## Applications from Magnetoencephalography: Neural Detection of Attended Voices and Signal Enhancement

Jonathan Z. Simon

Institute for Systems Research

Department of Electrical & Computer Engineering

Department of Biology

University of Maryland

http://www.isr.umd.edu/Labs/CSSL/simonlab

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#### Neural processing of speech and complex auditory scenes

#### Magnetoencephalography







#### Neurally Inspired Algorithms





#### Advanced Neuroimaging



## Outline

- Magnetoencephalography (MEG)
  Brief introduction
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- Neural Detection of Attended Voices
- Signal Enhancement / Noise Reduction

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## Magnetoencephalography

- Non-invasive, Passive, Silent Neural Recordings
- Simultaneous Whole-Head Recording (~200 sensors)
- Sensitivity
  - high: ~100 fT (10<sup>-13</sup> Tesla)
  - low: ~10<sup>4</sup> ~10<sup>6</sup> neurons
- Temporal Resolution: ~I ms
- Spatial Resolution
  - coarse: ~ I cm
  - ambiguous



### Functional Brain Scanning

Hemodynamic techniques

#### Functional Brain Scanning

= Non-invasive recording from human brain

Electromagnetic techniques



**PET** positron emission tomography

> fMRI & MEG can capture effects in single subjects

**EEG** electroencephalography











Excellent Spatial Resolution (~1 mm)

Poor Temporal Resolution (~I s)

Limited Spatial Resolution (~1 cm)

Excellent Temporal Resolution (~1 ms)

### Functional Brain Scanning

Hemodynamic techniques

#### Functional Brain Scanning

= Non-invasive recording from human brain

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positron emission tomography

> fMRI & MEG can capture effects in single subjects

**EEG** electroencephalography











Excellent Spatial Resolution (~1 mm)

Poor Temporal Resolution (~I s)

Limited Spatial Resolution (~1 cm) Excellent Temporal Resolution (~1 ms)

#### Functional Brain Scanning



## Neural Signals & MEG





Photo by Fritz Goro

- •Direct electrophysiological measurement
  - •not hemodynamic
  - •real-time
- •No unique solution for distributed source
- •Measures spatially synchronized cortical activity
- •Fine temporal resolution (~ 1 ms)
- Moderate spatial resolution (~ 1 cm)

#### Magnetic Field Strengths 10-4 Earth's field 10<sup>-5</sup> 10<sup>-6</sup> Intensity of magnetic signal (T) 45 10-7 10<sup>-8</sup> Urban noise FVAT 10<sup>-9</sup> BRAIN (neurons) Contamination at lung EYE (retina) Spontaneous activity Steady activity Evoked by sensory stimulation Evoked activit 10<sup>-10</sup> أ قرة SPINAL COLUMN (neurons) Evoked by sensory stimulation LUNGS Heart ORS Magnetic contaminants HEART 10<sup>-11</sup> Cardiogram (muscle) Fetal heart LIVER $( \cdot )$ Timing signals (His Purkinje system) Iron stores Muscle GI TRACK 10<sup>-12</sup> Spontaneous signal ( $\alpha$ -wave) FETUS Cardiogram Stimulus response Magnetic contaminations Signal from retina 10<sup>-13</sup> LIMBS Steady ionic current MUSCLE **Evoked** signal Under tension 10<sup>-14</sup> **Biomagnetic Signals** Intrinsic noise of SQUID 10<sup>-15</sup>

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### MEG Auditory Field

#### Flattened Isofield Contour Map



## Time Course of MEG Responses

Pure Tone

#### Magnetic Field (fT) 120 M150 M100 -150 0 100 200 300 150 r M50 M150 Magnetic Field (fT) 150 0 100 200 300 ms time (ms)

#### **Broadband Noise**

#### **Auditory Evoked Responses**

- MEG Response Patterns Time-Locked to Stimulus Events
- Robust
- Strongly Lateralized



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### Phase-Locking in MEG to Slow Acoustic Modulations



MEG activity is precisely phase-locked to temporal modulations of sound

Ding & Simon, J Neurophysiol (2009) Wang et al., J Neurophysiol (2012)



# MEG Responses Predicted by STRF Model



## Neural Reconstruction of Speech Envelope



## Neural Reconstruction of Speech Envelope



Ding & Simon, J Neurophysiol (2012) Zion-Golumbic et al., Neuron (2013) Reconstruction accuracy comparable to single unit & ECoG recordings











# Unselective vs. Selective Neural Encoding





## Unselective vs. Selective Neural Encoding





![](_page_24_Picture_2.jpeg)

![](_page_24_Picture_3.jpeg)

![](_page_24_Picture_4.jpeg)

## Speech Reconstruction Results

![](_page_25_Figure_1.jpeg)

Identical Stimuli!

Ding & Simon, PNAS (2012)

## Single Trial Speech Reconstruction

![](_page_26_Figure_1.jpeg)

Ding & Simon, PNAS (2012)

## Single Trial Speech Reconstruction

![](_page_27_Figure_1.jpeg)

## Neural Detection of Attended Voice: Summary

- Can tell which voice a listener is attending to
- Can even track speech envelope of that voice
- Since attention can be manipulated (familiar vs. unfamiliar speaker, familiar vs. unfamiliar language, familiar vs. unfamiliar verbal content):

Access to familiarity of voice / speech content

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![](_page_30_Figure_1.jpeg)

![](_page_31_Figure_1.jpeg)

![](_page_32_Figure_1.jpeg)

![](_page_33_Figure_1.jpeg)

#### **External Noise**

![](_page_34_Picture_1.jpeg)

![](_page_34_Picture_2.jpeg)

#### External Noise

Can be estimated using Reference Channels

![](_page_35_Picture_2.jpeg)

#### External Noise Removal: I

#### c.f. Classic Scalar Regression

![](_page_36_Figure_2.jpeg)

#### External Noise Removal: I

#### c.f. Classic Scalar Regression

![](_page_37_Figure_2.jpeg)

But scalar regression fails when:

Noise Reference is *filtered* with respect to Noisy channel Noise Reference is *time-shifted* with respect to Noisy channel More independent Noise sources than Reference channels

#### Time-Shift Principle Component Analysis

![](_page_38_Figure_2.jpeg)

Generalizes Scalar Regression:

Include Multiple Time-Shifted versions of References Linear Combinations (PCA) of Time-Shifts are Filters Increases effective number of References

Signal cleaned using TSPCA and 3 Reference channels

![](_page_39_Figure_2.jpeg)

Signal cleaned using TSPCA and 3 Reference channels

![](_page_40_Figure_2.jpeg)

Signal cleaned using TSPCA and 3 Reference channels

![](_page_41_Figure_2.jpeg)

Signal cleaned using TSPCA and 3 Reference channels

![](_page_42_Figure_2.jpeg)

#### **TSPCA** Summary

- TSPCA removes ~98% of noise power
- SNR increase > 10 dB at noisiest frequencies

![](_page_43_Figure_3.jpeg)

SNR<sub>E</sub>: ratio of Signal other than Environmental Noise to Environmental Noise

### **TSPCA** Summary

- TSPCA removes ~98% of noise power
- SNR increase > 10 dB at noisiest frequencies

![](_page_44_Figure_3.jpeg)

- No Target Distortion: only Reference channels are filtered
- Tested on wide range of systems
- User Friendly: Single Parameter to be chosen in advance:
  N = (# of taps), not algorithm sensitive
- Caveats: For small duration signals, N cannot be to large Processing time  $O(N^2)$

#### Sensor Noise

![](_page_45_Figure_1.jpeg)

#### Sensor Noise Reduction: SNS

Sensor Noise Suppression

Targets Sensor Noise, including: Transducer Noise (e.g., SQUID) Electronics Noise (e.g., FLL, amplifier)

## SNS Methodology

![](_page_47_Picture_1.jpeg)

Assumption: Every neural source is picked up by multiple sensors

Consequence: Any component observed on only one sensor is **artifactual**.

Requires spatially dense sensors

Otherwise model-free

#### SNS Example

#### "Glitch" Removal

![](_page_48_Figure_2.jpeg)

#### SNS Example Power and PCA Spectra

![](_page_49_Figure_1.jpeg)

sensor-specific signal dimensions

### SNS Summary

- Removes Sensor Noise Glitches
- Esp. high frequency noise
- No Target Distortion (unless target loads only I sensor)
- Allows:

Cleaner Data More usable epochs (no need to discard glitches) Reduction of spurious dimensionality (e.g., for PCA, ICA)

## Strongly-Mixed-Noise Reduction

Neural Signal-of-Interest vs. Neural Noise

- Neural sources of Signal-of-Interest may overlap with Neural Noise
- Time courses of Signal-of-Interest may correlate with Neural Noise
- But still separable if there exists a Stimulus-Based Criterion to distinguish between them

## Strongly-Mixed-Noise Reduction: DSS

**Denoising Source Separation** 

- Algorithm creates Spatial Filters based Stimulus-Based separation criterion (generates Separated Components)
- Neural sources of Signal-of-Interest must be spatially distinct from Neural Noise (overlap OK)
- Time courses of Signal-of-Interest must be distinguishable from Neural Noise (correlation OK)

Särelä and Valpola, J. Mach. Learn. Res. (2005) de Cheveigné and Simon, J. Neurosci. Methods (2008b)

#### **DSS** Example

Spectra of MEG Steady State Response (to dual modulation)

Before DSS (20 Best Channels) First DSS component

![](_page_53_Figure_4.jpeg)

![](_page_53_Figure_5.jpeg)

### DSS Example

Phase coding parameter  $\alpha$  (by subject)

![](_page_54_Picture_2.jpeg)

Before DSS (20 Best Channels)

First DSS component

#### **DSS Example**

![](_page_55_Figure_1.jpeg)

### DSS: How it Helps

"Select best components, discard others"

![](_page_56_Figure_2.jpeg)

## DSS Summary

- Removes Noise deeply mixed with Signal
- Complementary with:
  - Other denoising algorithms (TSPCA, SNS)
  - Standard analysis tools (beamforming, dipole source analysis, etc.)
- Flexible: case-dependent bias criteria can be used: Bandpassed evoked response (e.g. theta, gamma) Any stimulus-dependent representation of response
- Caveats:

Bias should be robust, so temporarily remove outliers (e.g. ~20% of trials), but OK to use in end

• When SNR is poor (weaker evoked response), may fail, or give component-of-interest as 2nd component.

## Denoising Summary

- Different noise sources are best removed using different methods
- Each denoising step decreases dimensionality of signal space, increasing the power of the next step
- TSPCA: Removes External noise represented (imperfectly) in Reference Channels (user friendly)
- SNS: Removes Sensor noise uncorrelated with other channels (user friendly)
- DSS: Removes more "entrenched" noise (tunable)

## Summary

- Magnetoencephalography: powerful, sensitive
- Sensitivity allows neural tracking of speech, attended vs. unattended, and all it entails
- Sensitivity includes sensitivity to noise, which must then be removed.
  - Powerful Noise Removal techniques

### Thank You

## Comparison with EEG

- High temporal resolution
- Inexpensive, Room temperature
- Slow, careful set-up
- Electric fields strongly distorted

![](_page_61_Picture_5.jpeg)

- Brain = inhomogeneous, anisotropic, dielectric
- Poor spatial neural reconstruction unless very carefully modeling of currents and entire head
- Inverse problem: worse? better?
- Many more neural sources
- Complementary with MEG