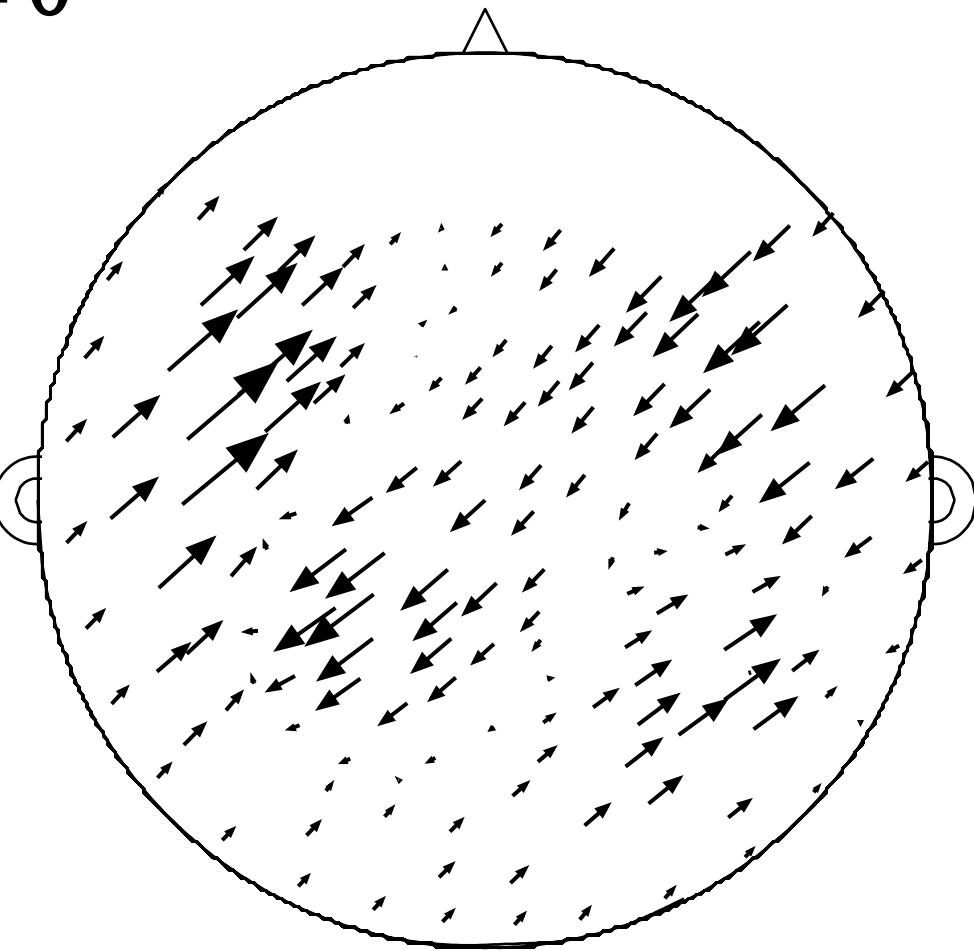
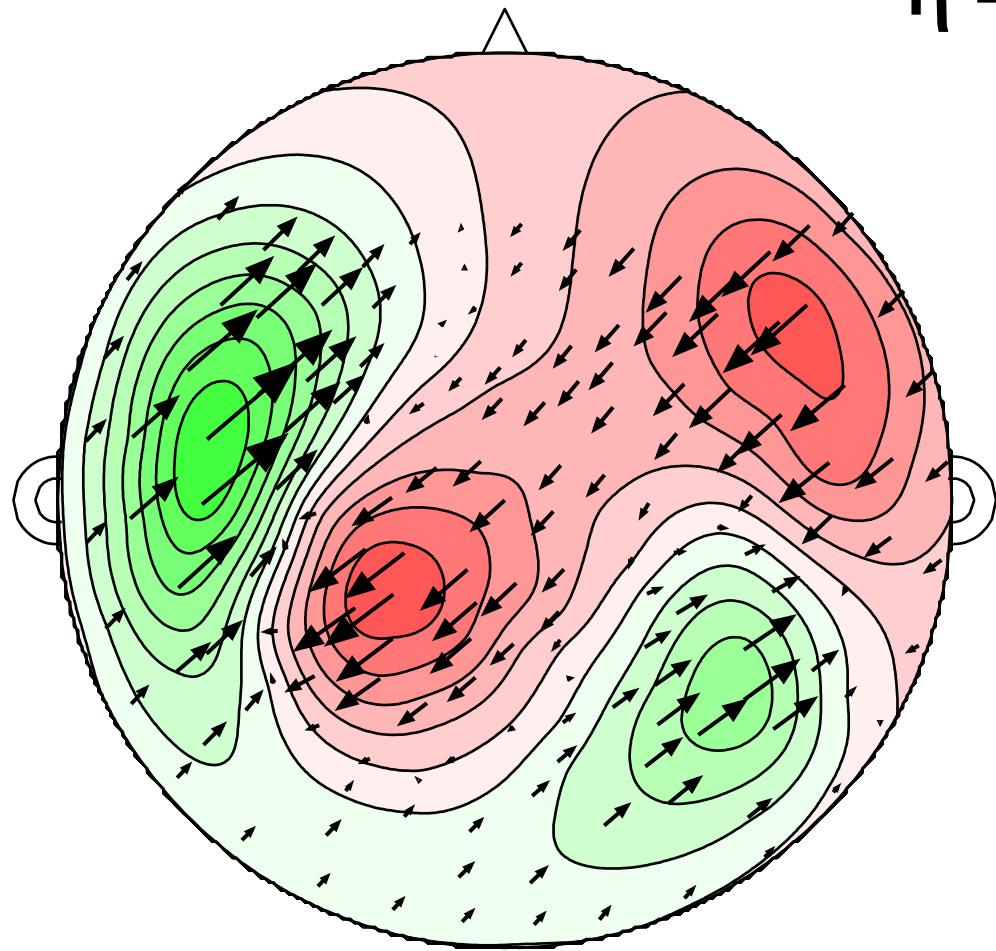
$\hat{V}_{\text{Max}}, \hat{V}_{\text{Min}}$   
Orientations



Physiologically Simple  
Current Sources:  $\eta = 0$

# Single Orientation Current Sources

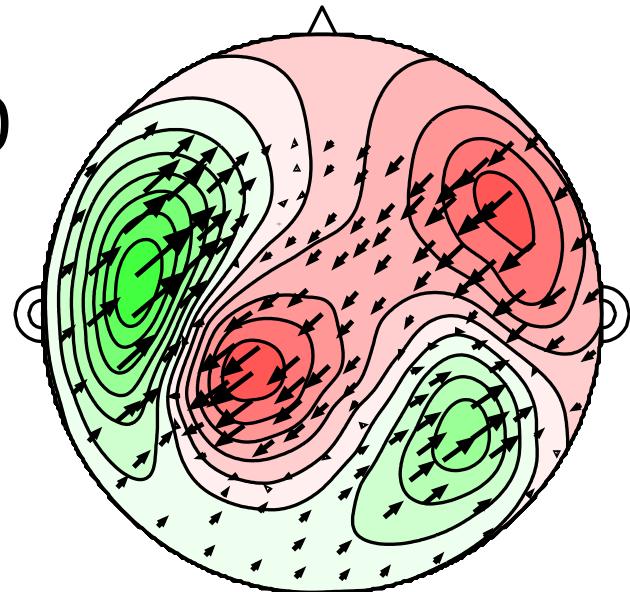
$$\eta = 0$$



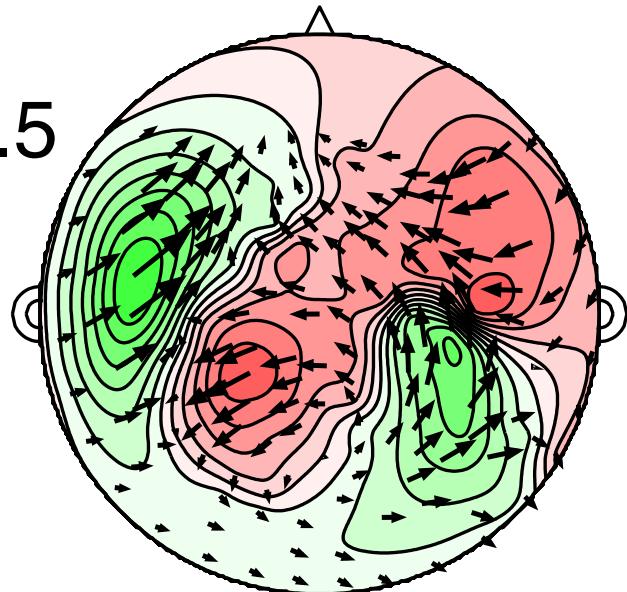
# Simulated Sharpness

Compound/Effective Current Sources

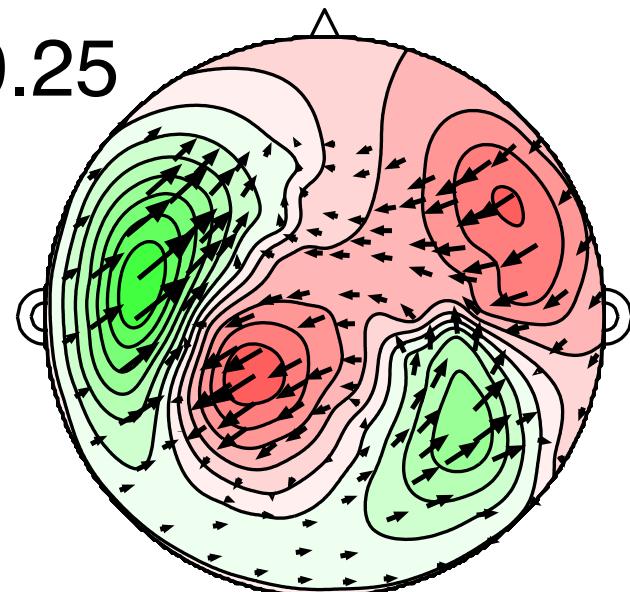
$$\eta_L = 0$$
$$\eta_R = 0$$



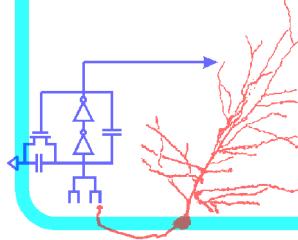
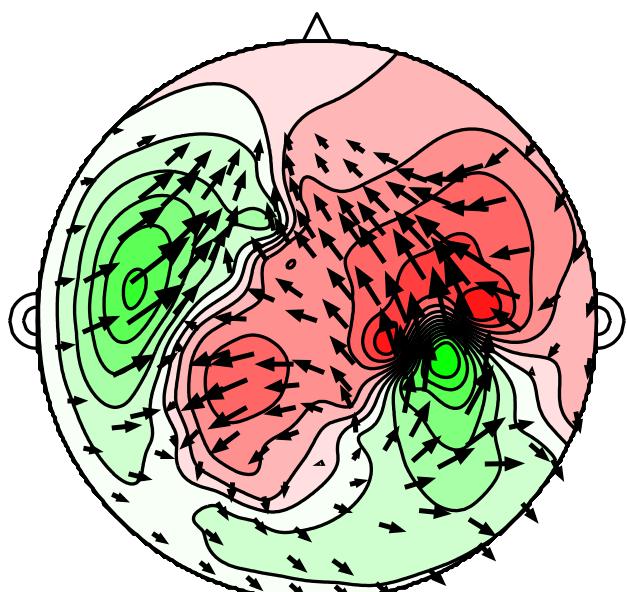
$$\eta_L = 0$$
$$\eta_R = 0.5$$



$$\eta_L = 0$$
$$\eta_R = 0.25$$



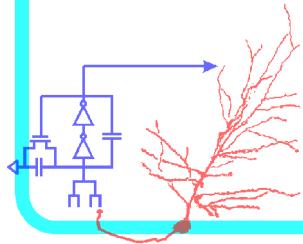
$$\eta_L = 0$$
$$\eta_R = 1$$



# Summary

- Fully Complex MEG necessary
  - Complex Magnetic Flux
  - Generated by Complex Neural Currents
- Complex Neural Current Sources
  - Six Degrees of Freedom:
  - Orientation (2), Strength, Phase, Sharpness, Minor orientation (1)
  - Sharpness → Compound Neural Source

Simon, J. Z. and Y. Wang (2005) *Fully Complex Magnetoencephalography*, J. Neurosci. Methods. 149(1), 64-73.



# Computational Sensorimotor Systems Laboratory

Jonathan Z. Simon

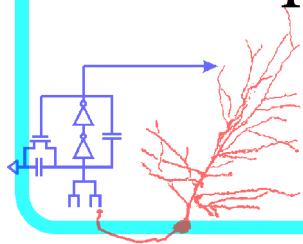
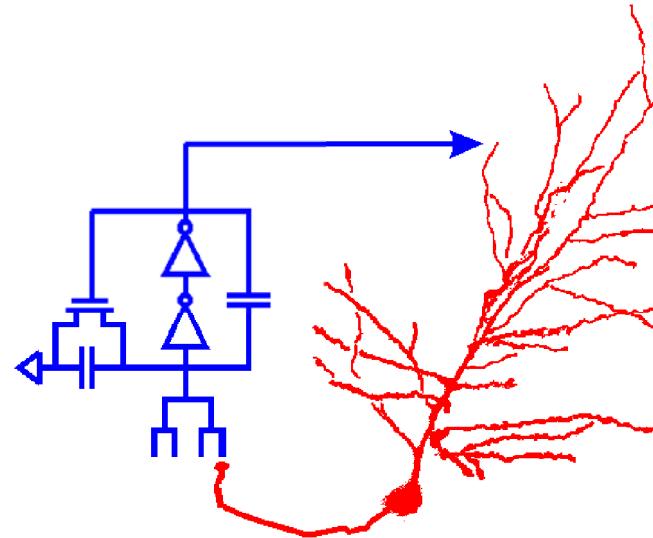
Yadong Wang\*

Juanjuan Xiang  
Maria Chait  
Huan Luo

Timothy Horiuchi

David Poeppel  
Jeff Walker

\*Supported by NIH R01 DC05660



*Thank You*

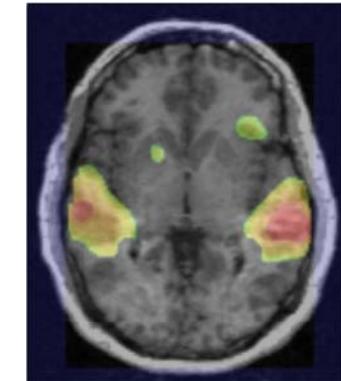
# Functional Imaging

Non-invasive recording  
from human brain  
(Functional brain imaging)

Hemodynamic  
techniques

Positron emission  
tomography  
PET

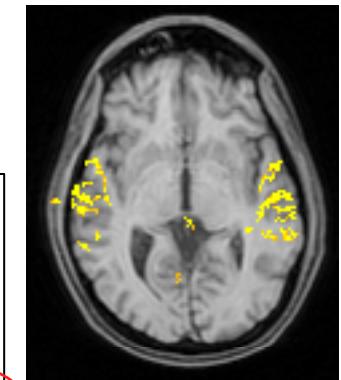
*Excellent spatial resolution*  
( $\sim 1\text{-}2\text{ mm}$ )  
*Poor temporal resolution*  
( $\sim 1\text{ s}$ )



Functional magnetic  
resonance imaging  
fMRI

PET, EEG require  
across-subject  
averaging

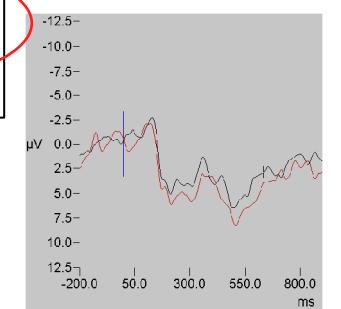
fMRI and MEG can  
capture effects in  
single subjects



Electroencephalography  
EEG

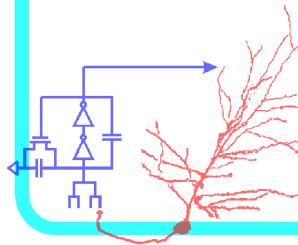
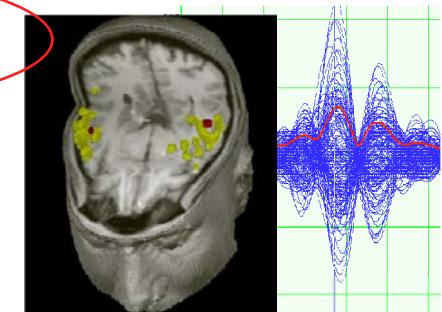
*Poor spatial resolution*  
( $\sim 1\text{ cm}$ )

*Excellent temporal resolution*  
( $\sim 1\text{ ms}$ )

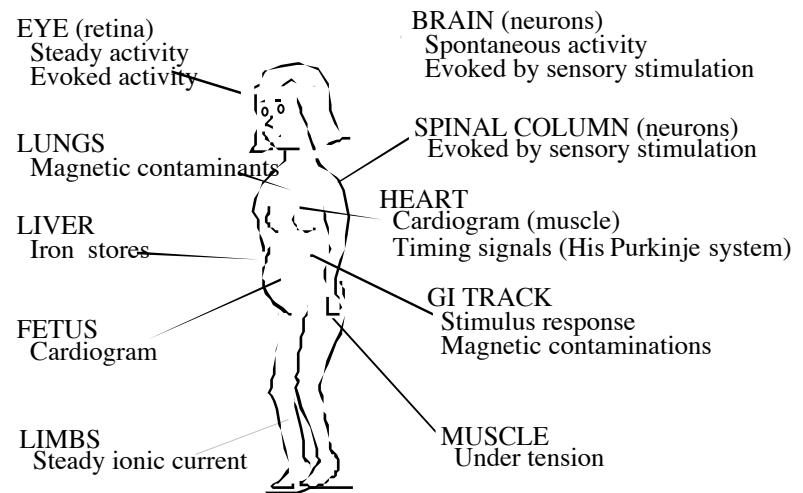
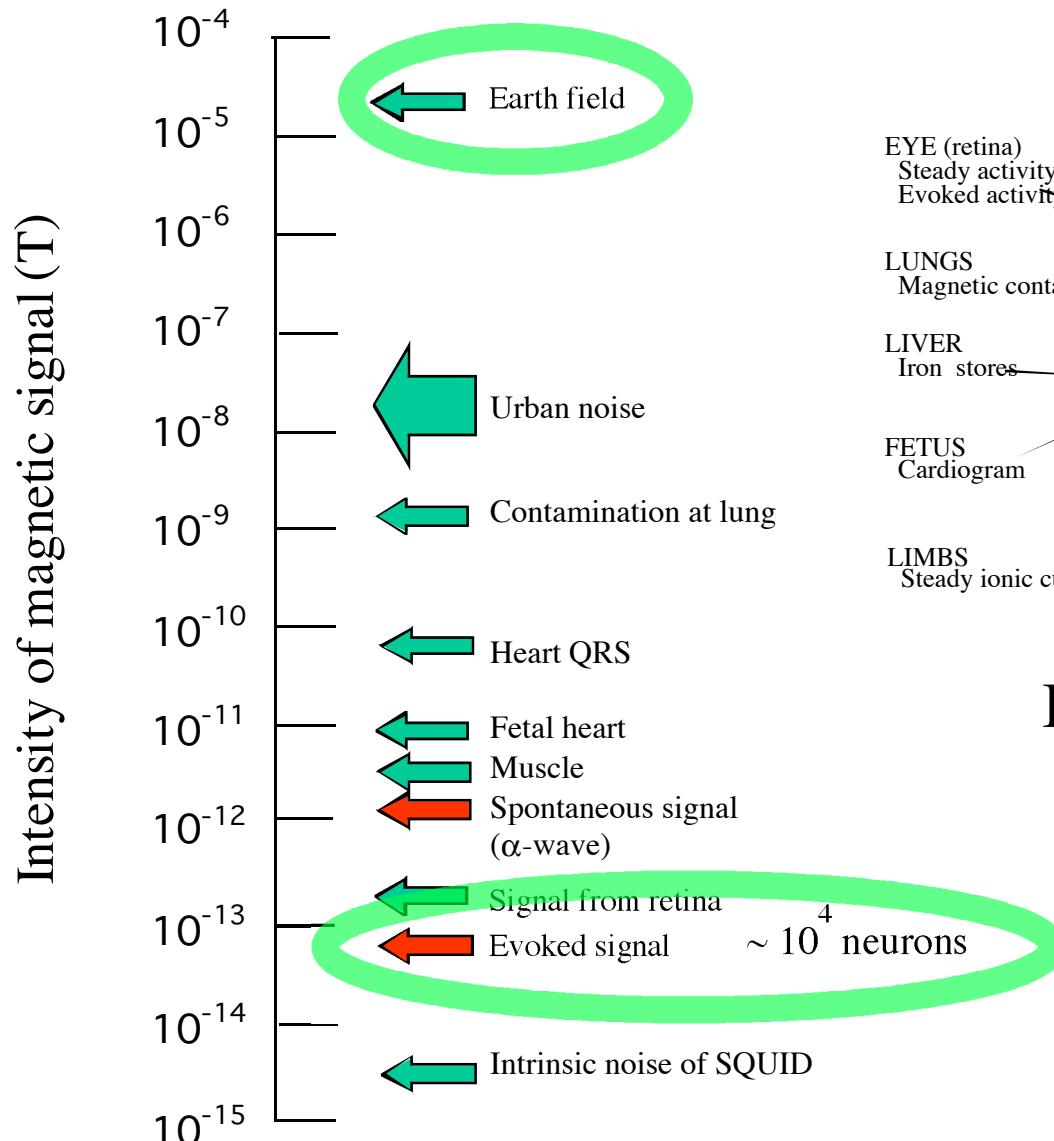
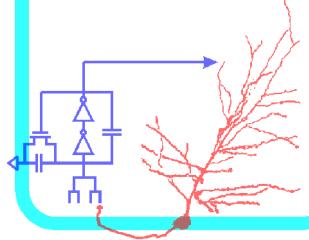


Electromagnetic  
techniques

Magnetoencephalography  
MEG



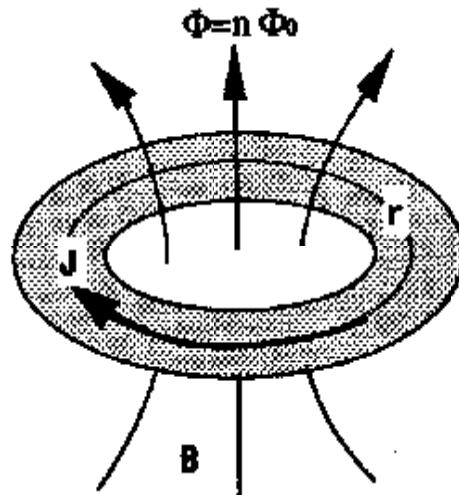
# Magnetic Field Strengths



## Biomagnetism

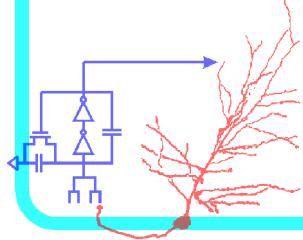
# Magnetic Flux Detectors

Superconductivity →  
Magnetic flux quantization →  
Josephson Effect →  
SQUID = Superconducting Quantum  
Interference Device



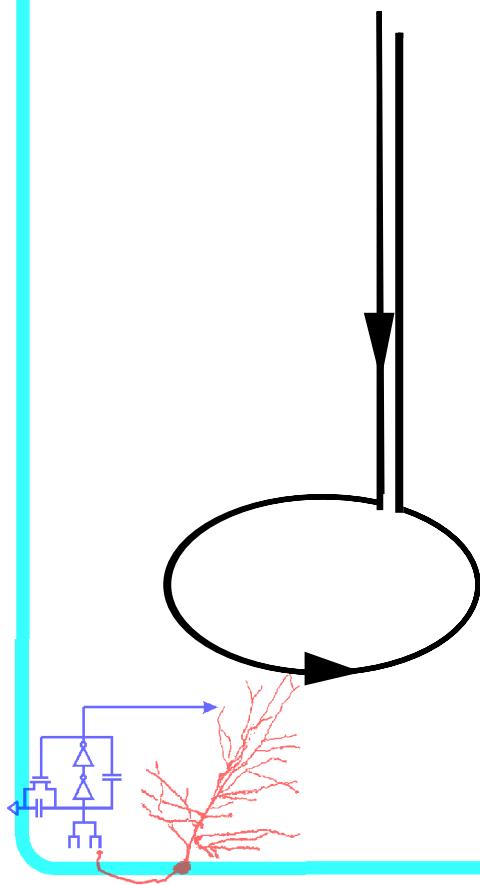
$$\Phi = n \frac{h}{2e} = n \Phi_0$$

$$\Phi_0 = \frac{h}{2e} = 2.07 \times 10^{-15} \text{ Wb}$$



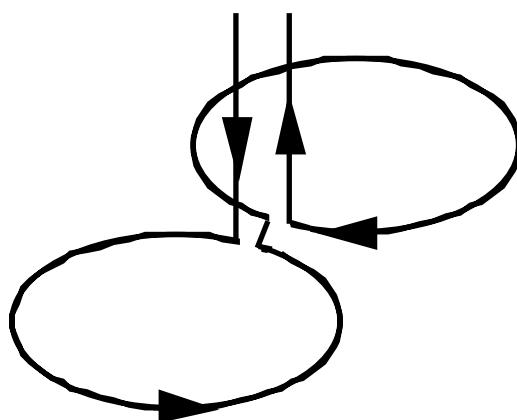
# Sensor Configurations

## SQUID Magnetometer

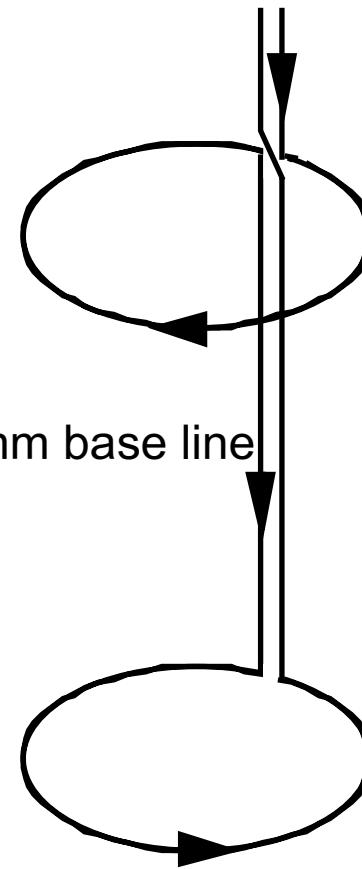


## SQUID Gradiometer

Noise reduction from  
Differential measurement



Planar type

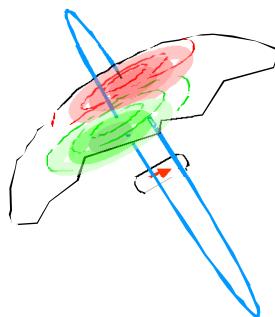


Axial type

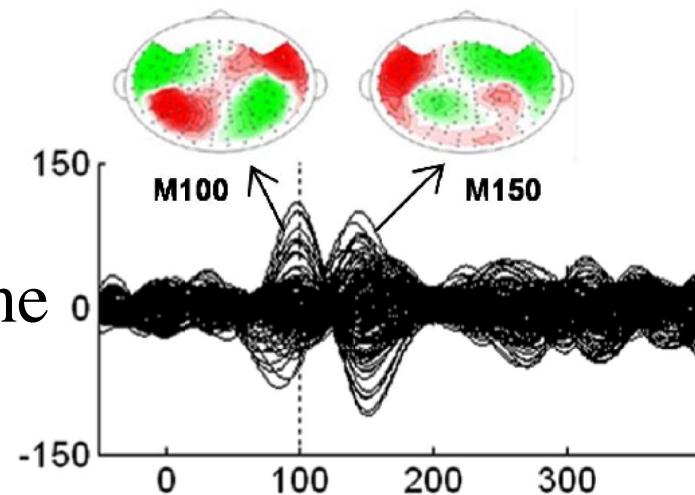
# Time Course of MEG Responses

## Evoked Responses

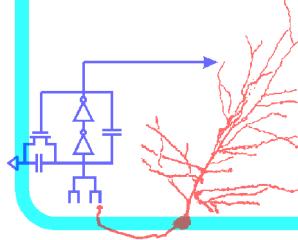
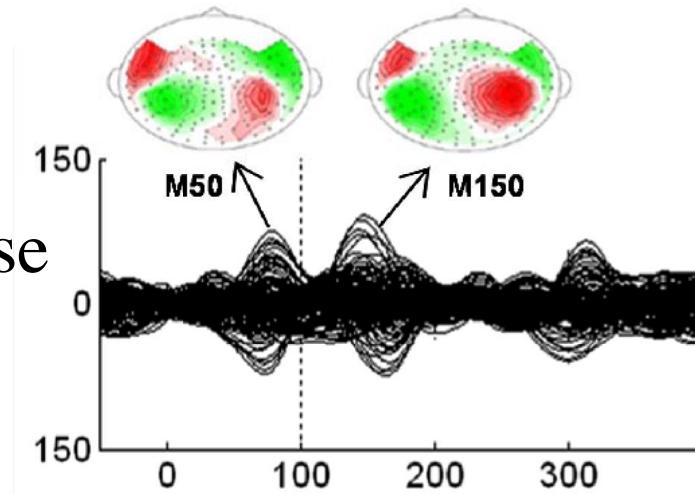
MEG Events Time-Locked  
to Stimulus Event



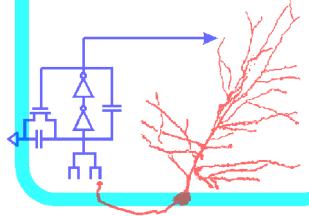
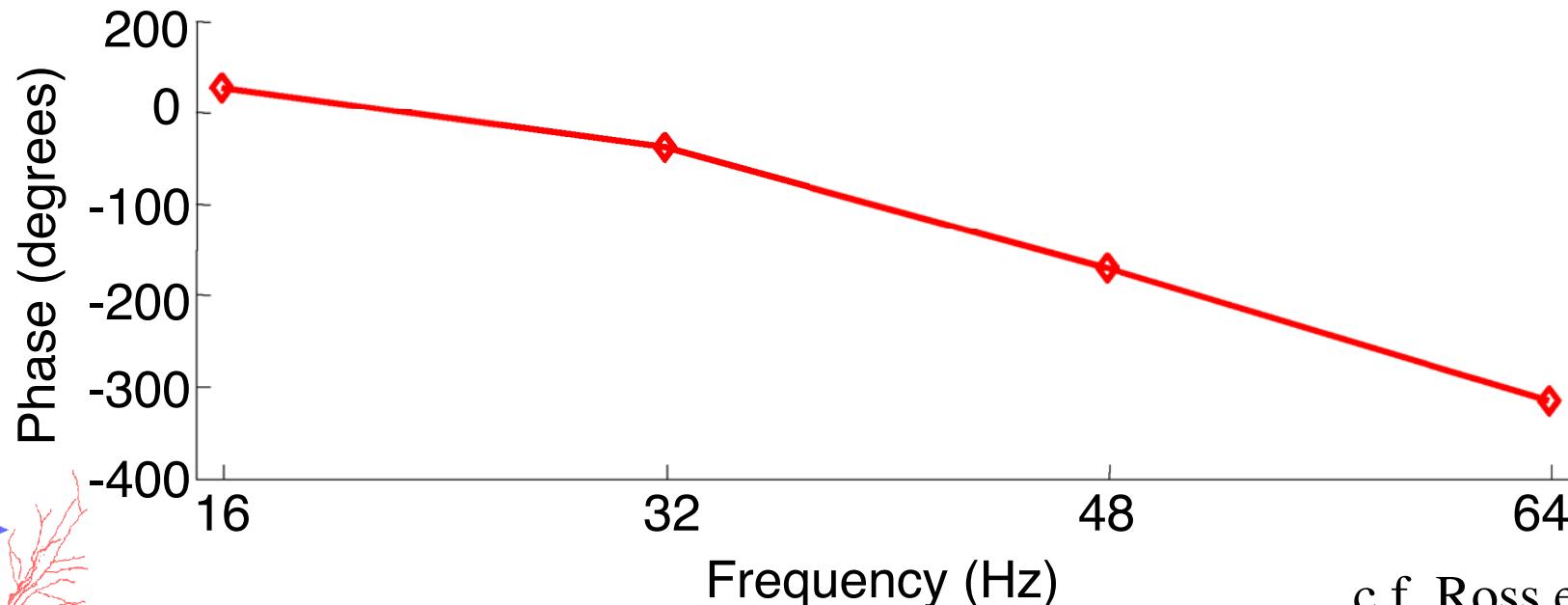
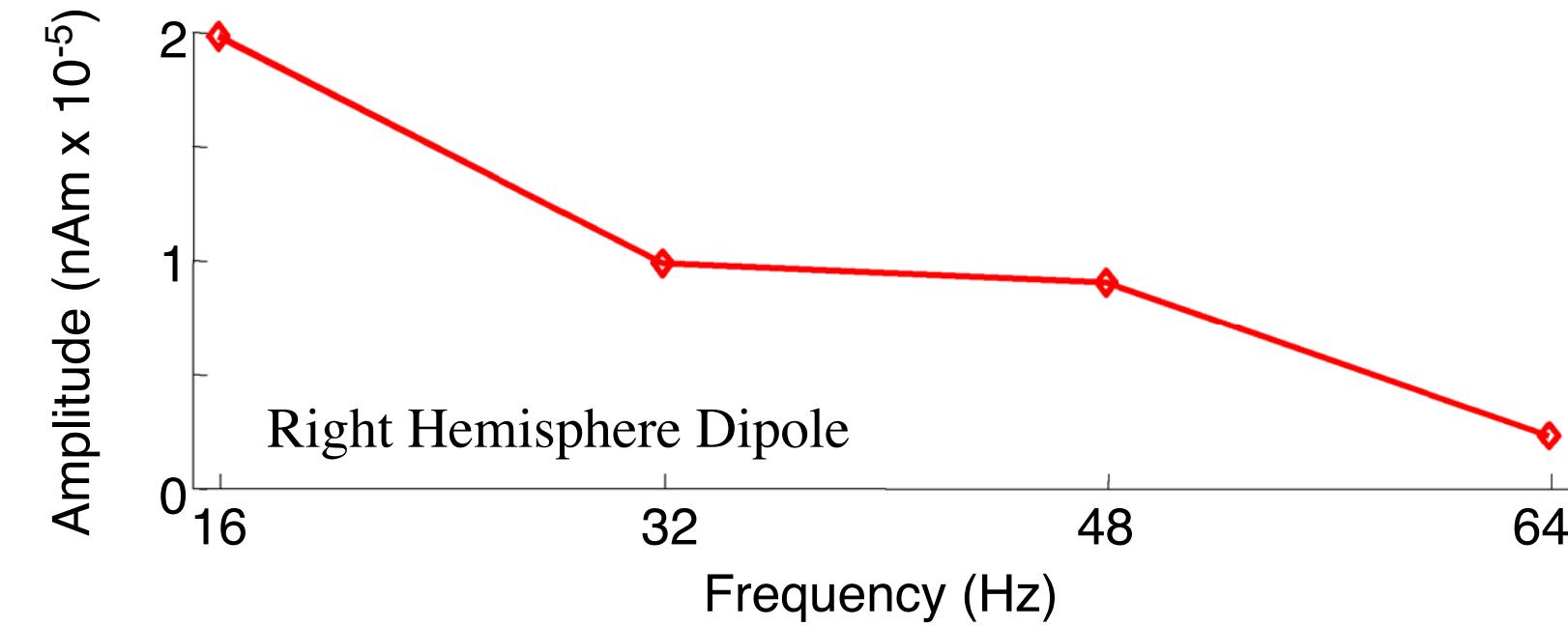
Pure Tone



Broadband Noise



# Neural Modulation Transfer Function



c.f. Ross et al. (2000)