Cortical Localization of the Auditory Temporal Response Function from MEG via non-convex Optimization

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Research Supported by:



- Background
- Motivation
- Unified Computational Framework
- Proposed Algorithm
- Results:
 - A Simulation Study
 - Analysis of MEG from story listening
- Summary

MEG in speech: TRFs

- Linear filter model
- Predicts MEG response from continuous stimulus.
- "Best" Kernel : temporal response function

M100 Attentional state



Cortical origin???

(*adapted from Ding & Simon (2013). Robust cortical encoding of slow temporal modulations of speech. In Basic Aspects of Hearing Springer, New York, NY.)

Existing methods:

Two stage operation Problems:

- High bias
- Leakage
- Limited spatial resolution

Full neural source localization power of MEG

Distributed source model

- N sensors over the scalp
- *T* time points
- MEG matrix, $\mathbf{Y}(N \times T)$

$$oldsymbol{y}_t := egin{bmatrix} y_t^{(1)} \ y_t^{(2)} \ y_t^{(N)} \ y_t^{(N)} \end{bmatrix}$$

(1)

(1)

Sensor space
$$\mathbf{f} \mathbf{Y} := \begin{bmatrix} y_1^{(1)} & y_2^{(1)} & \dots & y_t^{(1)} & \dots & y_T^{(1)} \\ y_1^{(2)} & y_2^{(2)} & \dots & y_t^{(2)} & \dots & y_T^{(2)} \\ \dots & \dots & \dots & \dots & \dots \\ y_1^{(N)} & y_2^{(N)} & \dots & y_t^{(N)} & \dots & y_T^{(N)} \end{bmatrix}$$

Г

(1)

- M voxels
- Time Primary current ~ virtual current dipole
 - Each dipole ~ 3 components, $j_{m,R,t}, j_{m,A,t}, j_{m,S,t}$
 - Neural current matrix, $I(3M \times T)$

(1) **7**

Distributed source model Y = LJ + W

- L: lead-field matrix (*N* × 3*M*) Maxwell's equations
- W: measurement noise matrix

Typically $N\sim 10^2$, $M\sim 10^4$

TRF model

• Assumption: neural sources process the stimulus linearly

$$j_{m,d,t} \stackrel{\bullet}{=} (\boldsymbol{\tau}_{m,d})^{\top} \mathbf{e}_t + v_{m,d,t}$$

- $\boldsymbol{\tau}_{m,d}$: dth component of 3D vector TRFs
- **e**_t : Stimulus history
- In matrix form:

$$J = \Phi S + V$$

- Φ : TRF matrix
- S : stimulus covariate matrix
- V: background activity matrix

Distributed Source ModelY = LJ + WTRF model $J = \Phi S + V$

Our Aim: directly estimate the TRF matrix, Φ given - MEG measurement matrix, Y - stimulus covariate matrix, S

Modelling Assumptions:

$$p(\mathbf{W}) \propto |\mathbf{\Sigma}_w|^{-T/2} \exp{-\frac{1}{2}} \|\mathbf{W}\|_{\mathbf{\Sigma}_w^{-1}}^2$$
$$p(\mathbf{V}|\mathbf{\Gamma}) \propto \prod_{m=1}^M |\Gamma_m|^{-T/2} \exp{-\frac{1}{2}} \sum_{m=1}^M \|V_m\|_{\Gamma_m^{-1}}^2,$$

$$||A||_B := \sqrt{\operatorname{tr} \{A^\top B A\}}$$

Joint distribution:

 $p(\mathbf{Y}, \boldsymbol{J} | \boldsymbol{\Phi}, \boldsymbol{\Gamma}) \propto |\boldsymbol{\Sigma}_w|^{-T/2} \exp{-\frac{1}{2} \|\mathbf{Y} - \mathbf{L}\boldsymbol{J}\|_{\boldsymbol{\Sigma}_w^{-1}}^2} \times |\boldsymbol{\Gamma}|^{-T/2} \exp{-\frac{1}{2} \|\mathbf{J} - \boldsymbol{\Phi}\mathbf{S}\|_{\boldsymbol{\Gamma}^{-1}}}$

Eliminate *J* by marginalization: $p(\mathbf{Y}|\mathbf{\Phi},\mathbf{\Gamma}) \propto |\mathbf{\Sigma}_w + \mathbf{L}\mathbf{\Gamma}\mathbf{L}^\top|^{-T/2} \times \exp\left(-\frac{1}{2}\|\mathbf{Y} - \mathbf{L}\mathbf{\Phi}\mathbf{S}\|^2_{(\mathbf{\Sigma}_w + \mathbf{L}\mathbf{\Gamma}\mathbf{L}^\top)^{-1}}\right)$

(P0)
$$\min_{\mathbf{\Phi}} \frac{1}{2} \|\mathbf{Y} - \mathbf{L}\mathbf{\Phi}\mathbf{S}\|_{(\mathbf{\Sigma}_w + \mathbf{L}\mathbf{\Gamma}\mathbf{L}^\top)^{-1}}^2$$

- Temporal smoothness: Gabor basis $oldsymbol{ au}_{m,d} = {f G}oldsymbol{ heta}_{m,d}$
- Sparsity: Add norm penalty (P1) $\min_{\Theta} \frac{1}{2} \|\mathbf{Y} - \mathbf{L}\Theta \widehat{\mathbf{S}}\|_{(\mathbf{\Sigma}_w + \mathbf{L}\Gamma \mathbf{L}^\top)^{-1}}^2 + \eta \|\Theta\|_{2,1,1}$

2,1,1-Mixed norm

- Direction invariant
- Penalizes only the length of 3D TRF vector
- No prior assumptions on the source activity directions!!!



(P1)
$$\min_{\boldsymbol{\Theta}} \frac{1}{2} \| \mathbf{Y} - \mathbf{L} \boldsymbol{\Theta} \widehat{\mathbf{S}} \|_{(\boldsymbol{\Sigma}_w + \mathbf{L} \boldsymbol{\Gamma} \mathbf{L}^\top)^{-1}}^2 + \eta \| \boldsymbol{\Theta} \|_{2,1,1}$$

- Easy to solve for Θ
- But requires knowledge of Γ
- Not available.
- Idea: Solve for both TRF matrix, and source variance

(P2)
$$\min_{\boldsymbol{\Theta},\boldsymbol{\Gamma}} \frac{T}{2} \log \left(\boldsymbol{\Sigma}_w + \mathbf{L} \boldsymbol{\Gamma} \mathbf{L}^{\top} \right) + \frac{1}{2} \| \mathbf{Y} - \mathbf{L} \boldsymbol{\Theta} \widehat{\mathbf{S}} \|_{(\boldsymbol{\Sigma}_w + \mathbf{L} \boldsymbol{\Gamma} \mathbf{L}^{\top})^{-1}}^2 + \eta \| \boldsymbol{\Theta} \|_{2,1,1}$$

(P2)
$$\min_{\boldsymbol{\Theta},\boldsymbol{\Gamma}} \frac{T}{2} \log \left(\boldsymbol{\Sigma}_w + \mathbf{L} \boldsymbol{\Gamma} \mathbf{L}^{\top} \right) + \frac{1}{2} \| \mathbf{Y} - \mathbf{L} \boldsymbol{\Theta} \widehat{\mathbf{S}} \|_{(\boldsymbol{\Sigma}_w + \mathbf{L} \boldsymbol{\Gamma} \mathbf{L}^{\top})^{-1}}^2 + \eta \| \boldsymbol{\Theta} \|_{2,1,1}$$

- Non-convex in г
- Direct optimization hard
- Update Γ and Θ alternatingly
- Co-ordinate descent algorithm



- non-convex problem
- 'Champagne' (Wipf et al., 2010)
- each pass is guaranteed to reduce cost function

- smooth + non-smooth
- forward-backward splitting
- 'FASTA' (Goldstein et al., 2014)

Dataset

• MEG Data

- 17 participants.
 Two 60-second segments from 'The Legend of Sleepy Hollow' by Washington Irving.
 3 repetitions for each segment.
- Average "brain model" - 'fsaverage', FreeSurfer. – scaled and coregistered to each subject's head. - volume source space. - free orientation lead-field matrix.

Dataset (Continued...)

• Stimulus representation:

 acoustic envelope, average over frequency band of an auditory spectrogram representation

• Statistical Tests:

– spatial smoothing w/ Gaussian kernel (s.d. 10 mm).

tested for consistent directionality vs.
uniformity (Mardia, 2009) using permutation test.

Simulation Results:

- finer source space
- direction constrained



Auditory response functions



Only significant (p <.05) values are shown.

- a new framework for direct TRF localization
- integrates the TRF and distributed forward source models
- alternatingly update the TRFs and Source variances to optimize the objective.
- Improves estimates + their location

References:

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Some of this work has been accepted for presentation at 2018 annual meeting, Society for Neuroscience, San Diego, CA



Thank you! Questions?

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