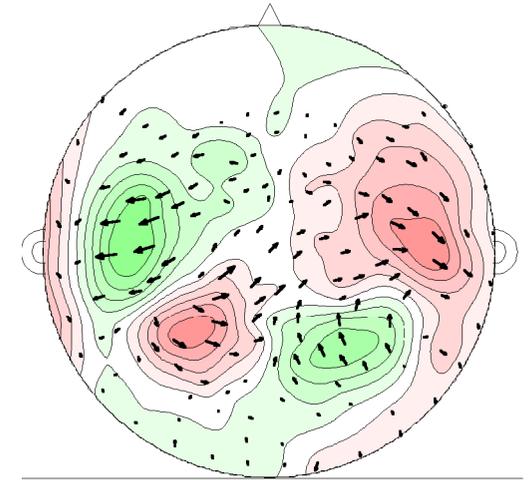


# Measuring Brain Dynamics: Investigating Auditory Processing with Magnetoencephalography



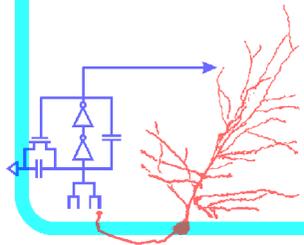
Jonathan Z. Simon

*Biology / Electrical & Computer Engineering*

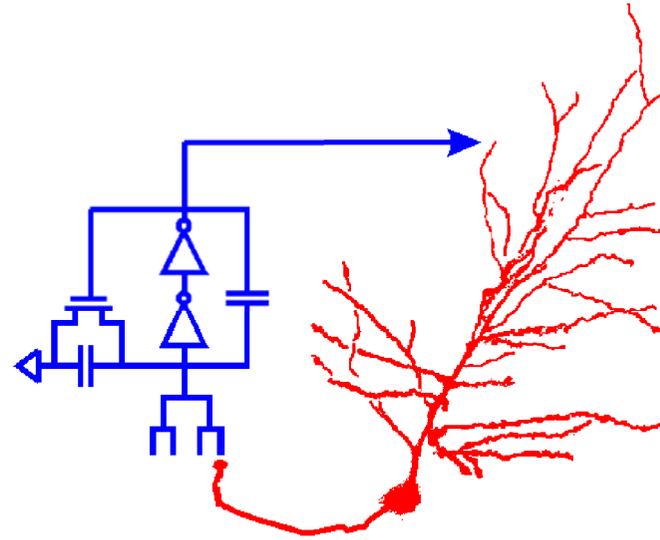
*Neuroscience and Cognitive Sciences*

*Bioengineering*

University of Maryland, College Park



# Computational Sensorimotor Systems Laboratory



Yadong Wang

Juanjuan Xiang

Nayef Ahmar

Maria Chait

Ling Ma

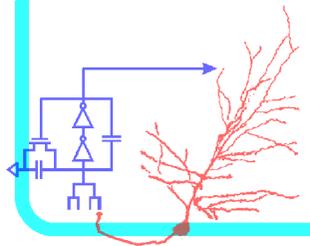
Huan Luo

David Poeppel  
Timothy Horiuchi

Madvhi Jain  
Jeff Walker

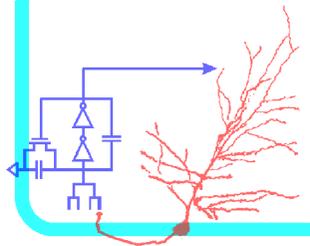
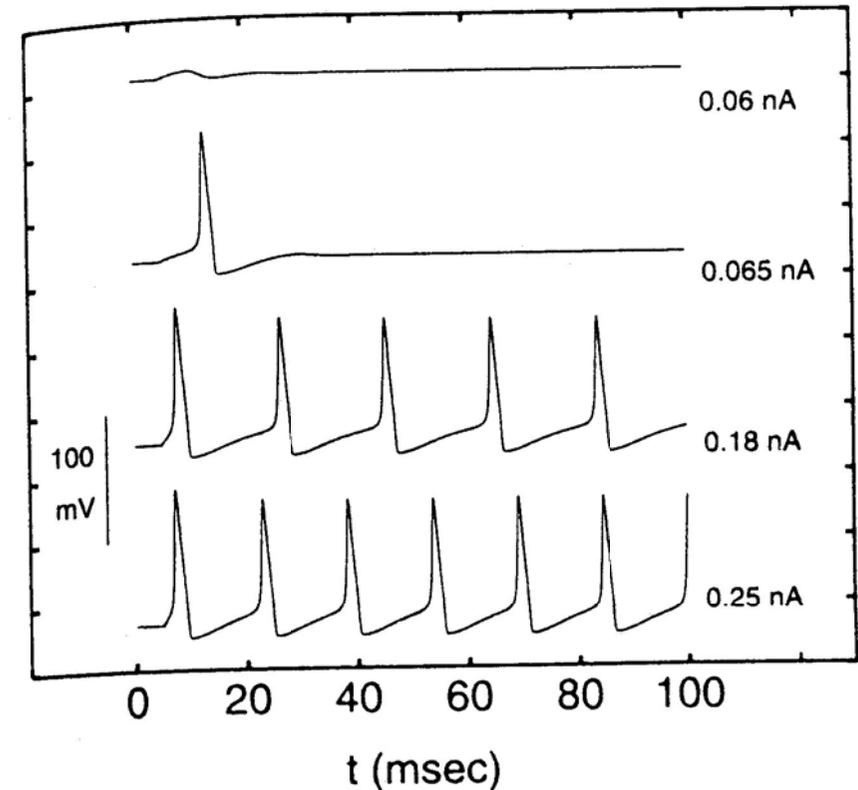
# Outline

- The Brain and How It Works
- The Auditory System
- Magnetoencephalography (MEG)
- Using MEG to explore the Auditory System

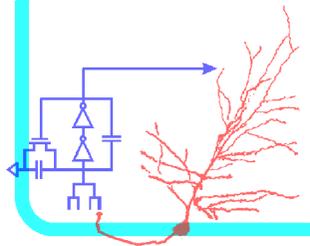
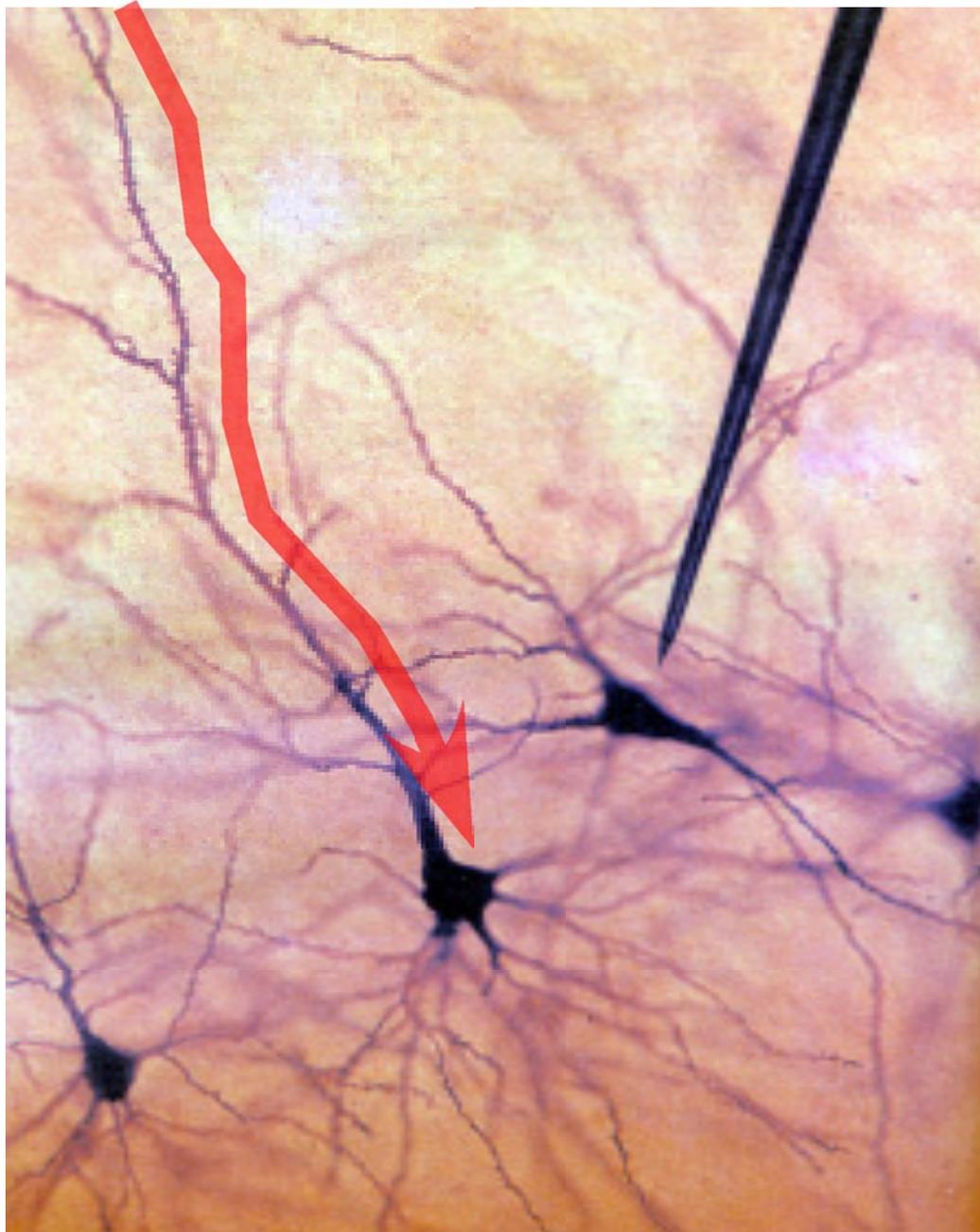


# Universal Neural Code

- Neural signals = spikes in voltage
- Spikes are “all-or-none”
  - Digital in amplitude
  - Analog in time
- Neural Input  $\approx$  current

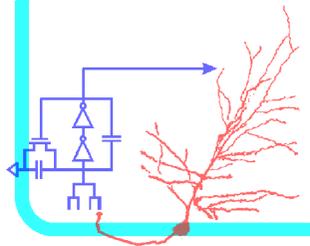


# Primary Neural Current



# Outline

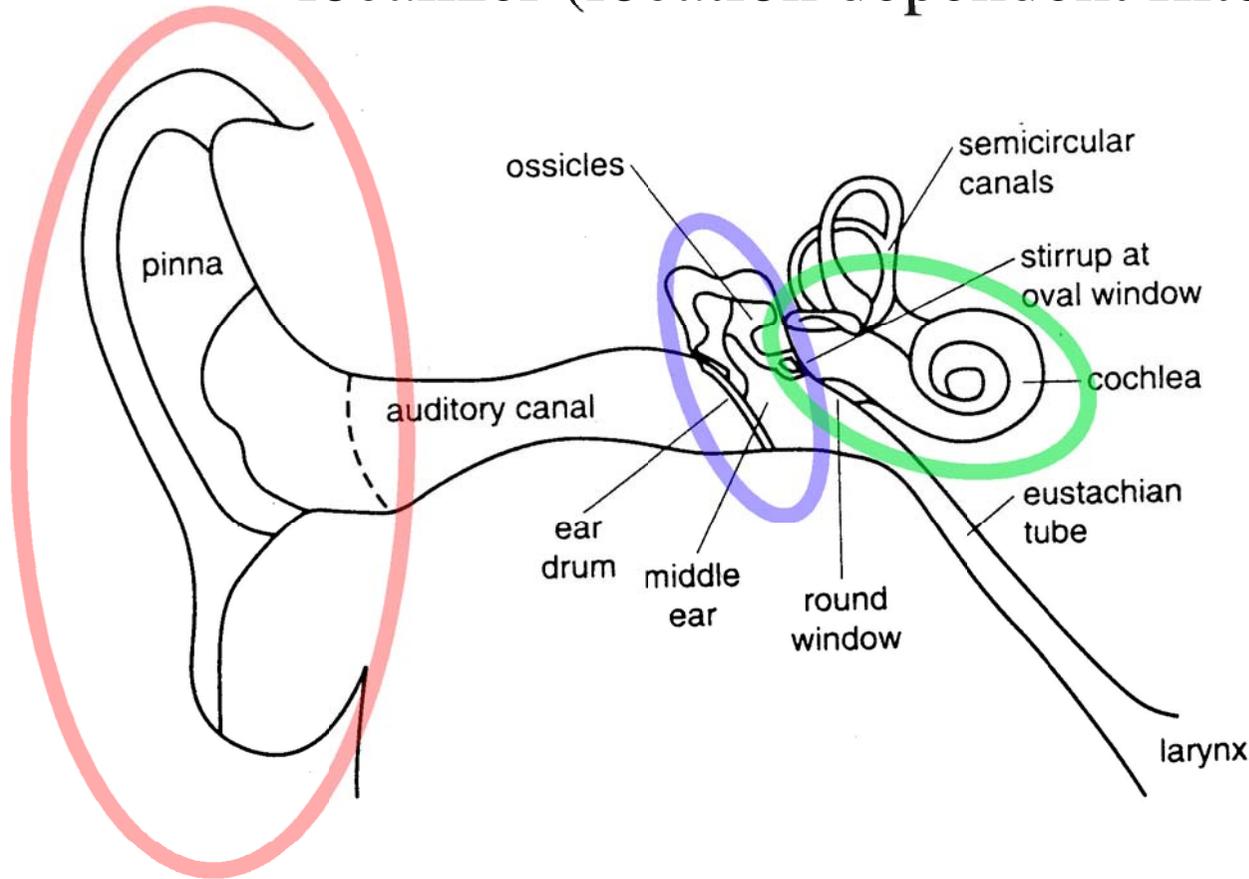
- The Brain and how it works
- **The Auditory System**
- Magnetoencephalography (MEG)
- Using MEG to explore the Auditory System



# What Is Hearing?

**Outer Ear (pinna)** useful but not essential

- collector
- localizer (location dependent filtering)



**Inner ear (cochlea)**

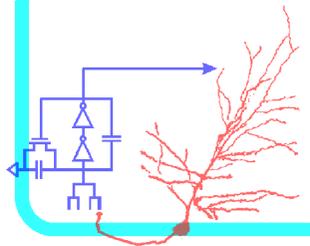
- essential
- neural “transducer”
- turns *acoustic* signals into spikes  
= *auditory* signals

Only features conveyed as neural signals perceived

- e.g. masked sounds  
not conveyed neurally

**Middle Ear** useful but not essential

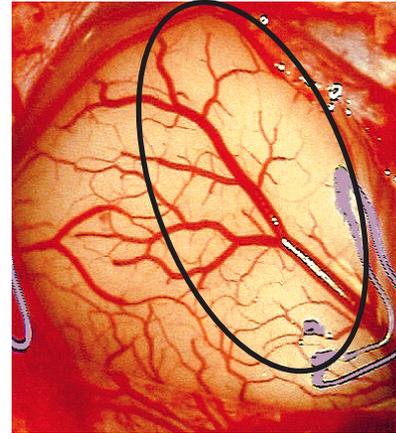
- impedance matching = minimized reflection



# The Auditory Pathway (oversimplified)

Parallel and serial neural processing in multiple stages

Auditory Cortex



ferret

*Phase-locks to envelope of acoustic waveform up to ~20 Hz*

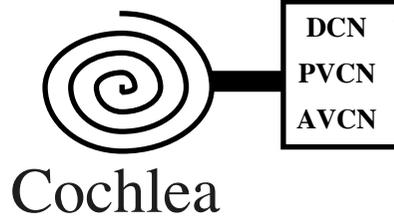
Cochlea

*Linear distance ~ log f*

*Phase-locks to acoustic waveform itself up to ~2 kHz*



human



Cochlea

Auditory Cortex

MGB

IC

NLL

LL

MSO

LSO

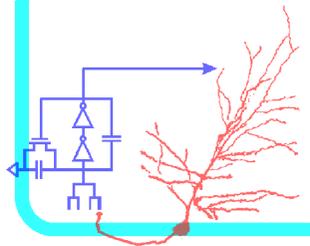
Contralateral

Ipsilateral

BB

# What Is the Auditory Neural Code?

- **Neural code is essentially unknown** for almost all auditory features
  - Especially in auditory cortex
  - Much progress in coding near periphery, especially coding of sound location
- **Most important auditory features are acoustically non-trivial**
  - e.g. speech, speaker ID, emotional content, pitch, timbre, sound location, and many, many others



# What Can We Hear?

**Table 1.6. Approximate ranges of hearing**

Species	Low	High (kHz)
Human	20 Hz	20
Chimpanzee	100 Hz	20
Rhesus monkey	75 Hz	25
Squirrel monkey	75 Hz	25
Cat	30 Hz	50
Dog	50 Hz	46
Chinchilla	75 Hz	20
Rat	1 kHz	60
Mouse	1 kHz	100
Guinea pig	150 Hz	50
Rabbit	300 Hz	45
Bats	3 kHz	120
Dolphin ( <i>Tursiops</i> )	1 kHz	130
Galago	250 Hz	45
Tupaia	250 Hz	45
Sparrow	250 Hz	12
Pigeon	200 Hz	10
Turtle	20 Hz	1
Frog	100 Hz	3
Goldfish	100 Hz	2
Ostariophysi	50 Hz	7
Other teleosts	50 Hz	1

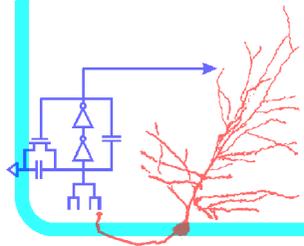
Data taken from Fay 1988

Human: 20 Hz to 20 kHz

Cat: 30 Hz to 50 kHz

Mouse: 1 kHz to 20 kHz

Bat: 1 kHz to 120 kHz



# What Can We Hear?

- **Spectro-Temporal Features of Any Sound**

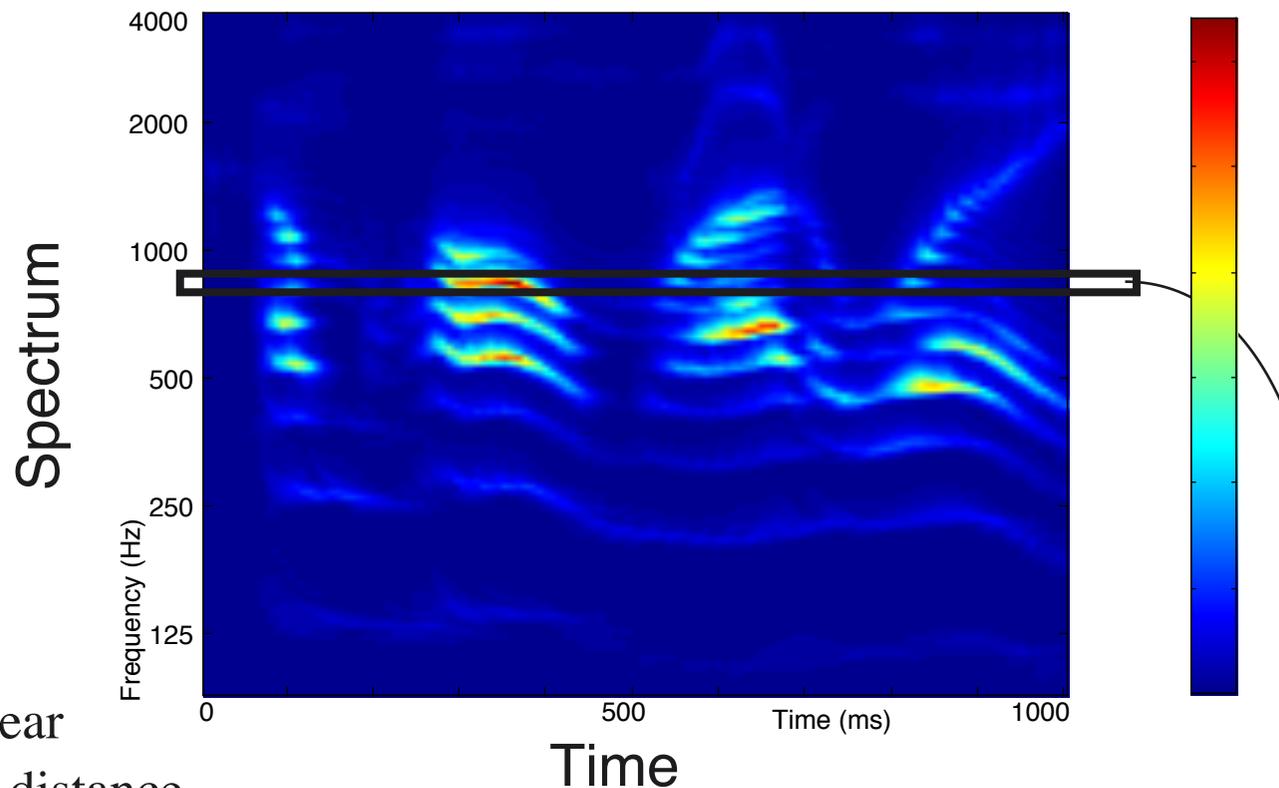
Spectral content of sound as a function of time.

Which spectral frequency bands have enhanced power?

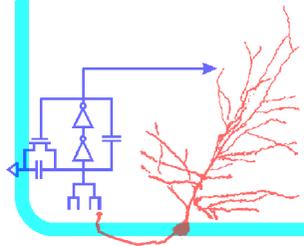
Which spectral frequency bands have diminished power?

How do these change as a function of time?

*“Come home right away.”*



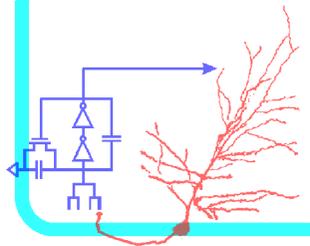
$\log f = \text{linear}$   
cochlear distance



*Characterization  
from frequency  
cross-section is  
very limited*

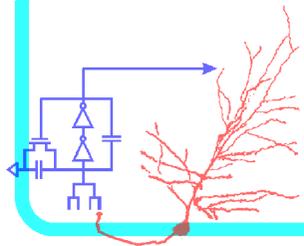
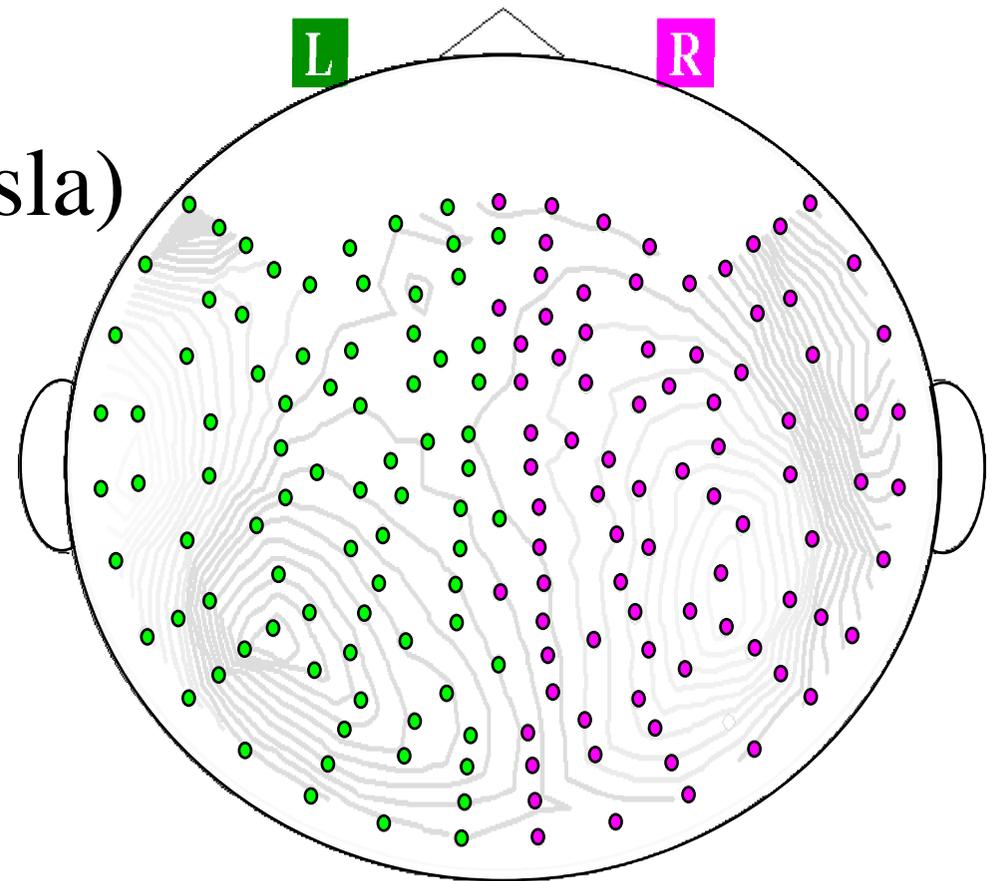
# Outline

- The Brain and how it works
- The Auditory System
- **Magnetoencephalography (MEG)**
- Using MEG to explore the Auditory System



# MEG – Magnetoencephalography

- Simultaneous Whole Head recordings  
160 sensors (3 reference)
- Exquisitely Sensitive  
~ 100 fT ( $10^{-13}$  Tesla)  
~  $10^4$  neurons
- Temporal Resolution  
~ 1 ms



# Functional Imaging

Non-invasive recording  
from human brain  
(Functional brain imaging)

Hemodynamic  
techniques

Positron emission  
tomography  
PET

Excellent *spatial resolution*  
( $\sim 1-2$  mm)  
Poor *temporal resolution*  
( $\sim 1$  s)

Functional magnetic  
resonance imaging  
fMRI

PET, EEG require  
across-subject  
averaging

fMRI and MEG can  
capture effects in  
single subjects

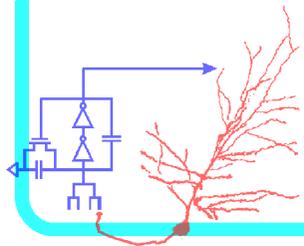
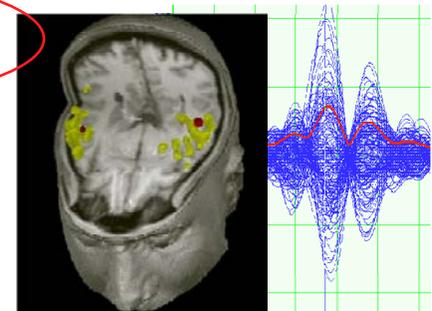
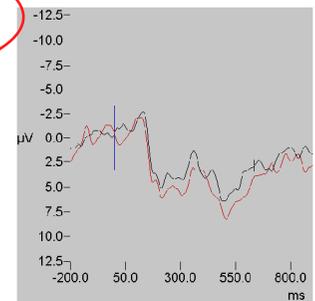
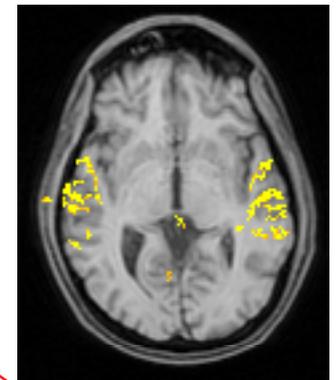
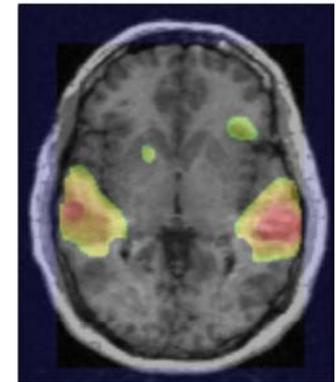
Electroencephalography  
EEG

Poor *spatial resolution*  
( $\sim 1$  cm)

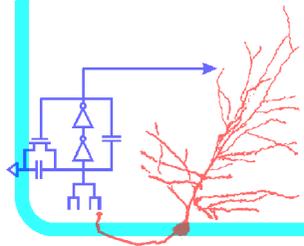
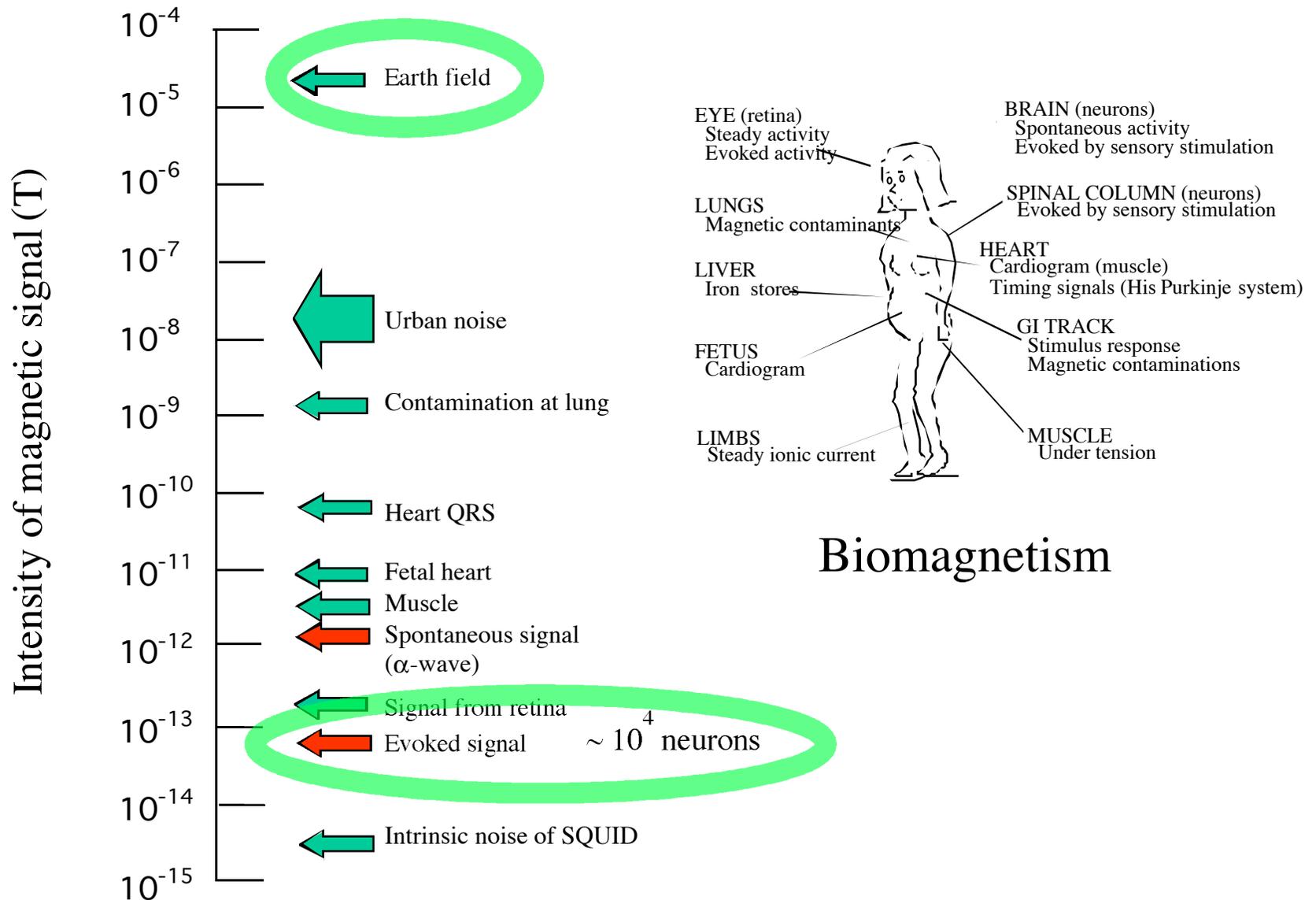
Excellent *temporal resolution*  
( $\sim 1$  ms)

Electromagnetic  
techniques

Magnetoencephalography  
MEG

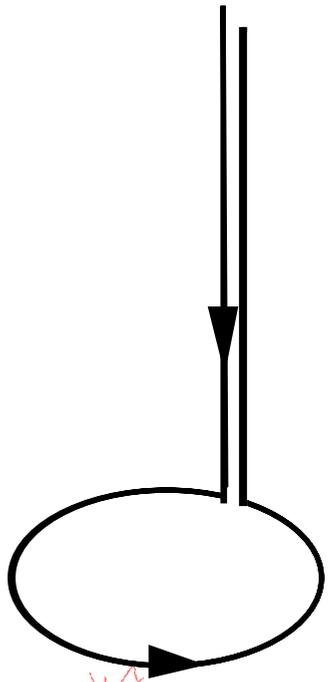


# Magnetic Field Strengths



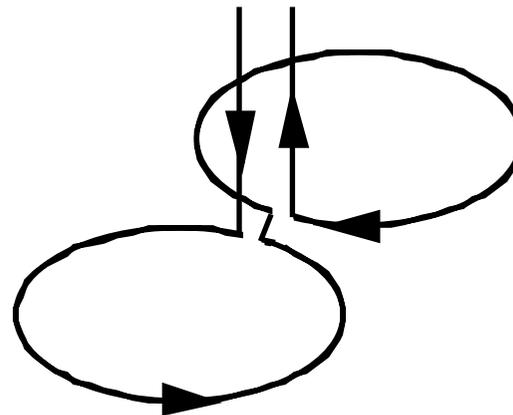
# Sensor Configurations

SQUID  
Magnetometer

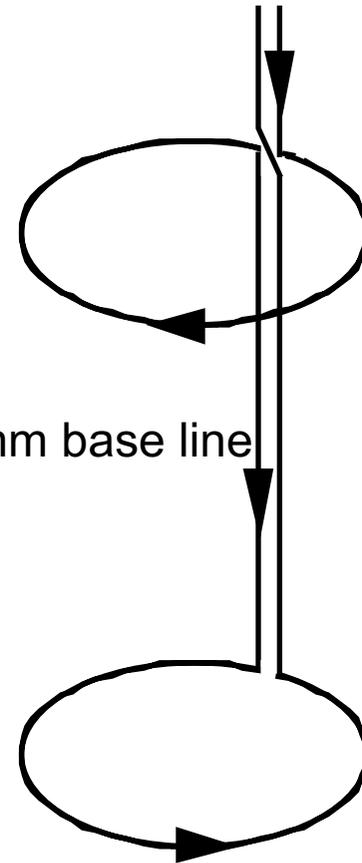


SQUID  
Gradiometer

Noise reduction from  
Differential measurement

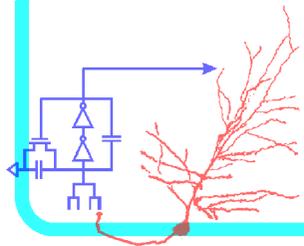
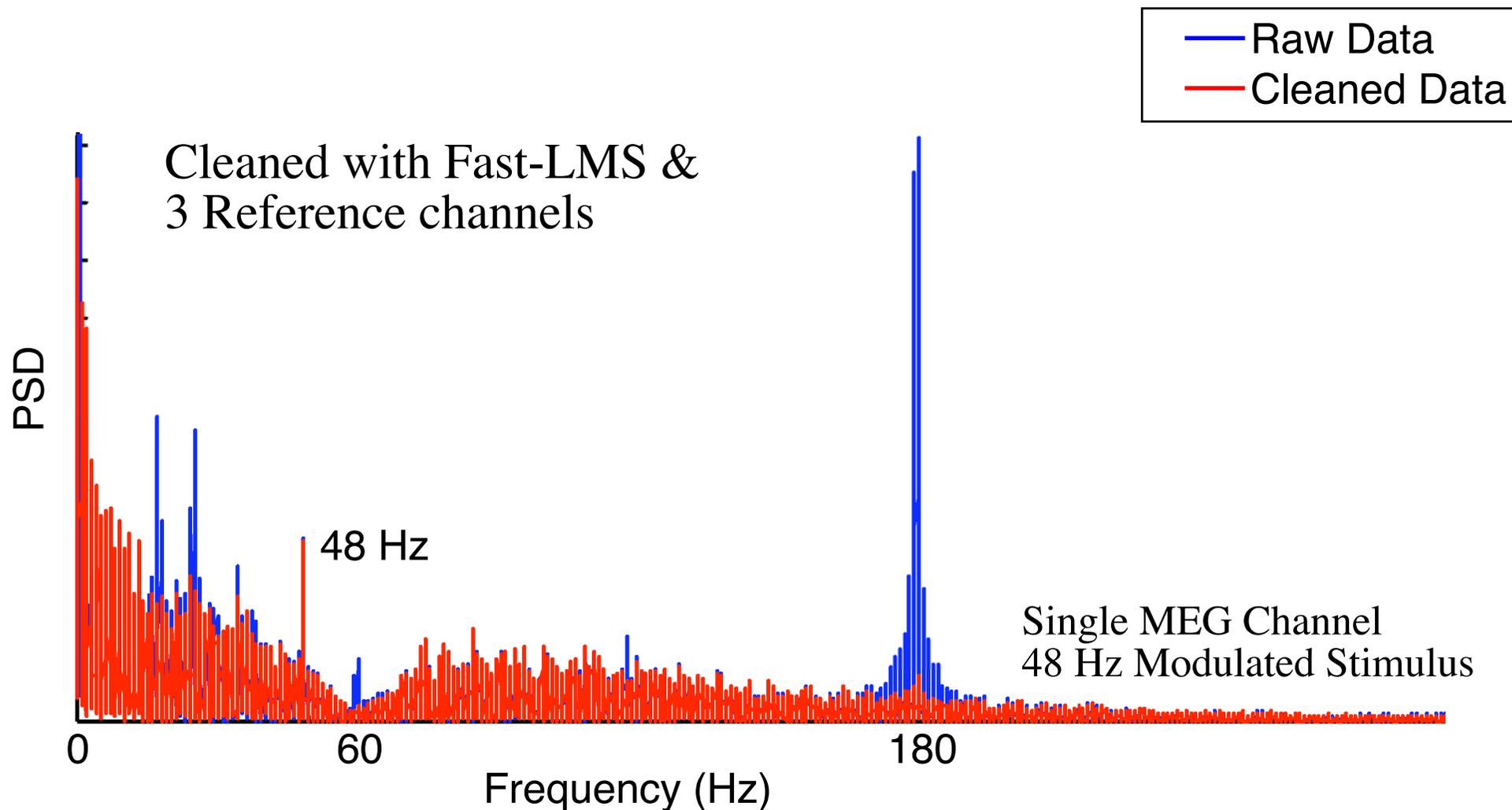


Planar type

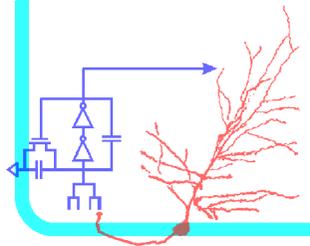


Axial type

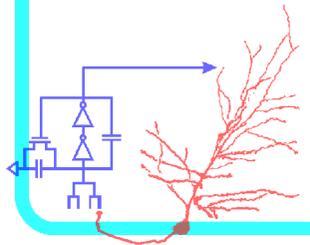
# Noise Reduction in Software



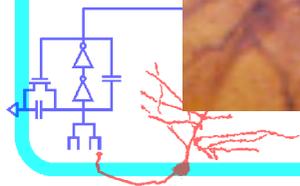
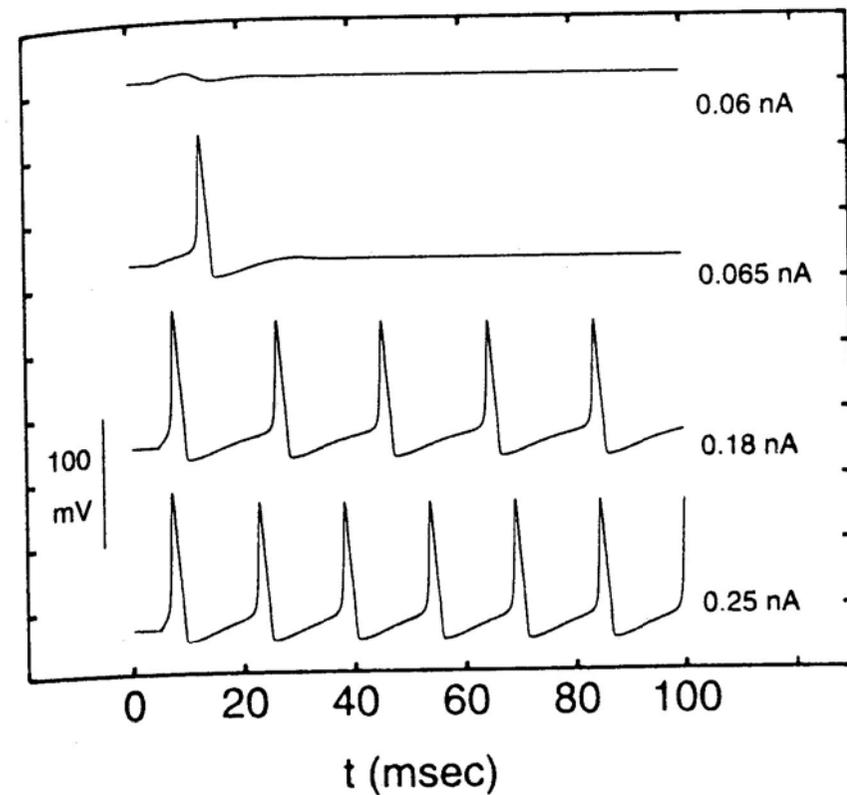
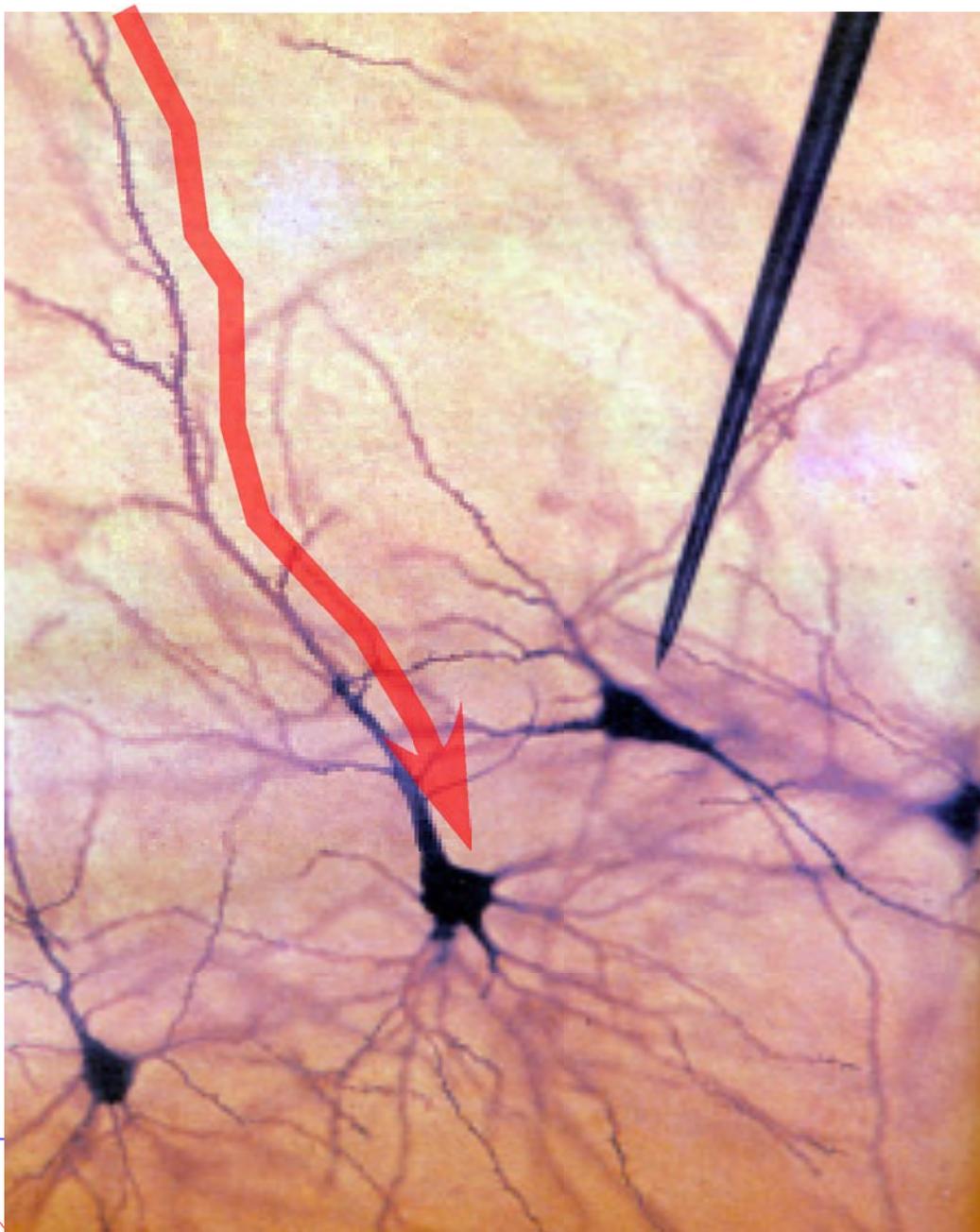
# Noise Reduction in Hardware



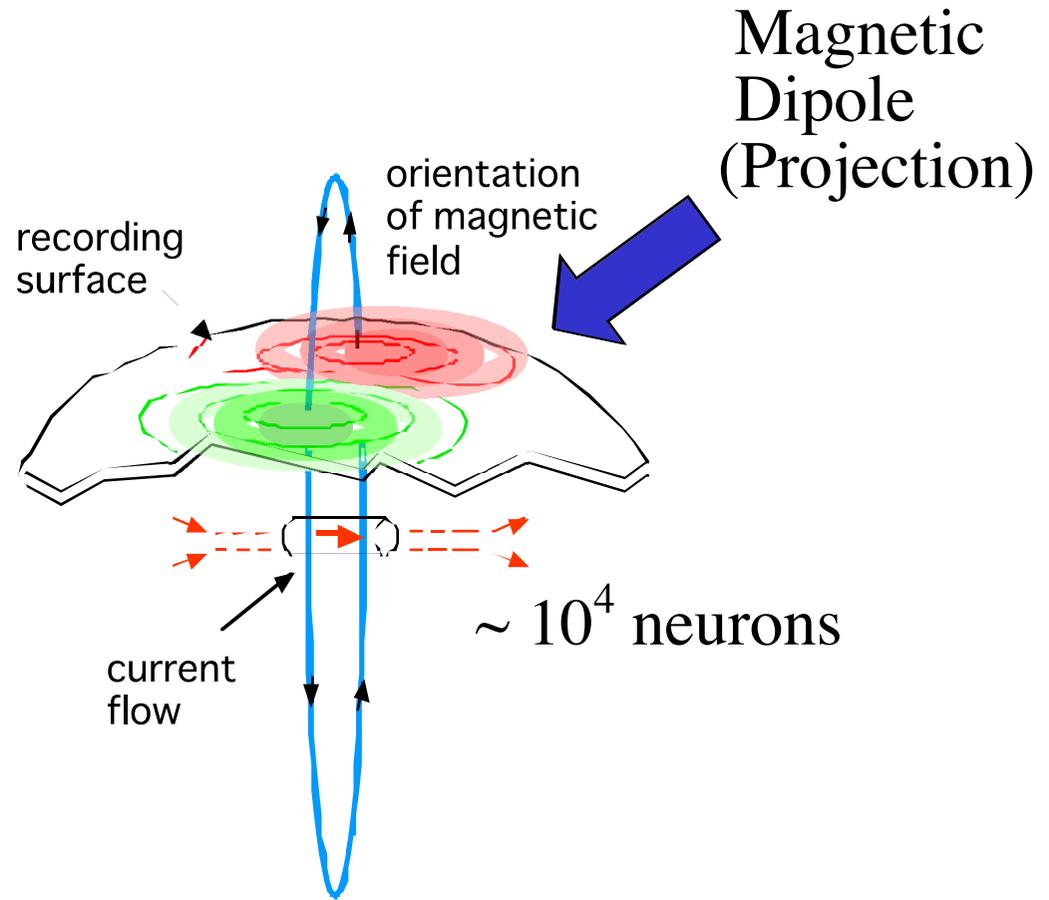
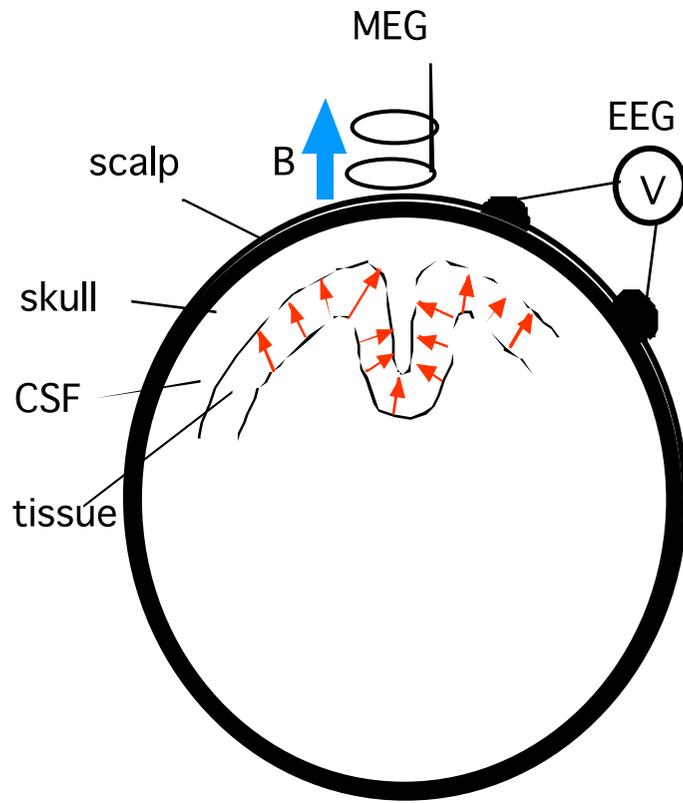
# MEG at University of Maryland



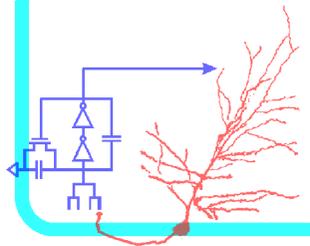
# Neural Activity = Neural Current



# MEG Magnetic Signal



Non-invasive measurement  
Direct measurement of Neural Activity



# MEG compared to EEG

Temporal resolution high as EEG

Fast, easy set-up

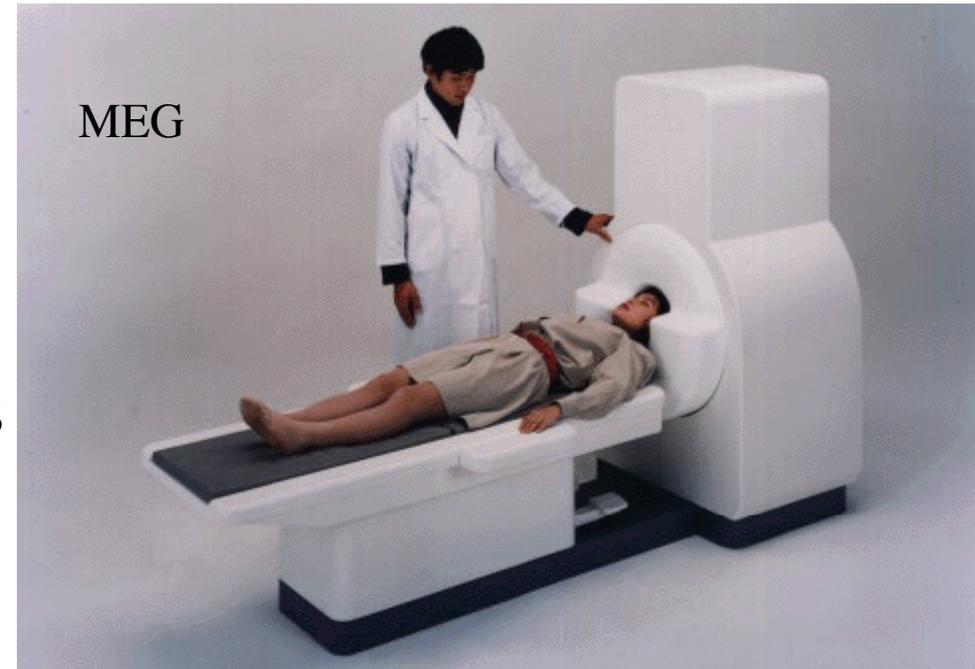
Magnetic fields are not attenuated or distorted, unlike electric fields

Higher spatial resolution

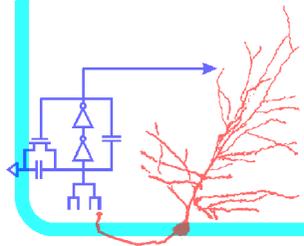
Expensive

Inverse problem worse? better?

## Complementary Techniques



EEG

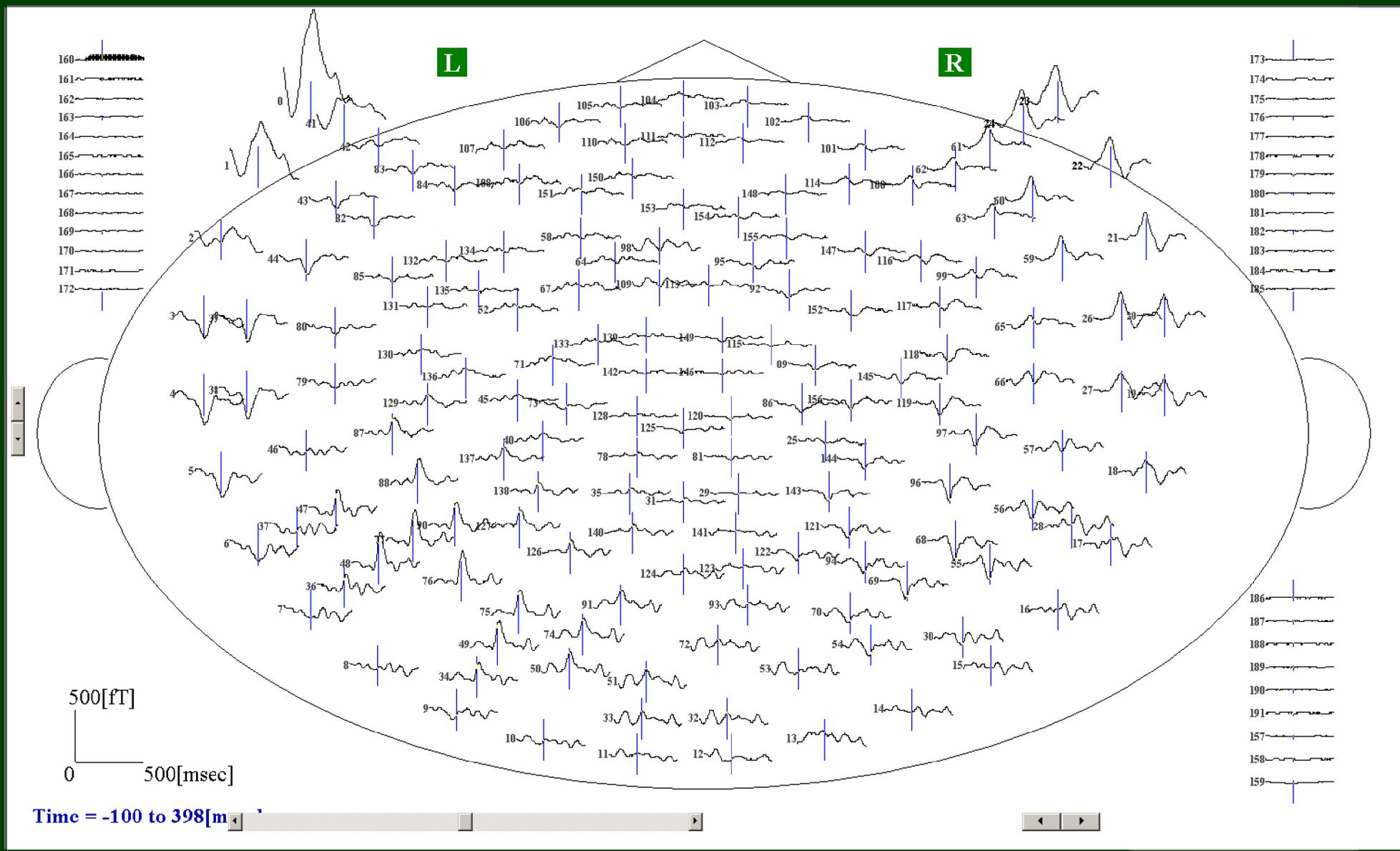


# MEG Response

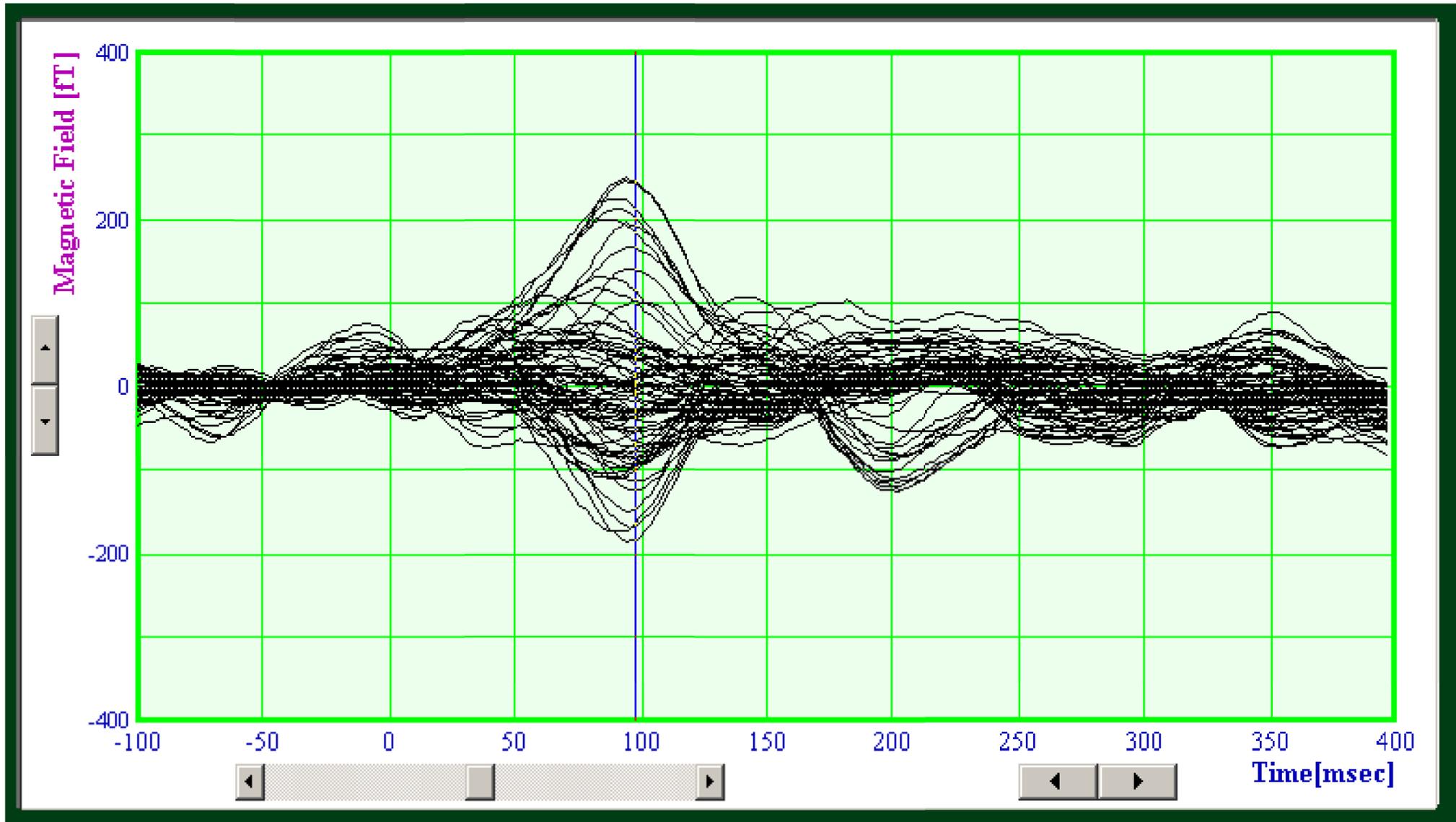
Time = 98.00[msec]

L

R

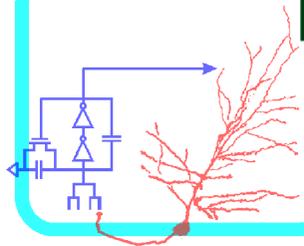
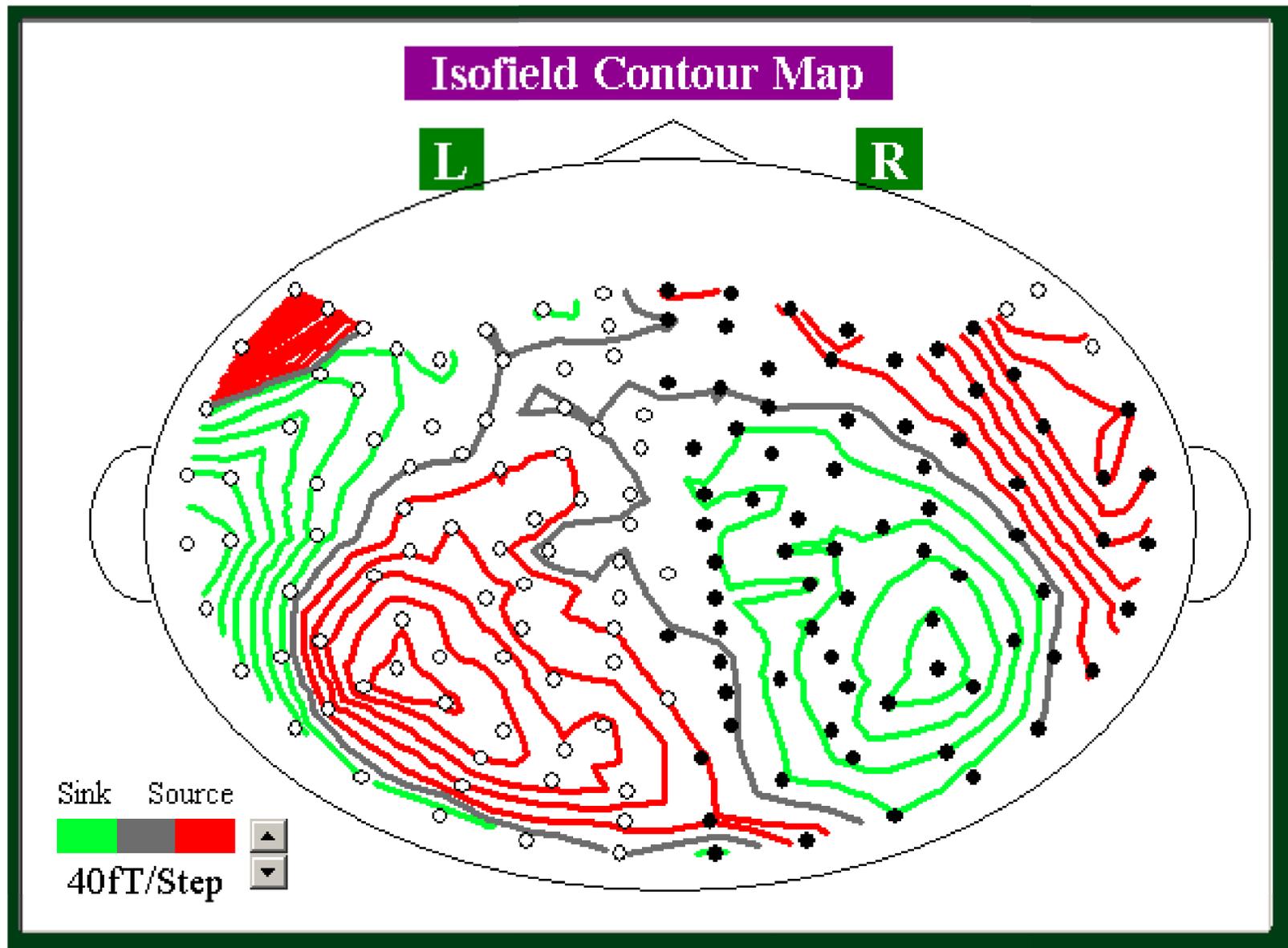


# MEG Response



**Time = 98.00[msec]**

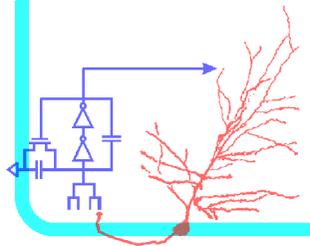
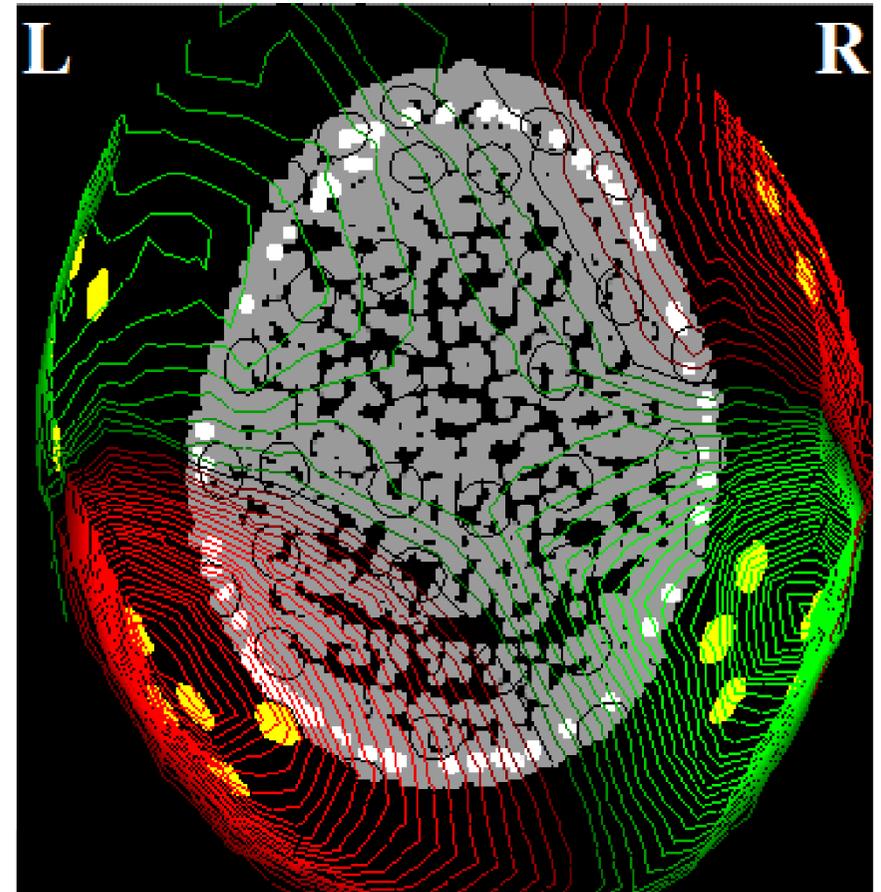
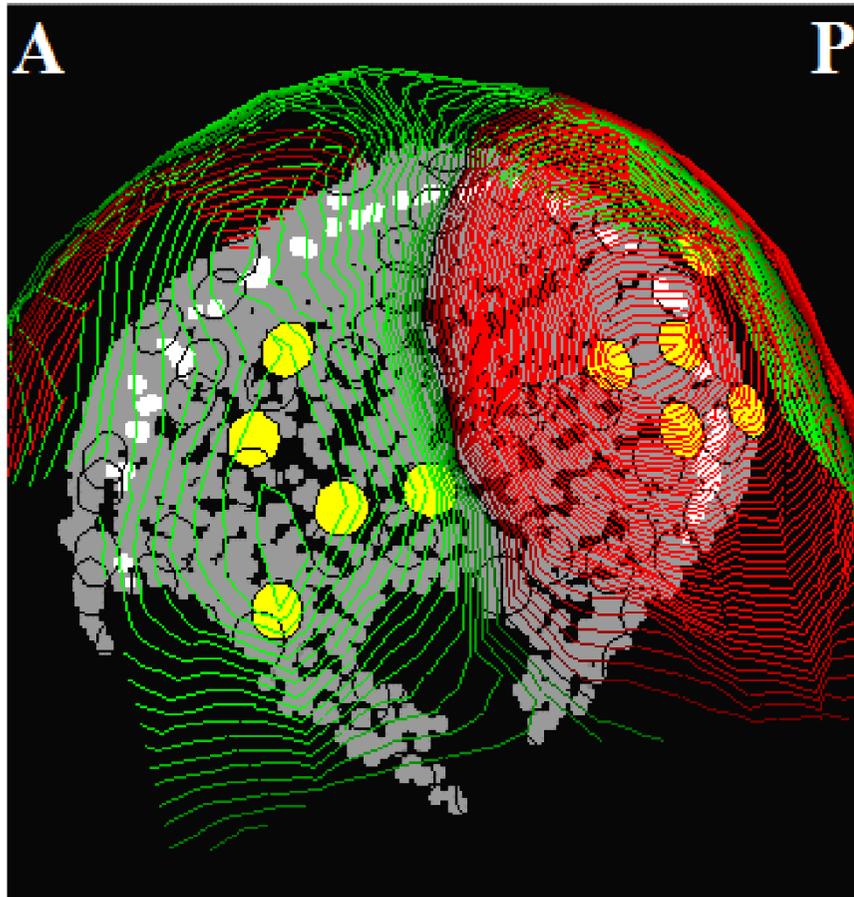
# MEG Response



# MEG Response

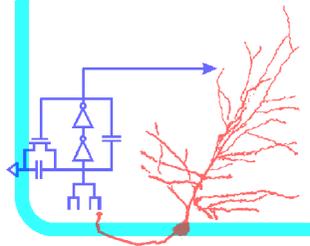
Sagittal View

Axial View



# Outline

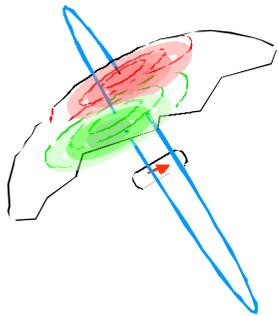
- The Brain and how it works
- The Auditory System
- Magnetoencephalography (MEG)
- Using MEG to explore the Auditory System



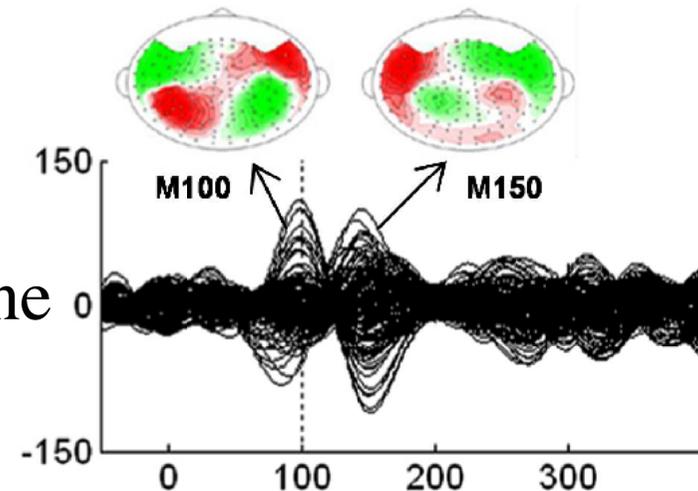
# Time Course of MEG Responses

## Evoked Responses

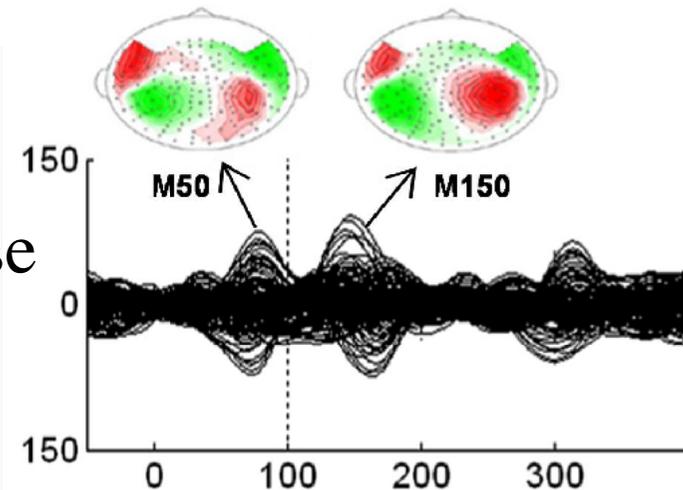
MEG Events Time-Locked to Stimulus Event



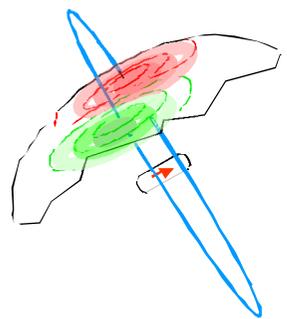
Pure Tone



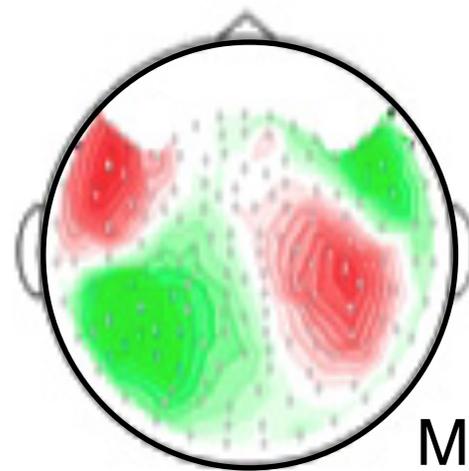
Broadband Noise



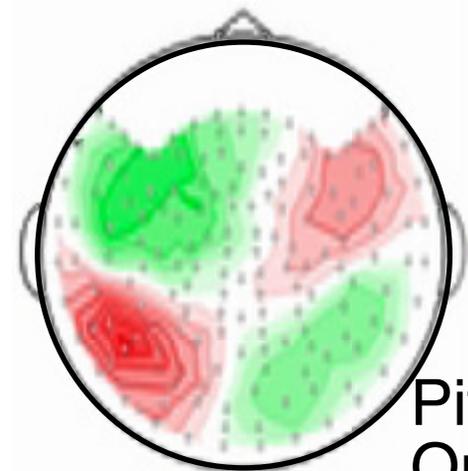
# Spatial Auditory MEG Responses



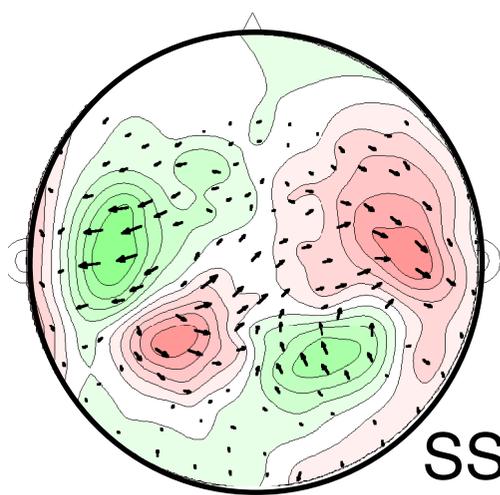
Auditory Responses  
*Robust*  
*Strongly Lateralized*



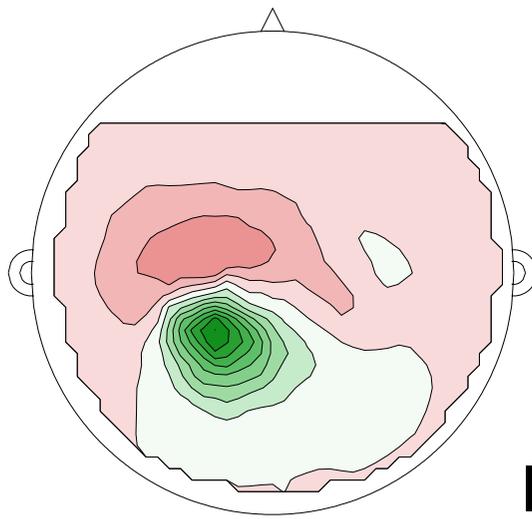
M50



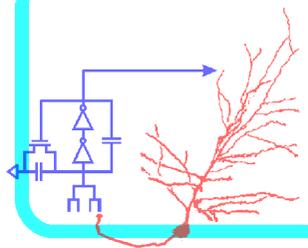
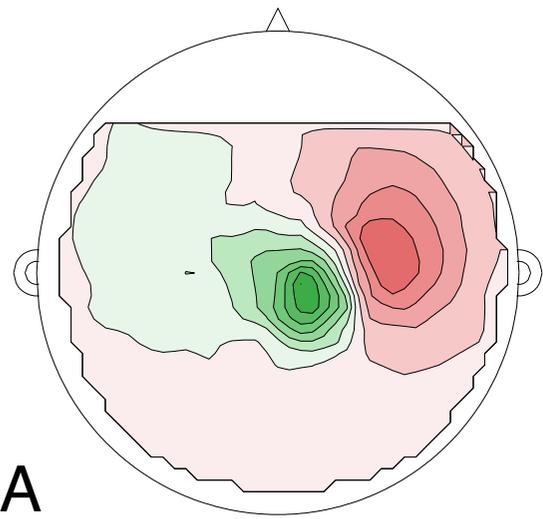
Pitch Onset



SSR



ICA



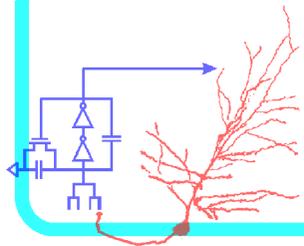
# An Alternative to Time: Frequency

- Use Stimuli localized in Frequency rather than time
- Examine Response at Same Frequency
- Well Established Method:

*Frequency Response* or *Transfer Function*

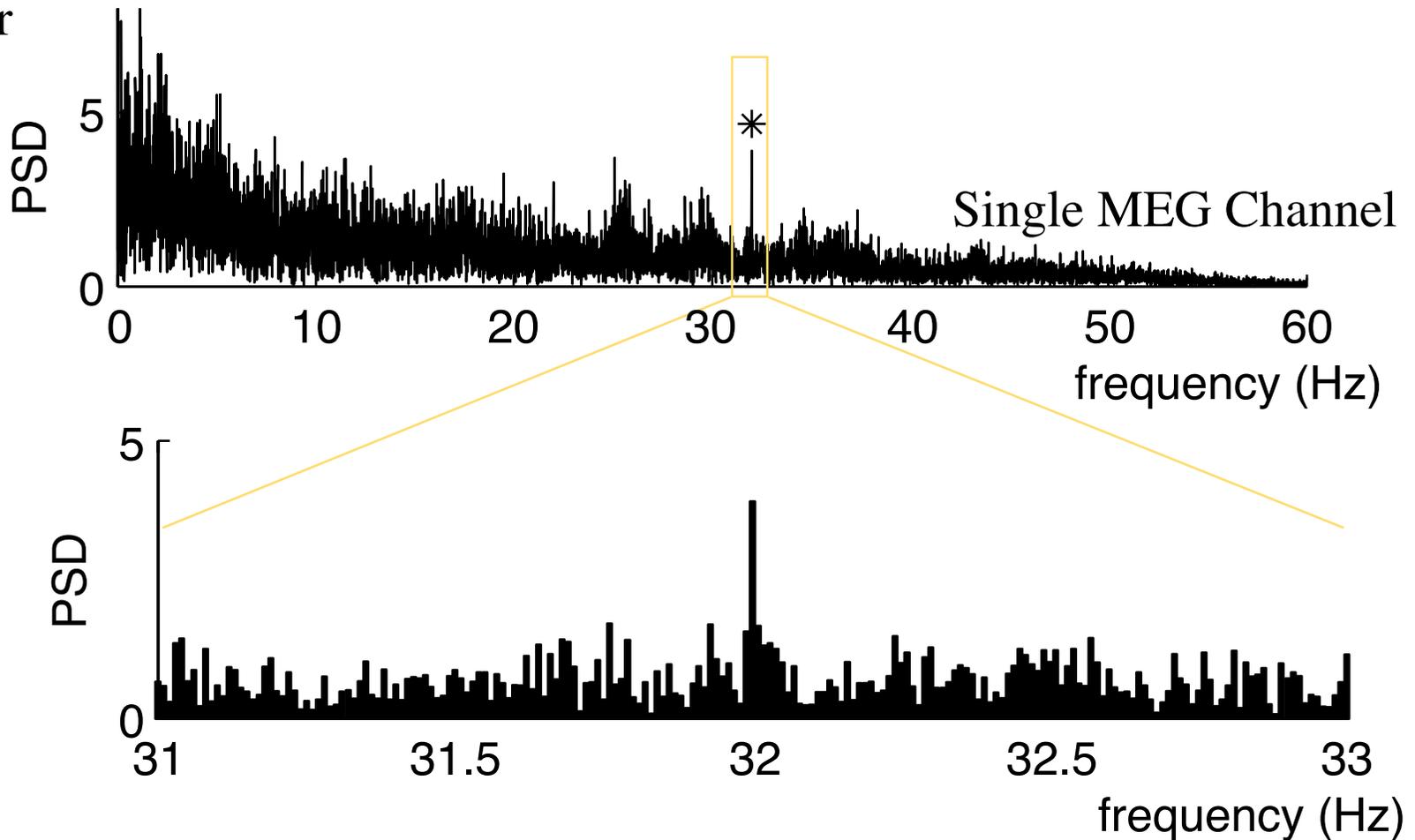
- Stimulus Modulated at Single Frequency:

*Steady State Response* (SSR)

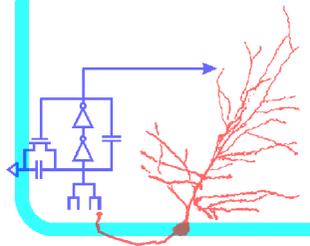


# Frequency Response

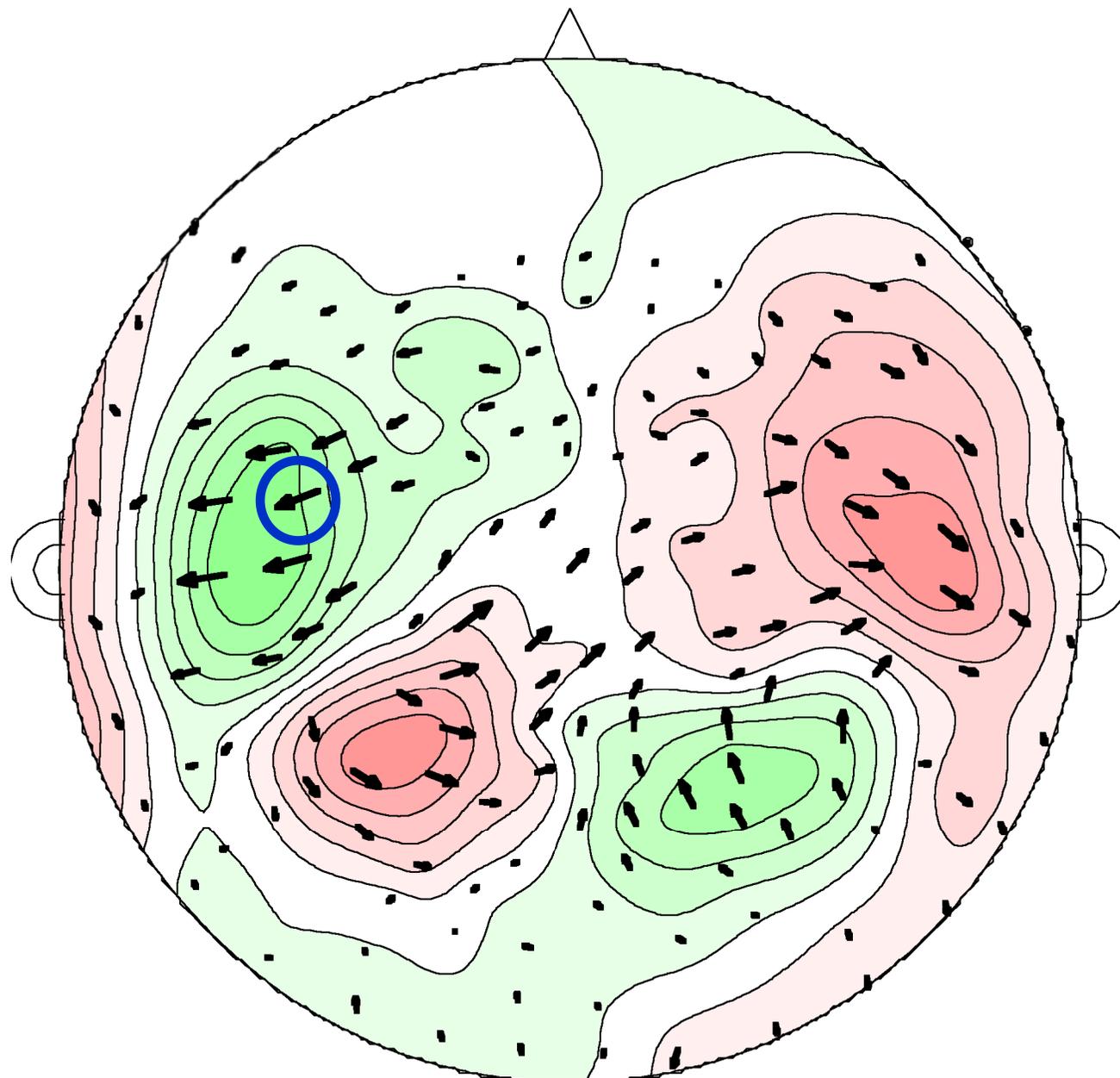
32 Hz Modulation  
400 Hz tone carrier  
100 trials @ 1 s  
(concatenated)



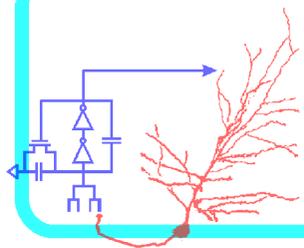
*Extremely* Precise Phase-Locking: 0.01 Hz  
No trial-to-trial jitter



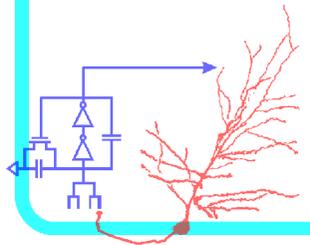
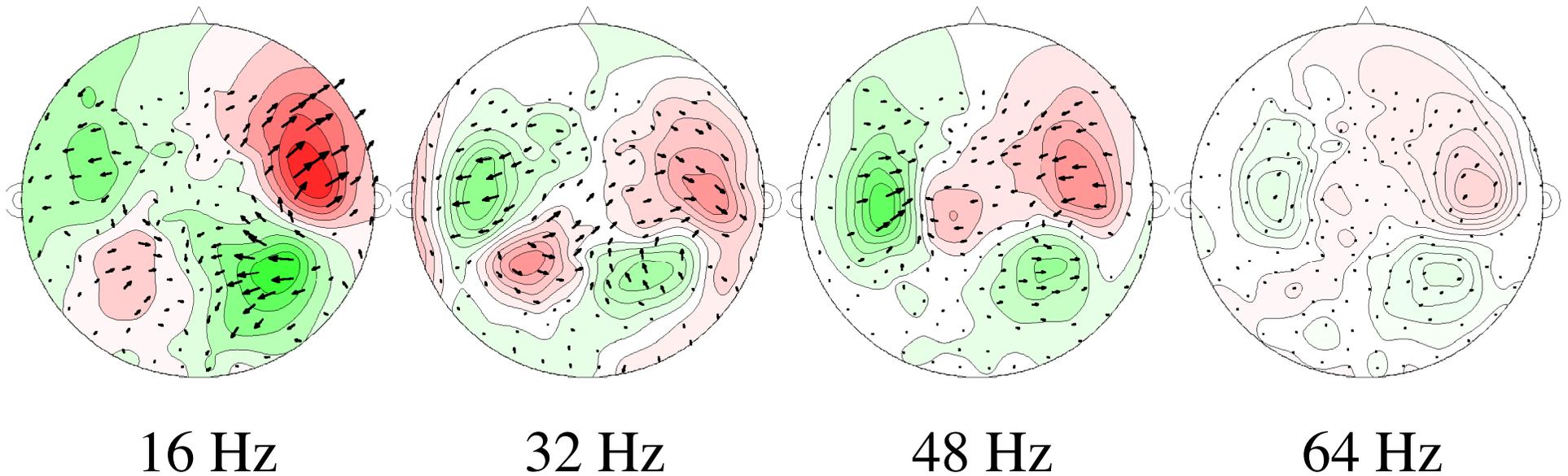
# Whole Head Steady State Response



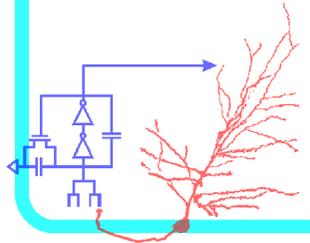
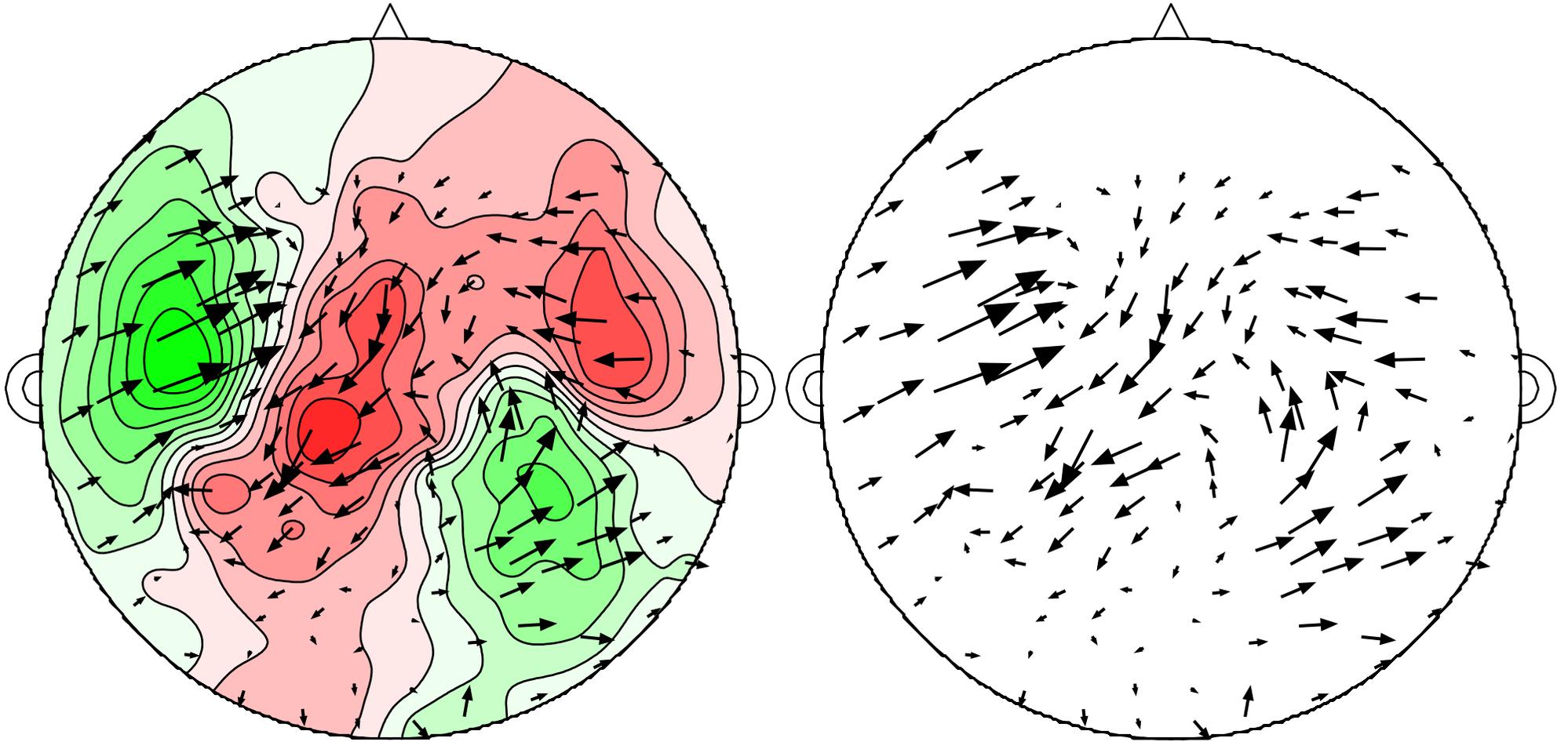
32 Hz



# Whole Head Transfer Function



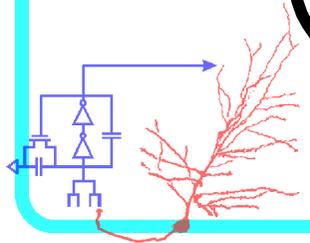
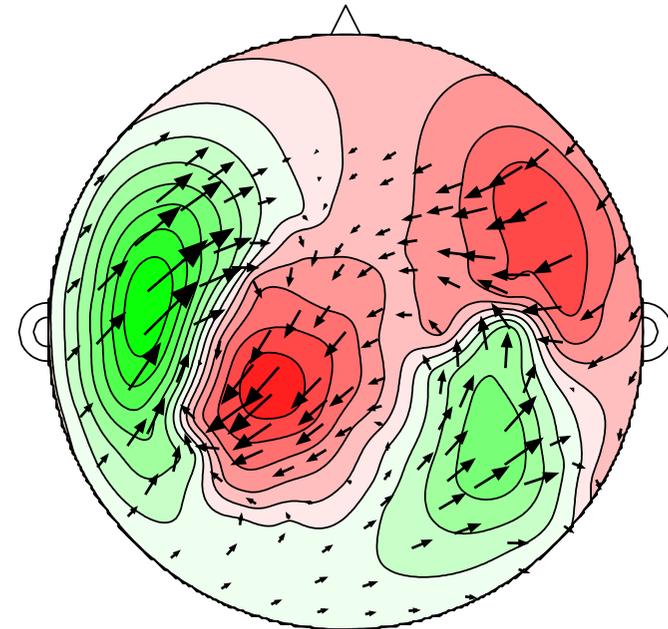
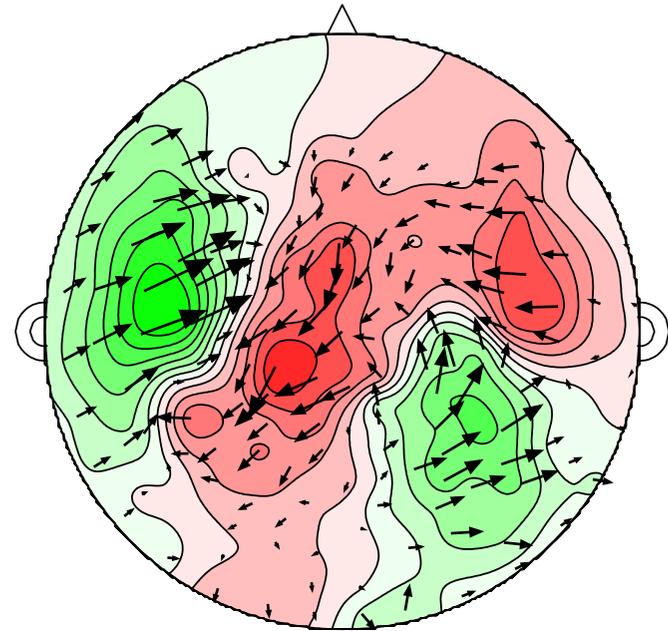
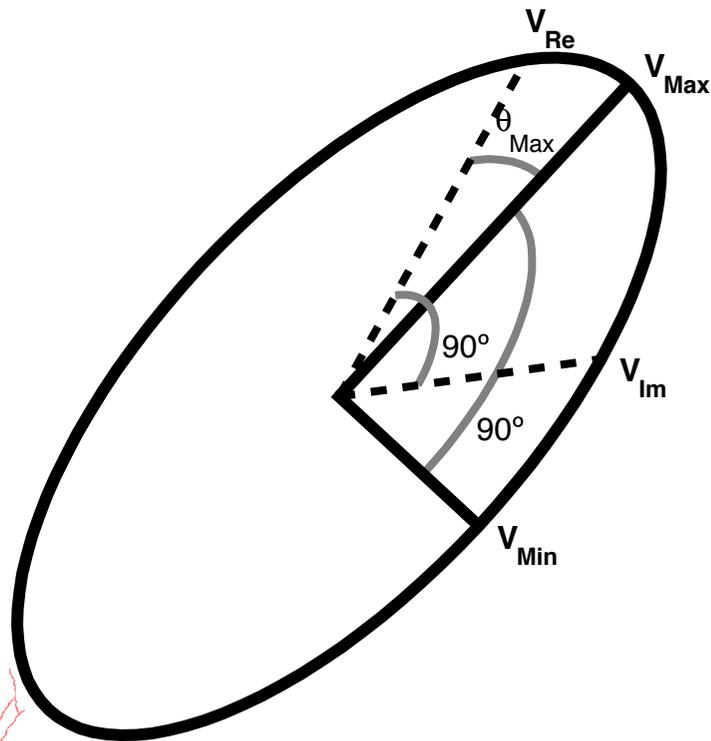
# Complex Magnetic Field



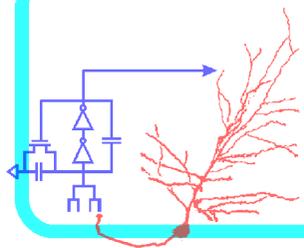
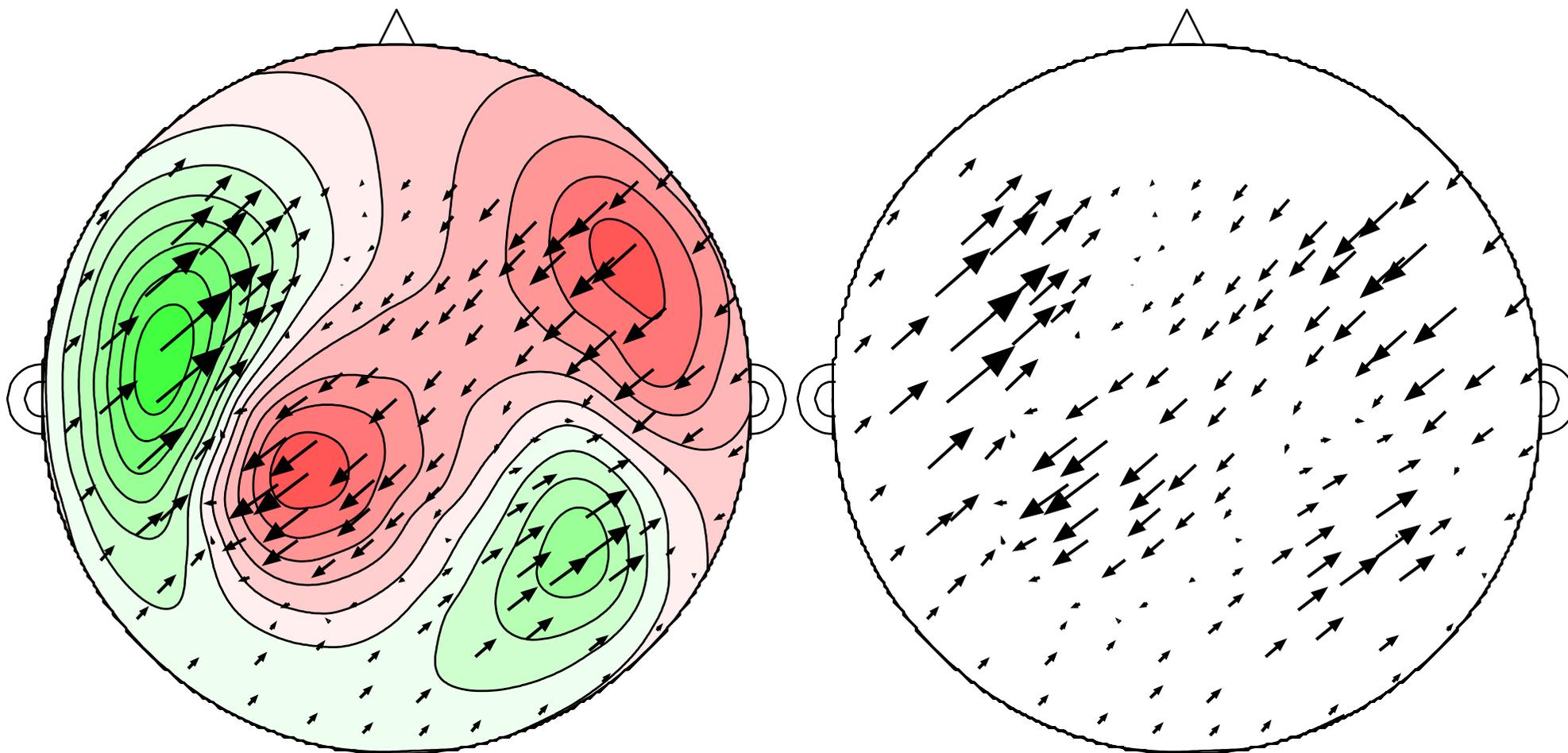
# Complex Neural Current Sources

$$\vec{V} = \vec{V}_{\text{Re}} + j\vec{V}_{\text{Im}}$$

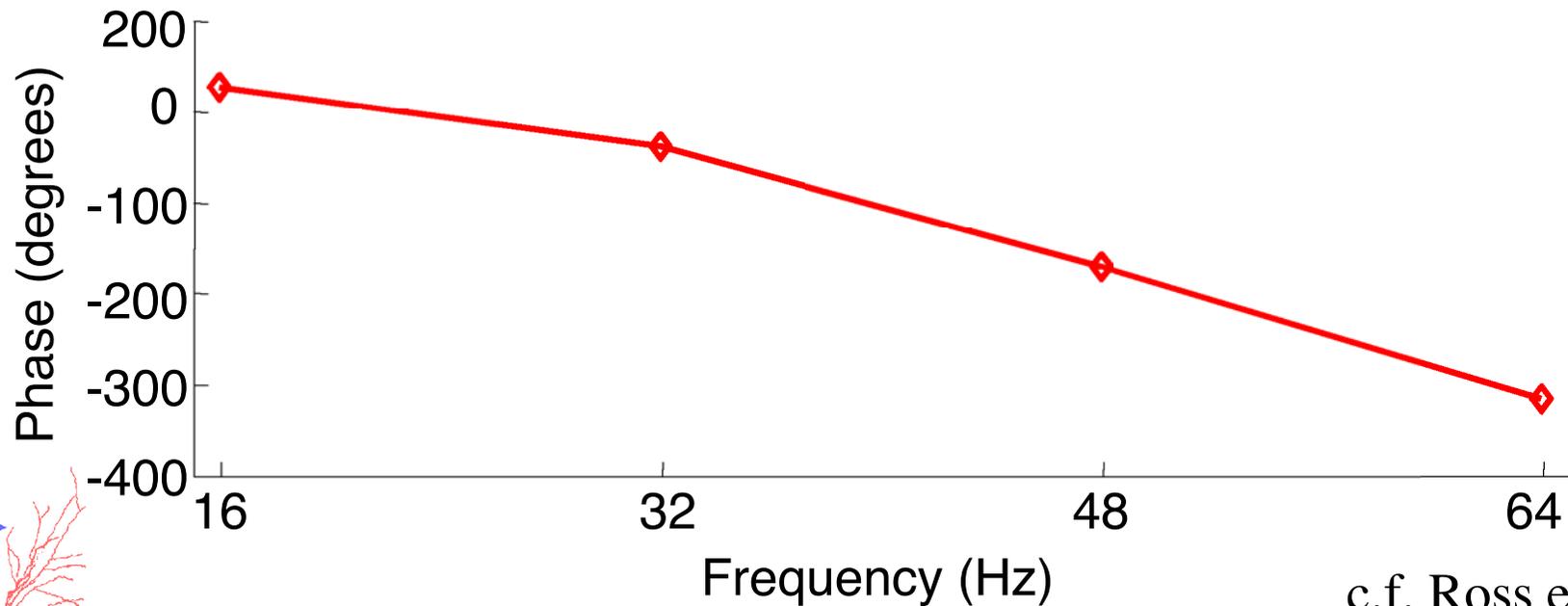
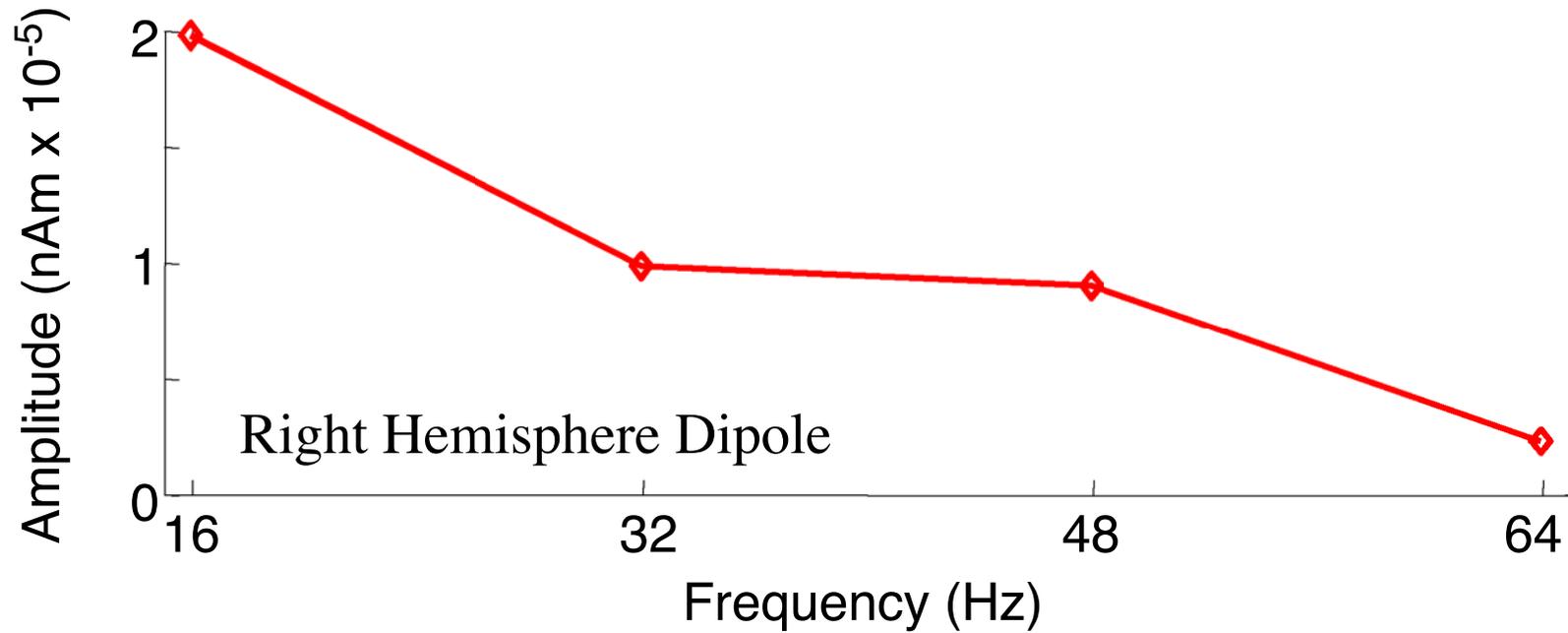
$$\vec{V}(\theta) = \vec{V}_{\text{Re}} \cos(\theta) + \vec{V}_{\text{Im}} \sin(\theta)$$



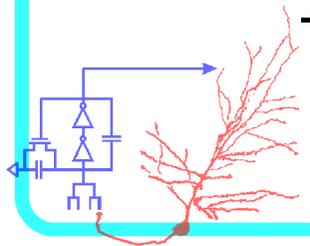
# Single Orientation Current Sources



# Neural Modulation Transfer Function

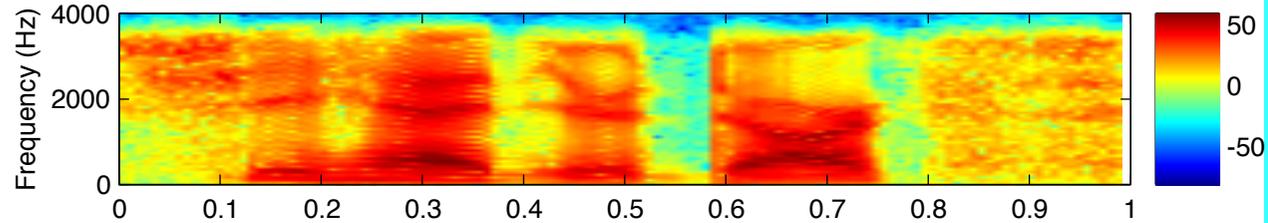


c.f. Ross et al. (2000)

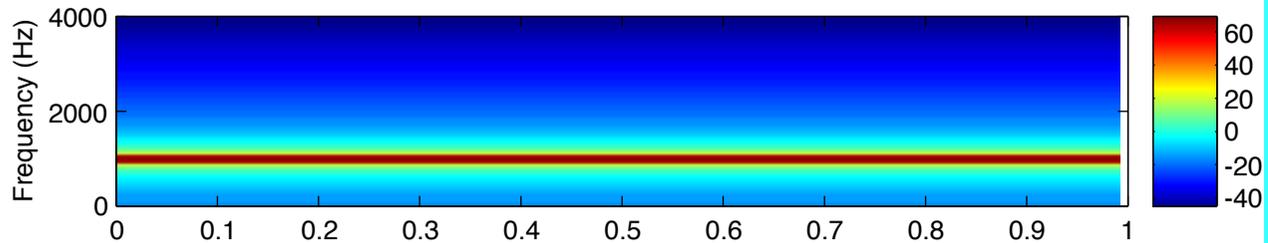


# The Dilemma of Complex Stimuli

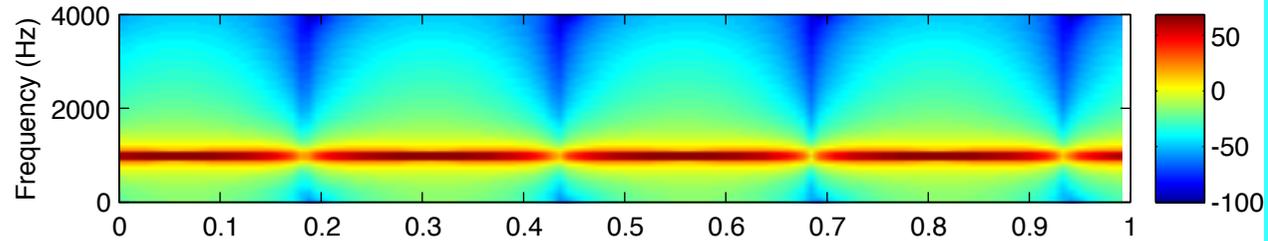
Speech



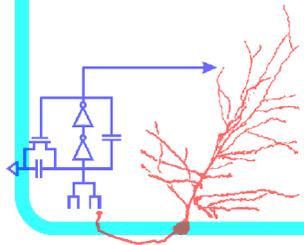
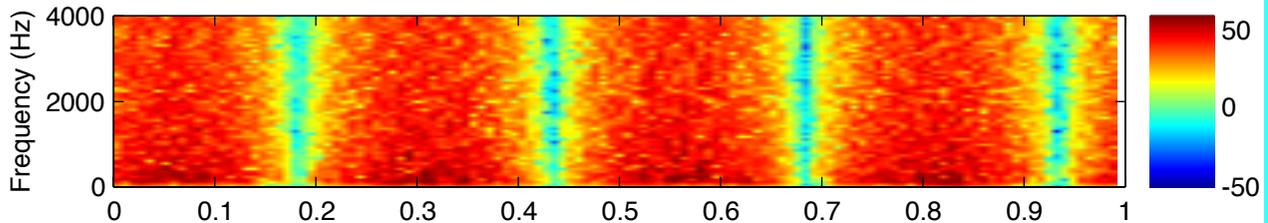
Pure Tone



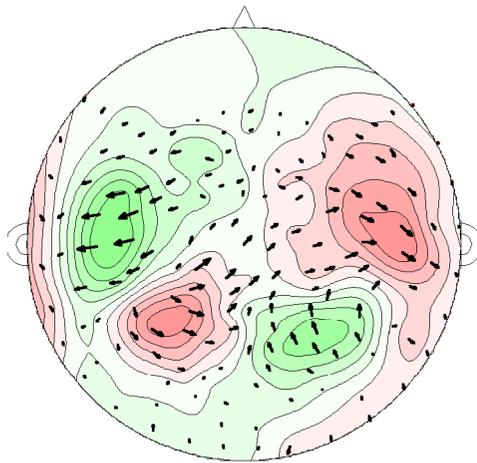
Modulated Pure Tone



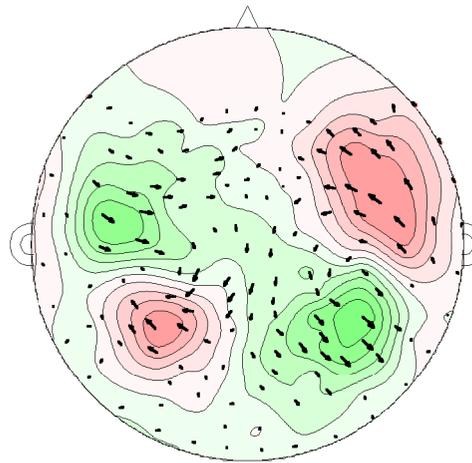
Modulated  
Broadband Noise



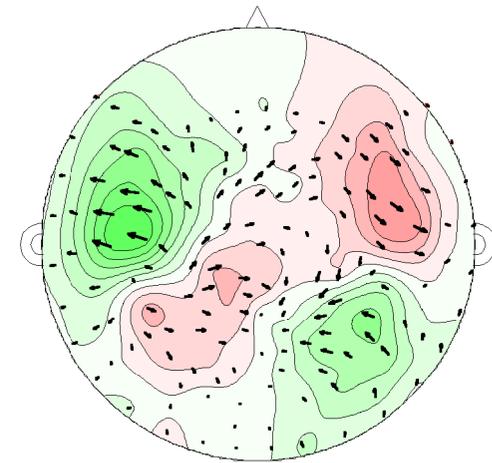
# SSR as Function of Bandwidth



Tone

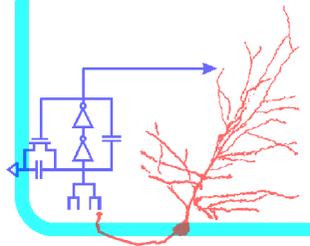


1/3 Octave Noise

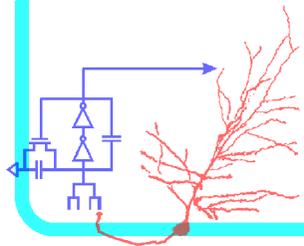
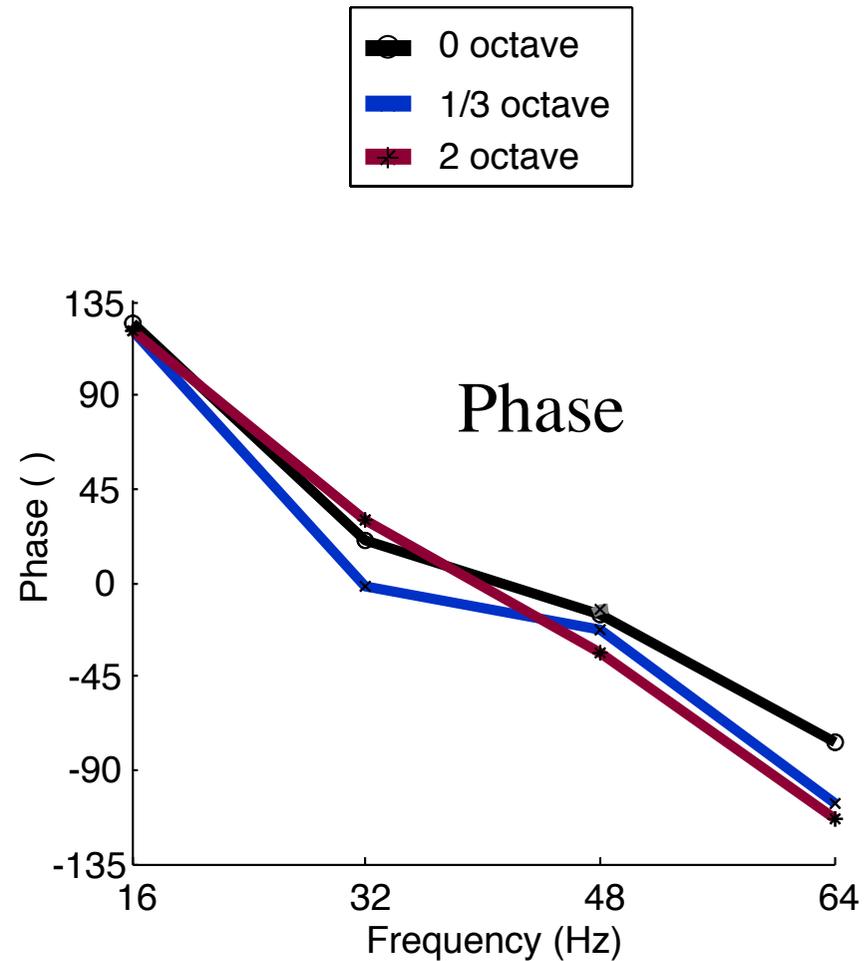
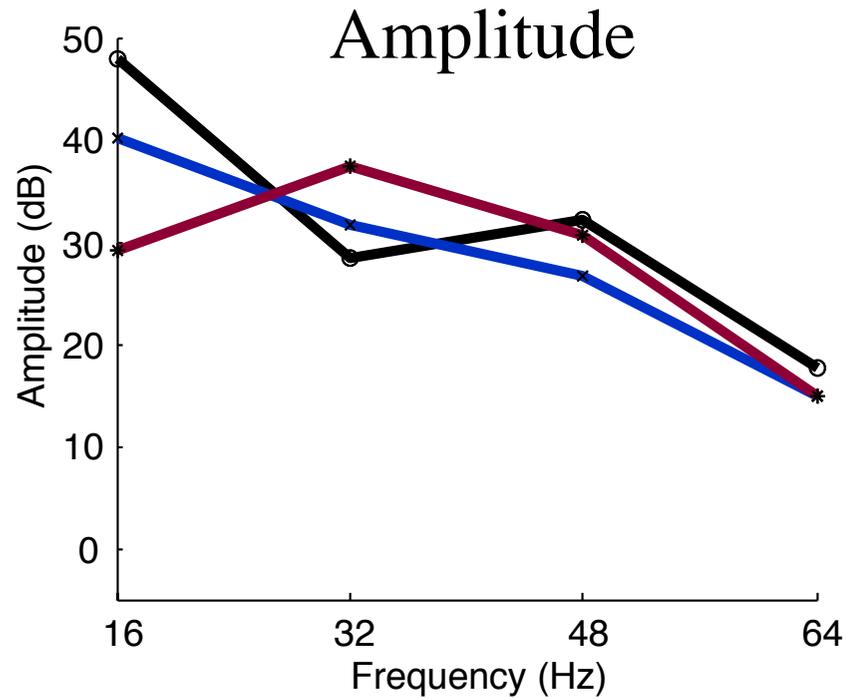


2 Octave Noise

32 Hz Modulation



# Multiple Transfer Functions



# Stimuli Revisited

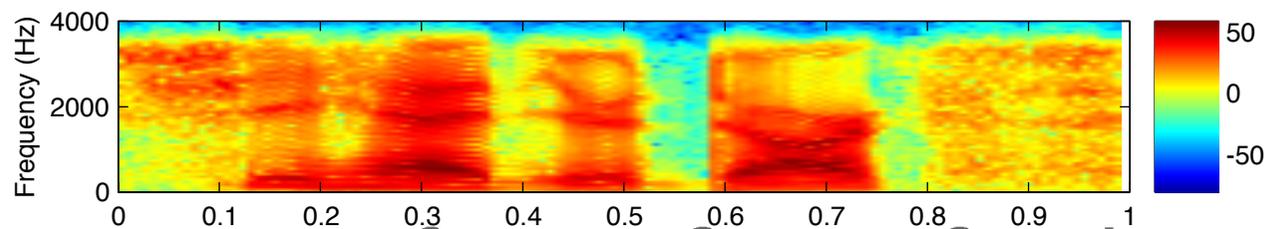
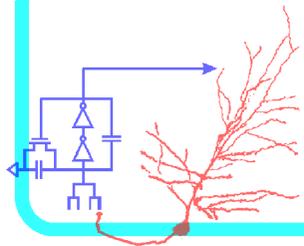
- Multiple Bandwidths: 0 to 5 octaves
- Low Modulation Frequencies: 2 to 32 Hz

Natural Sounds (e.g. speech)

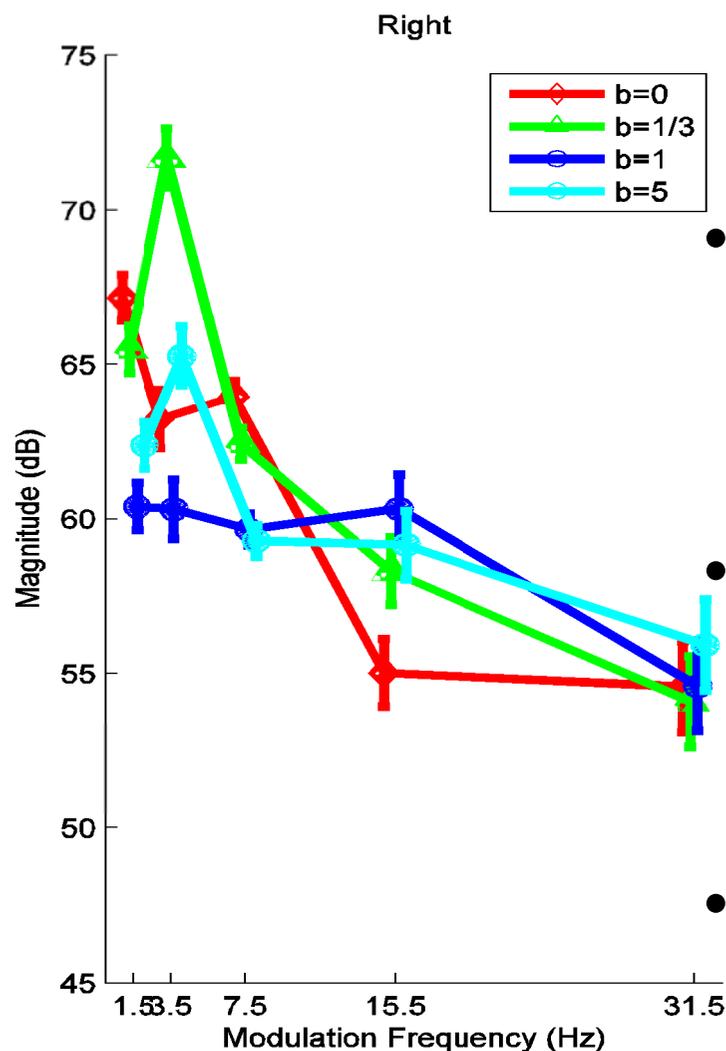
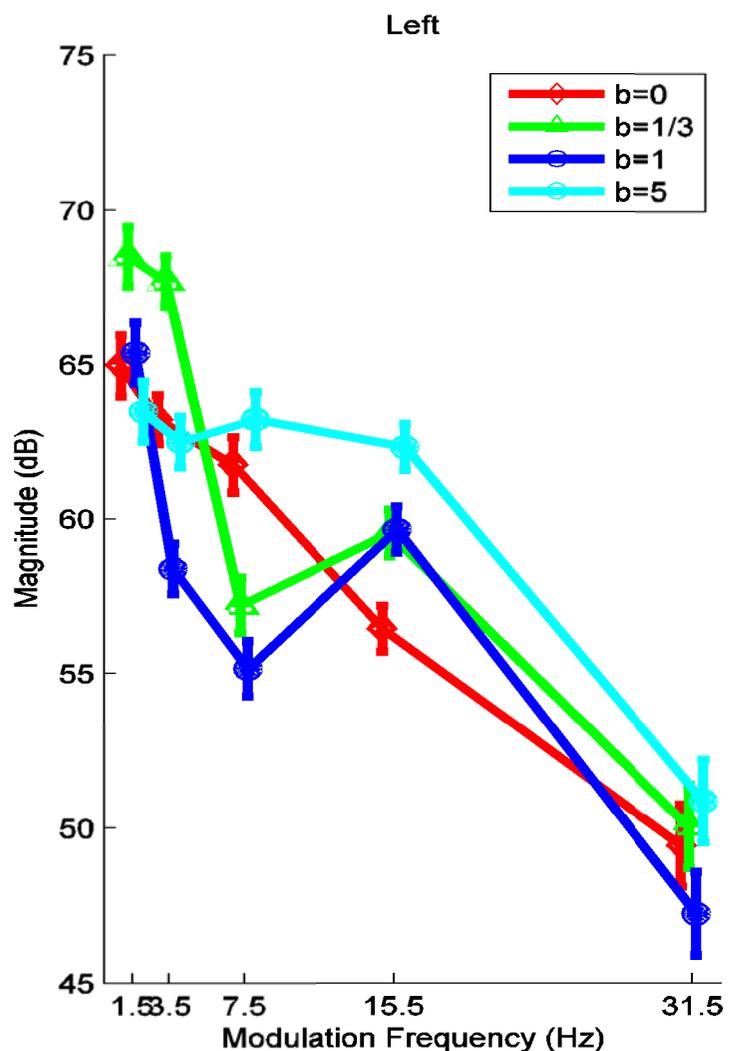
Intracranial Recordings from Human Auditory Cortex find peaks at 4-8 Hz in Liégeois-Chauvel et al. (2004).

- SSR vs. “Continuous Onsets”?

Evidence of significant ( $\sim 30\%$ ) linearity to *envelope of speech* from Ahissar et al. (2001).

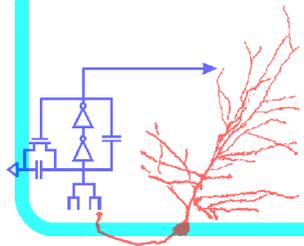


# Low Frequency Transfer Functions



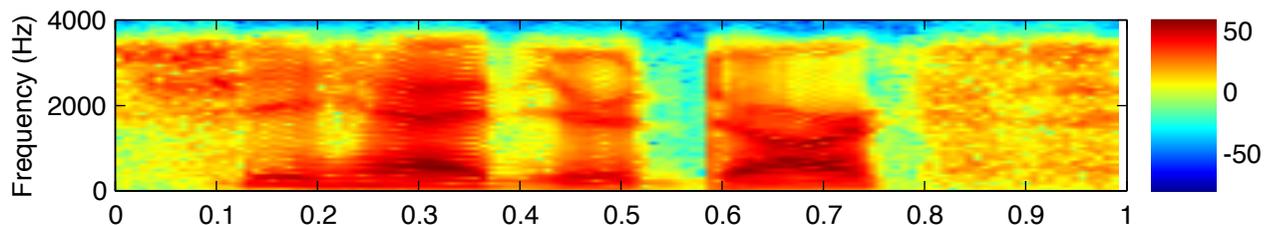
- Differences between Bandwidths Not Significant
- Increasing Response at Decreasing Frequencies
- Hemispheric Differences

12 Subjects

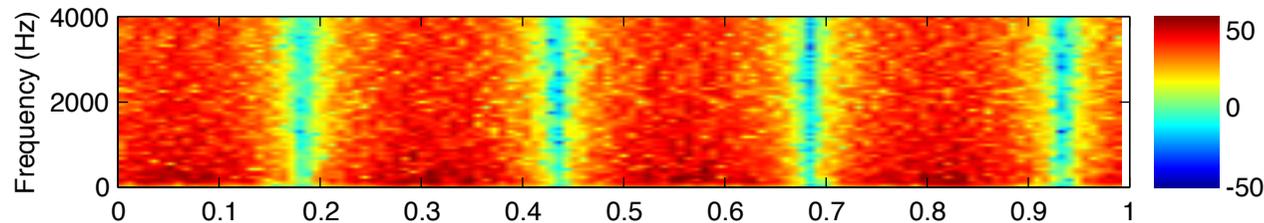


# Next on "To Do" List

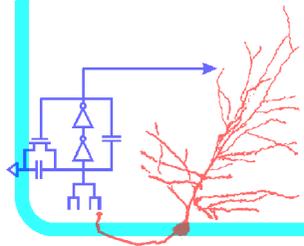
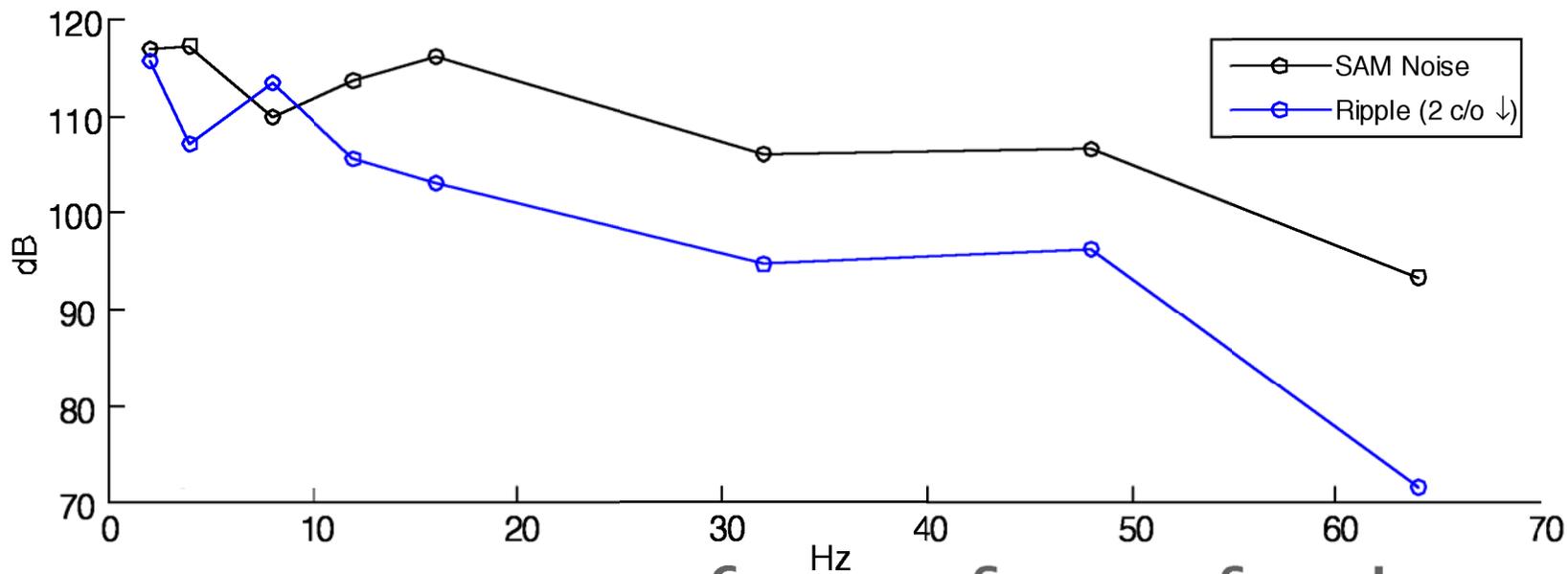
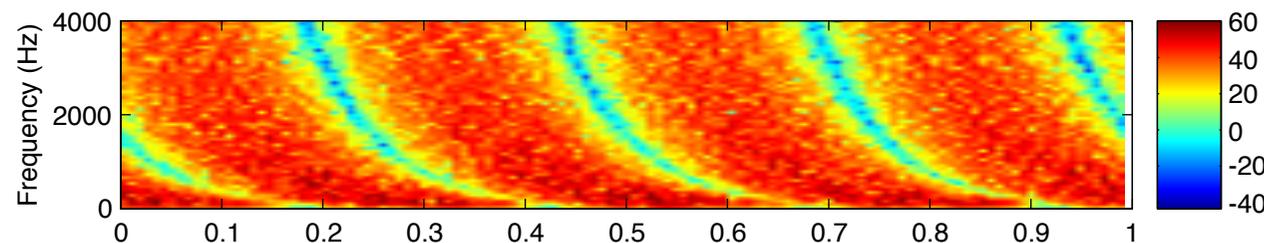
Speech



Modulated  
Broadband Noise

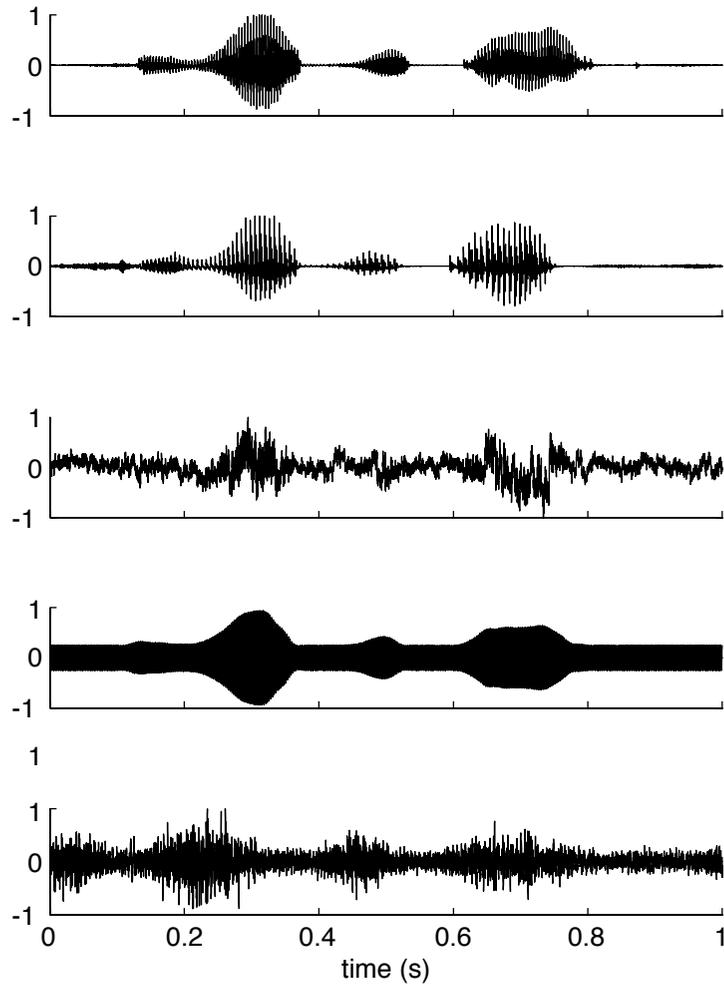


Auditory Ripple

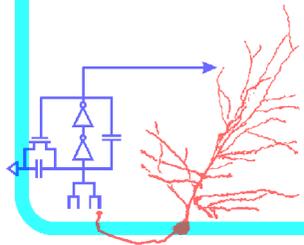
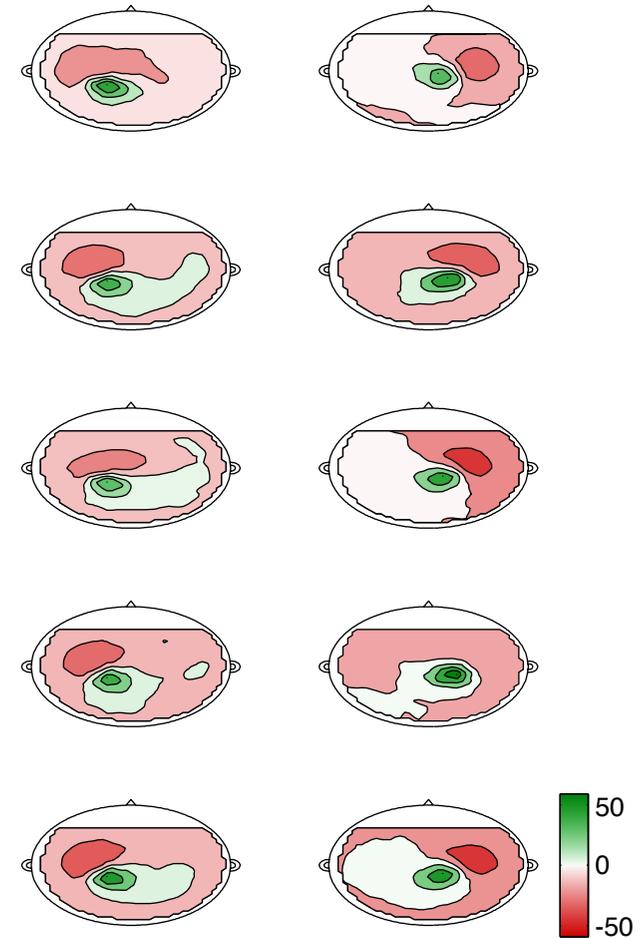


# Related Project: Speech + ICA

## Speech & Speech-like Stimuli

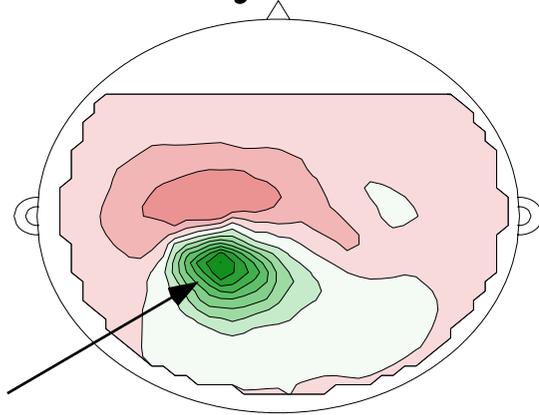


## Auditory Independent Component Responses

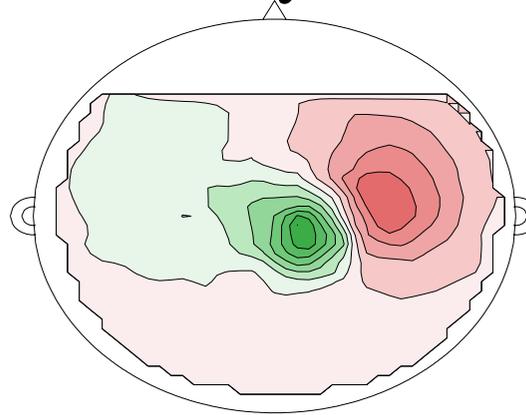


# Independent Component Analysis

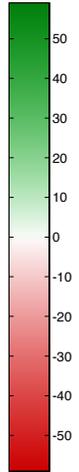
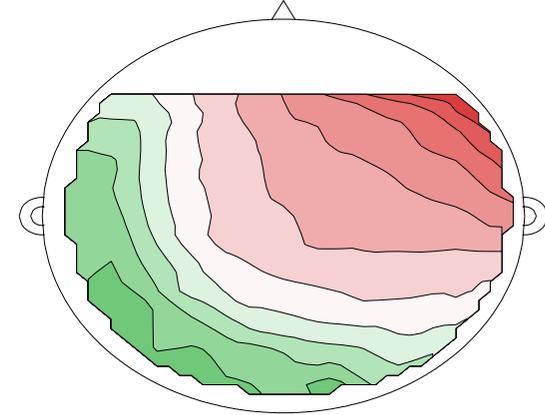
Left  
Auditory Cortex



Right  
Auditory Cortex

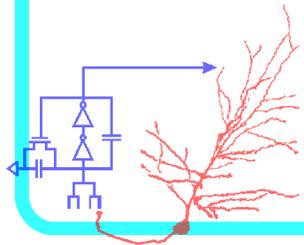
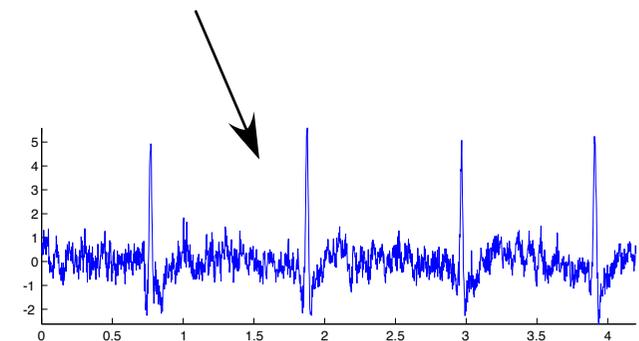
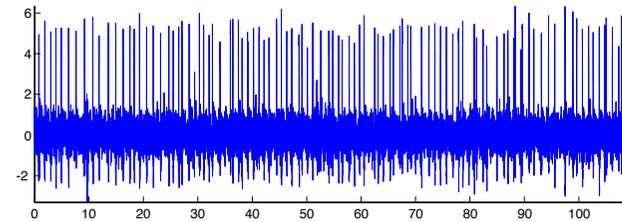


Heartbeat



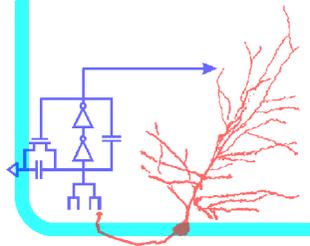
## ICA finds:

- Independent Neural Sources in *Auditory* areas
- Independent Neural Sources in *non-Auditory* areas
- Independent non-Neural Sources



# Summary

- Magnetoencephalography (MEG)
  - Directly generated by neural currents
  - Excellent time/frequency resolution
  - Spatial Localizability an open question
- Whole Head SSR
  - Spatial Phase Coherence
  - Complex Dipoles
  - Dipole Modulation Transfer Functions
  - Complementary to Time Based Methods  
(e.g. Speech with ICA)



*Thank You*