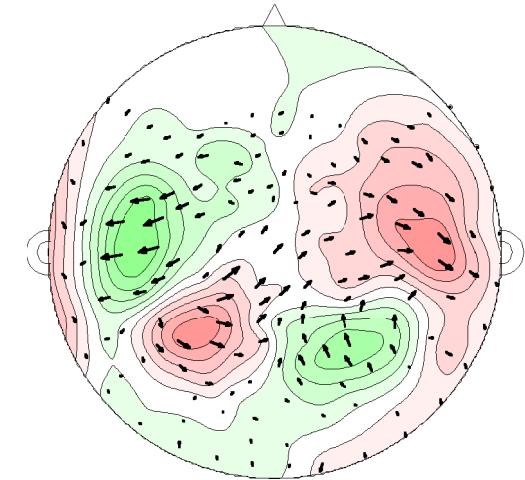


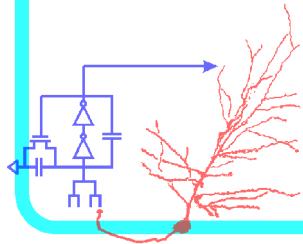
Neural Coding of Multiple Stimulus Features in Auditory Cortex



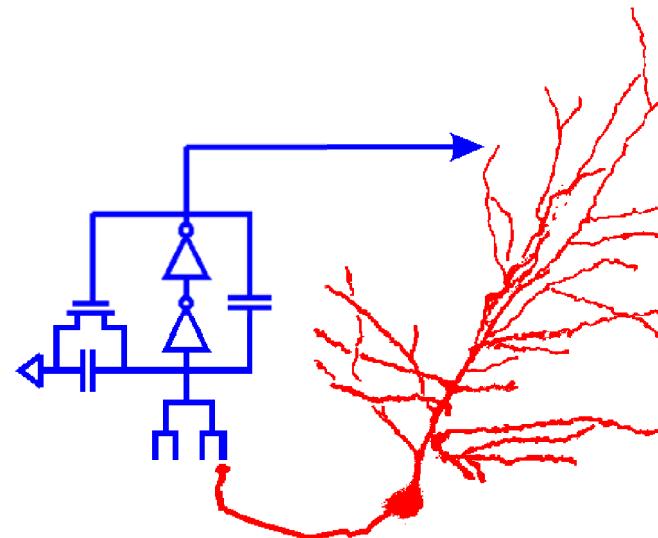
Jonathan Z. Simon

Neuroscience and Cognitive Sciences
Biology / Electrical & Computer Engineering

University of Maryland, College Park



Computational Sensorimotor Systems Laboratory



Huan Luo

Maria Chait

Juanjuan Xiang

Nayef Ahmar

Yadong Wang

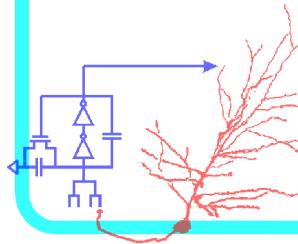
David Poeppel

Shihab Shamma

Catherine Carr

Cindy Moss

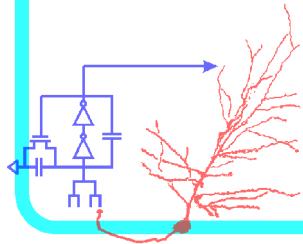
Timothy Horiuchi



Luo, H., Y. Wang, D. Poeppel & J. Z. Simon (2006), J. Neurophysiology

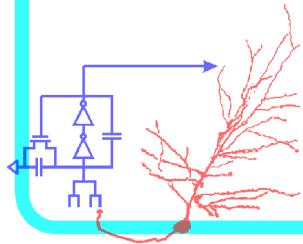
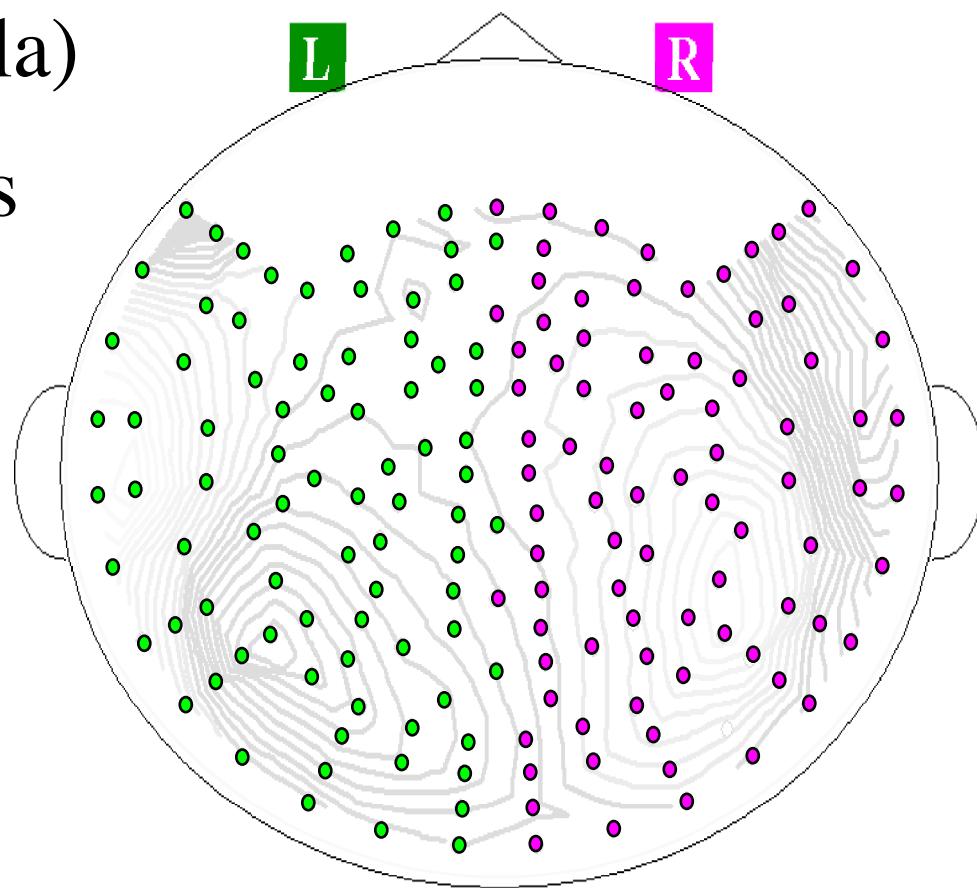
Introduction

- Magnetoencephalography (MEG) as a tool of Non-Invasive Auditory Physiology
- Neural Encoding of Simple Modulations
- Neural Encoding of Independent Modulation Pairs (AM & FM)



Magnetoencephalography (MEG)

- Non-invasive, Passive, Silent
- Simultaneous Whole-Head Recording (~200 sensors)
- Sensitivity
 - high: ~ 100 fT (10^{-13} Tesla)
 - low: $\sim 10^4 - \sim 10^6$ neurons
- Temporal Resolution: ~ 1 ms
- Spatial Resolution
 - coarse: ~ 1 cm
 - ambiguous



Neural Activity = Neural Current

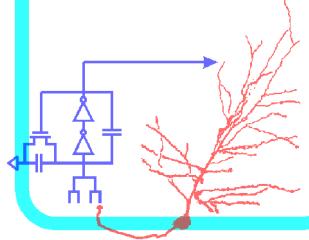
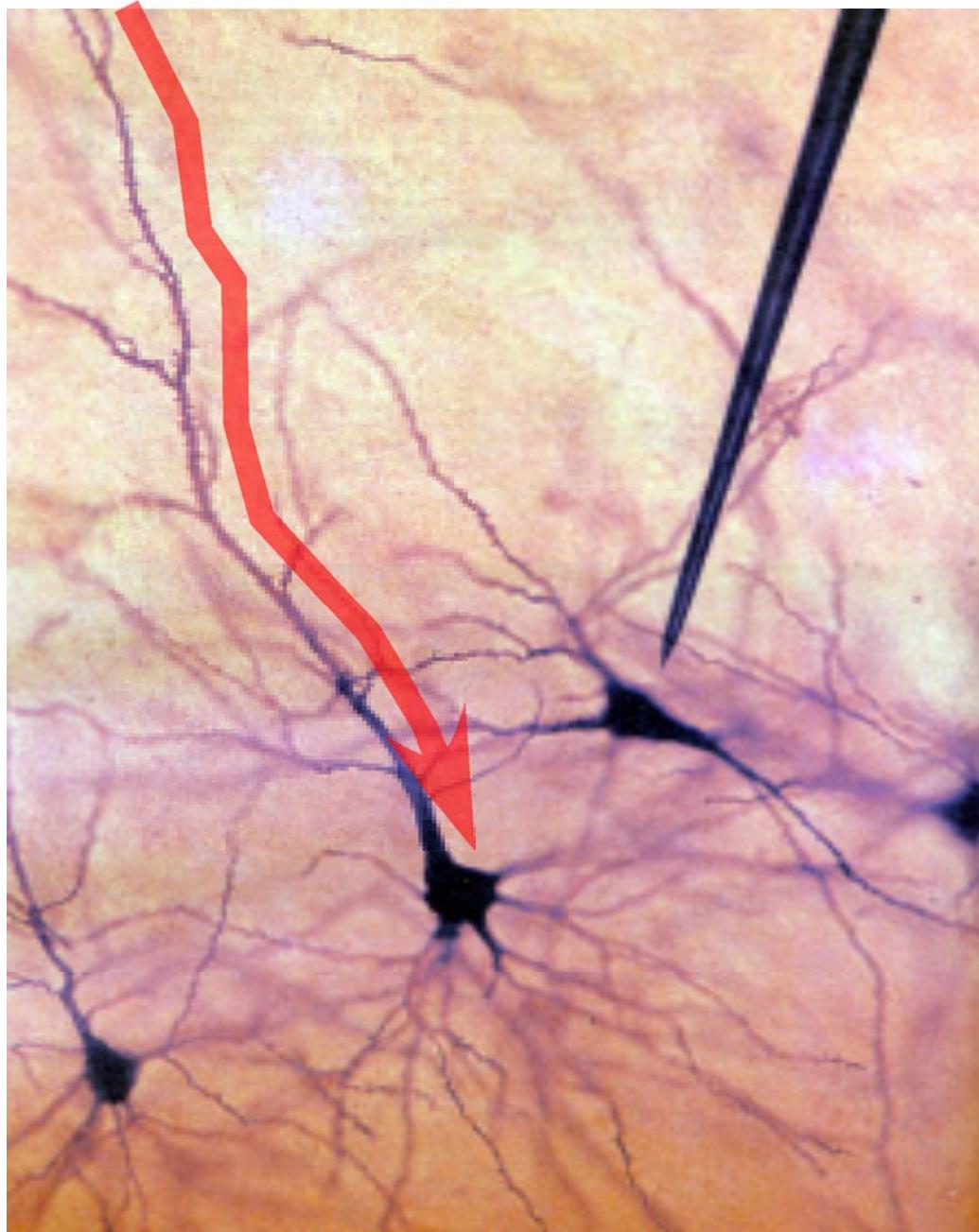
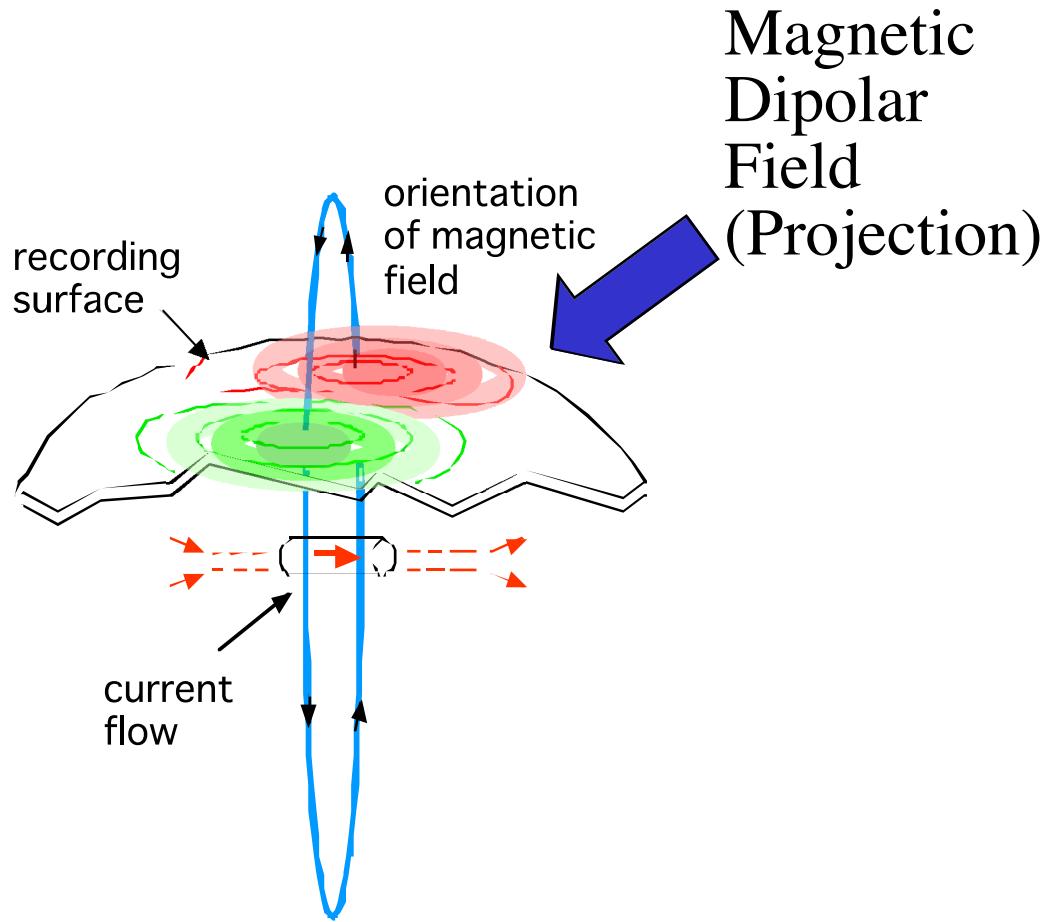
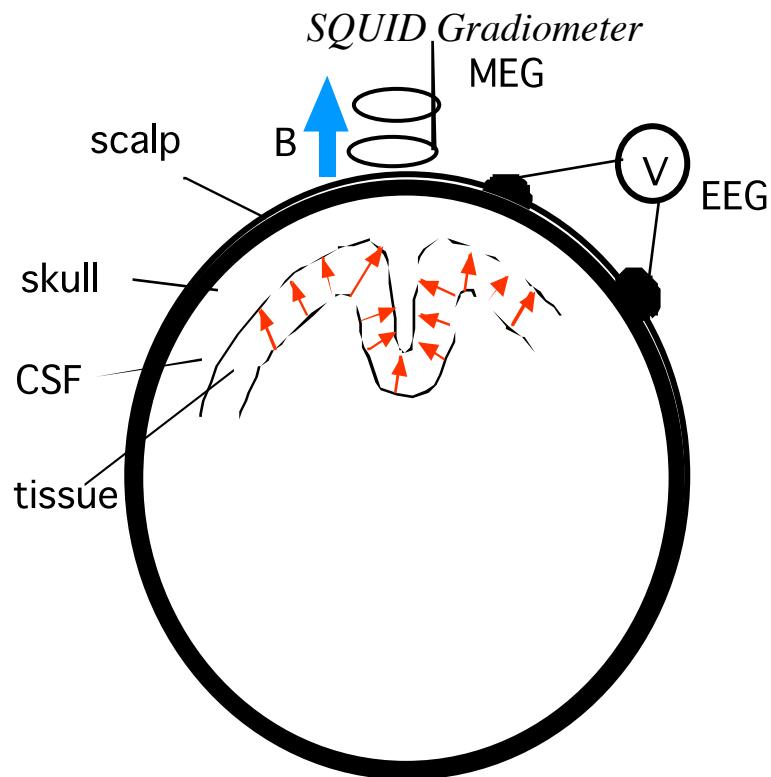


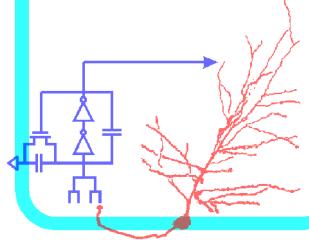
Photo by Fritz Goro

Computational Sensorimotor Systems Laboratory

MEG Magnetic Signal

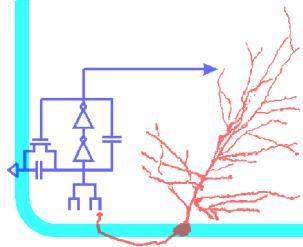
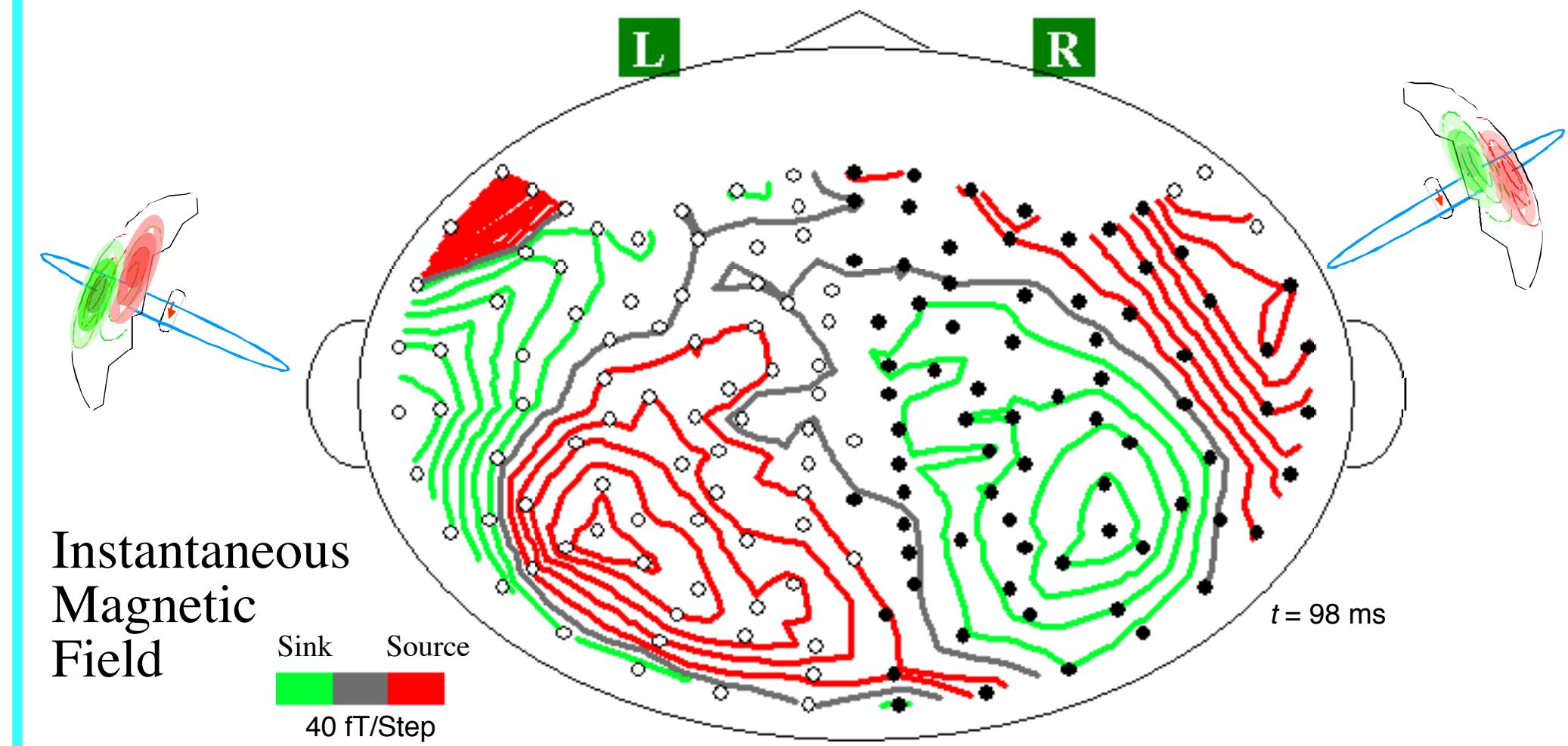


- Direct electrophysiological measurement
 - not hemodynamic
 - real-time
- No unique solution for distributed source



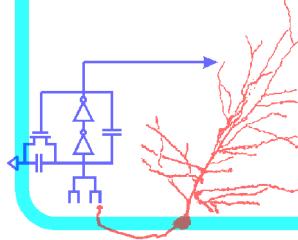
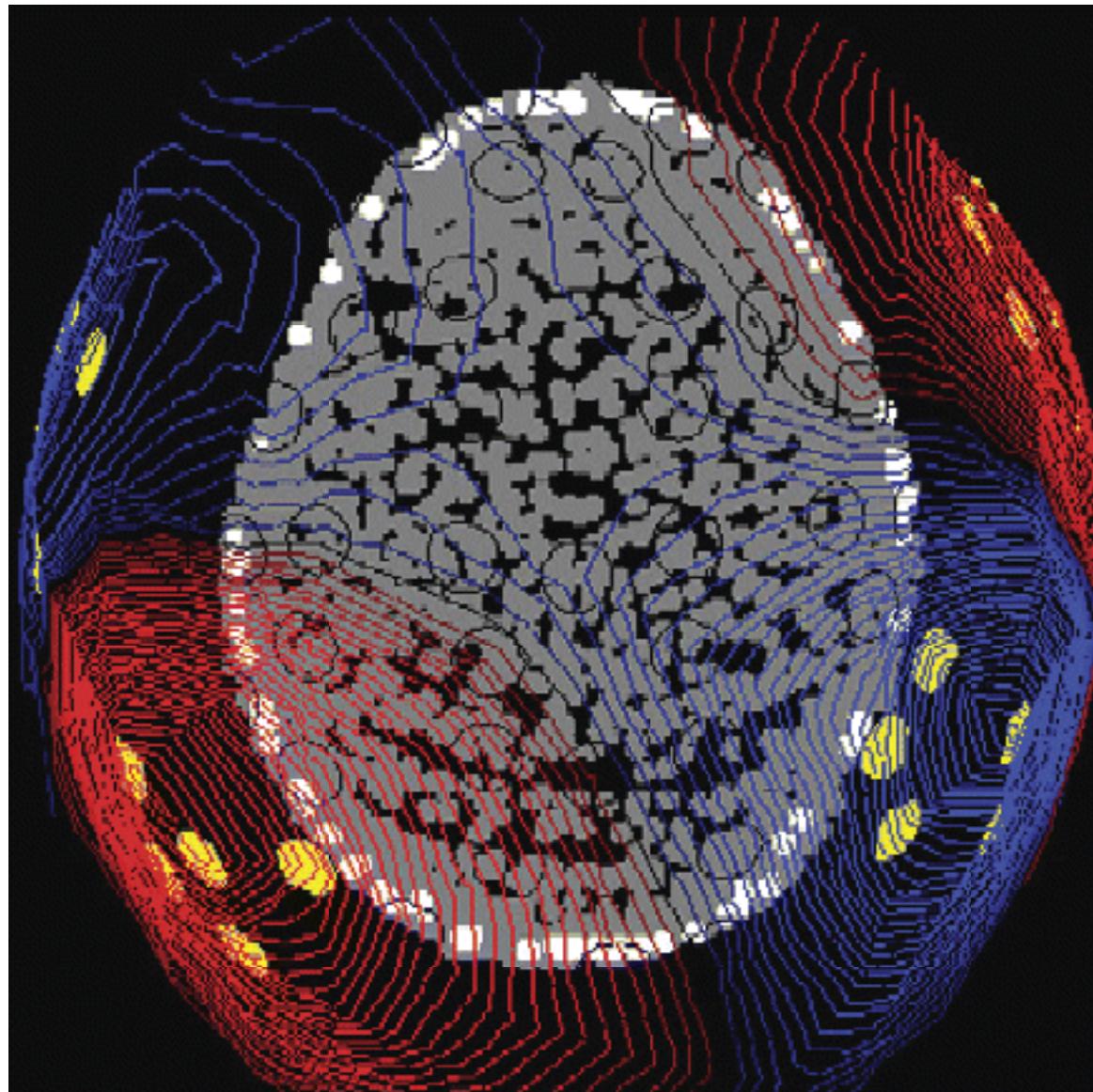
MEG Response

Flattened Isofield Contour Map

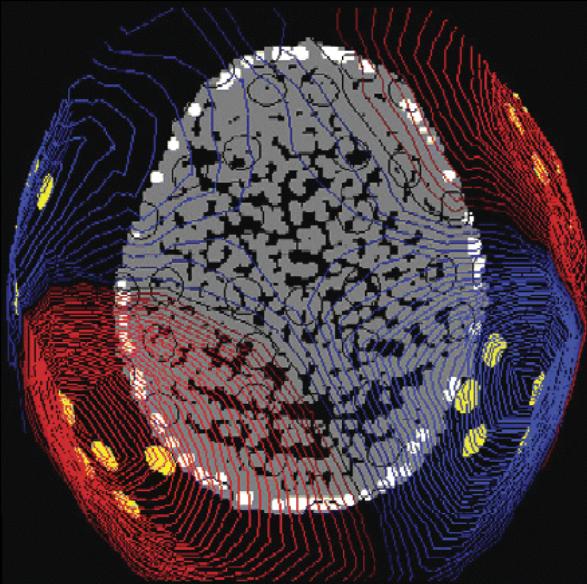


MEG Response

3-D Isofield Contour Map



Public Relations Moment



Cerebral CORTEX

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About the Cover

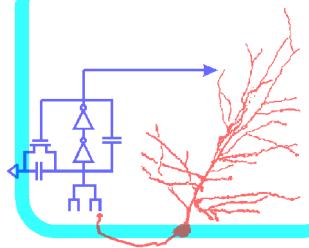
Cover Picture: Axial view of the cortically-generated magnetic field of a human listener, measured using whole-head magnetoencephalography (MEG), at a single moment in time. Isofield contours in red (respectively, blue) indicate the strength of outward (inward) magnetic flux; the digitized scalp surface is in gray. For each hemisphere, a magnetic dipole-like pattern is centered over temporal cortex, and the neural generator itself, located in planum temporale, is an inferiorly flowing neuronal electric current. The MEG channels responding most strongly (in the center of each flux area) are designated by filled yellow circles. The acoustic stimulus is a 1 kHz pure tone; time is 100 ms post onset. This image is generated with the MEG160 software (Yokogawa electric corporation, KIT, Japan). See Chait, Poeppl, and Simon, p. 835–848.

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Online ISSN 1460-2199 - Print ISSN 1047-3211

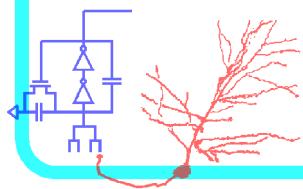
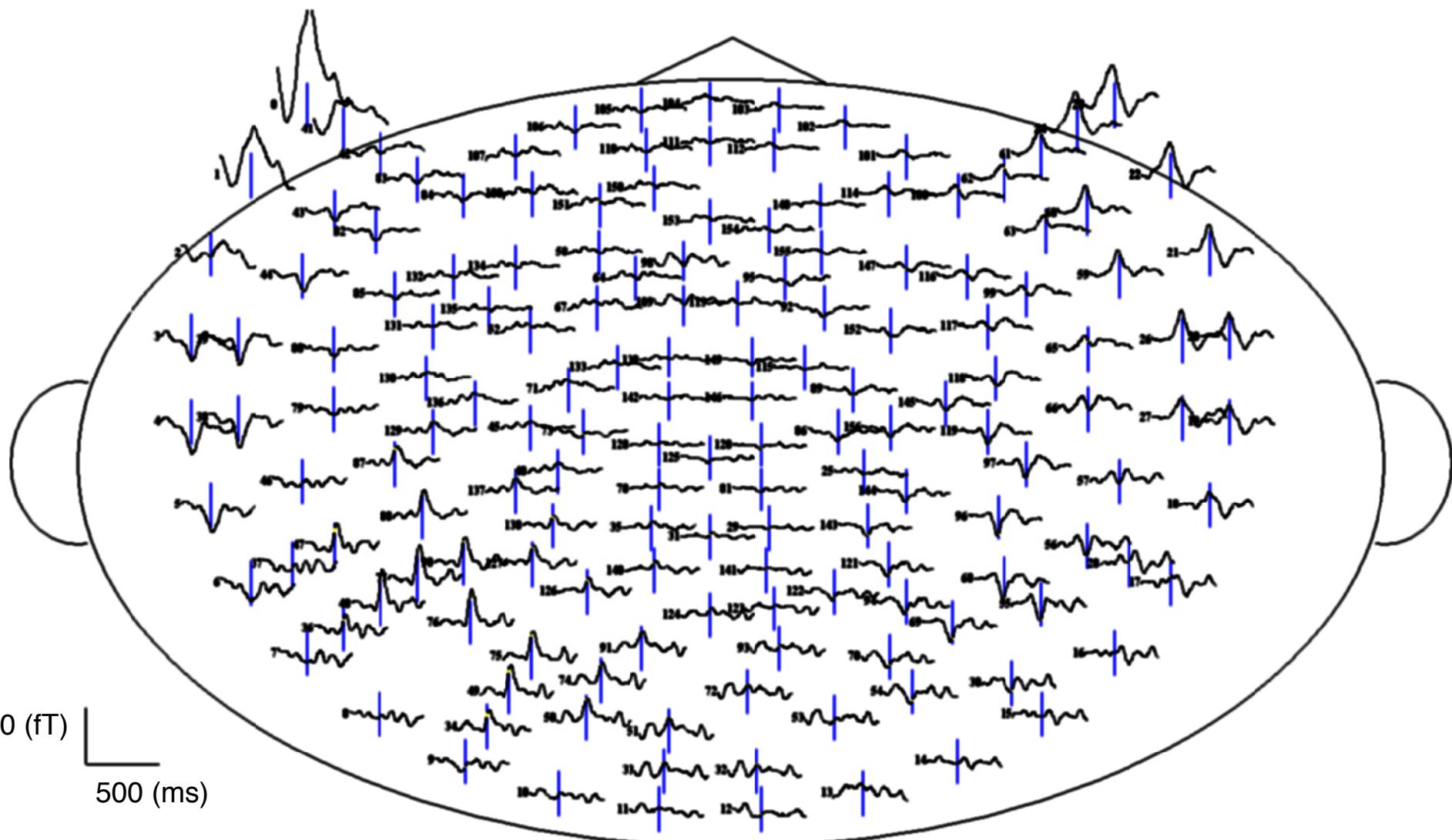
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MEG Response

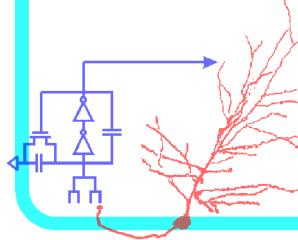
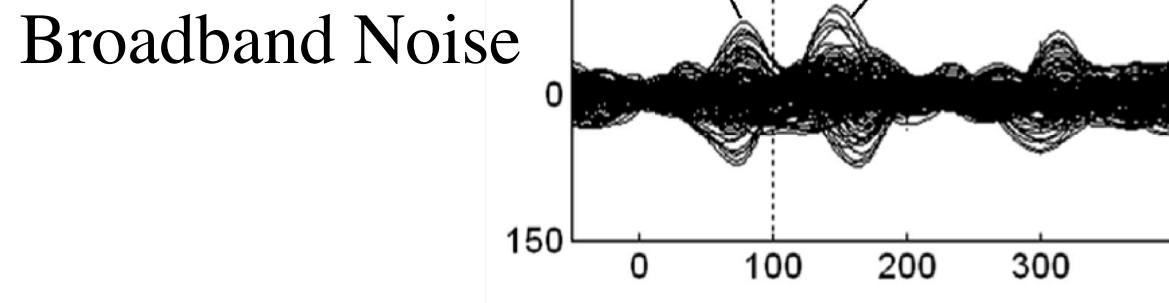
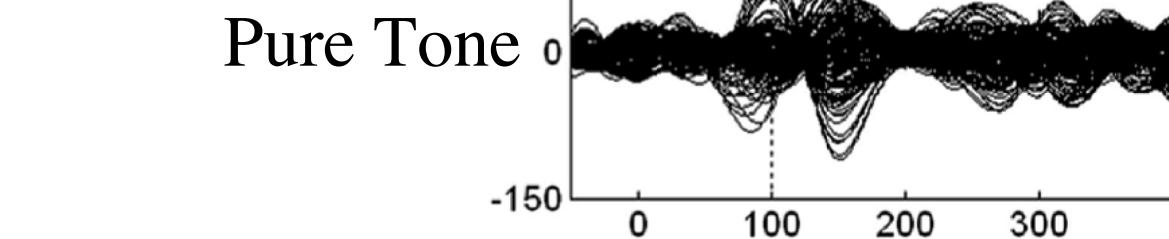
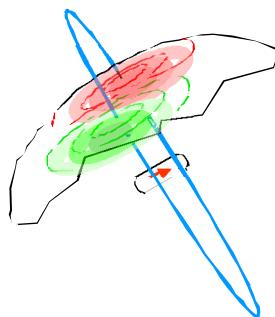
Spatial Map of Time Series



Time Course of MEG Responses

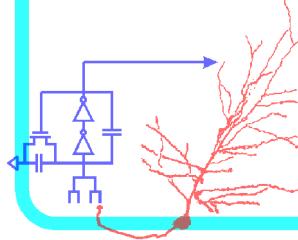
Evoked Responses

MEG Events Time-Locked
to Stimulus Event



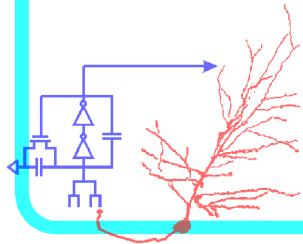
MEG as Auditory Physiology Tool

- Advantages of humans over animals
 - Subjects can be rented (by the hour)
 - Subjects can be trained in minutes
 - Better grasp of subjects perceptual space (?)
 - Access to Speech & Language processing (?)
- Advantage of Whole Head Recording
- Disadvantage of Neural Source Localization
 - Coarseness/Ambiguity in Source Location
 - Blindness to Many Kinds of Coding
- Neutral Aspects
 - Neural Source is Dendritic Current (not Spikes)
 - Humans not typical mammals (?)
 - New Technique/Immature Analysis Tools



Modulation Encoding

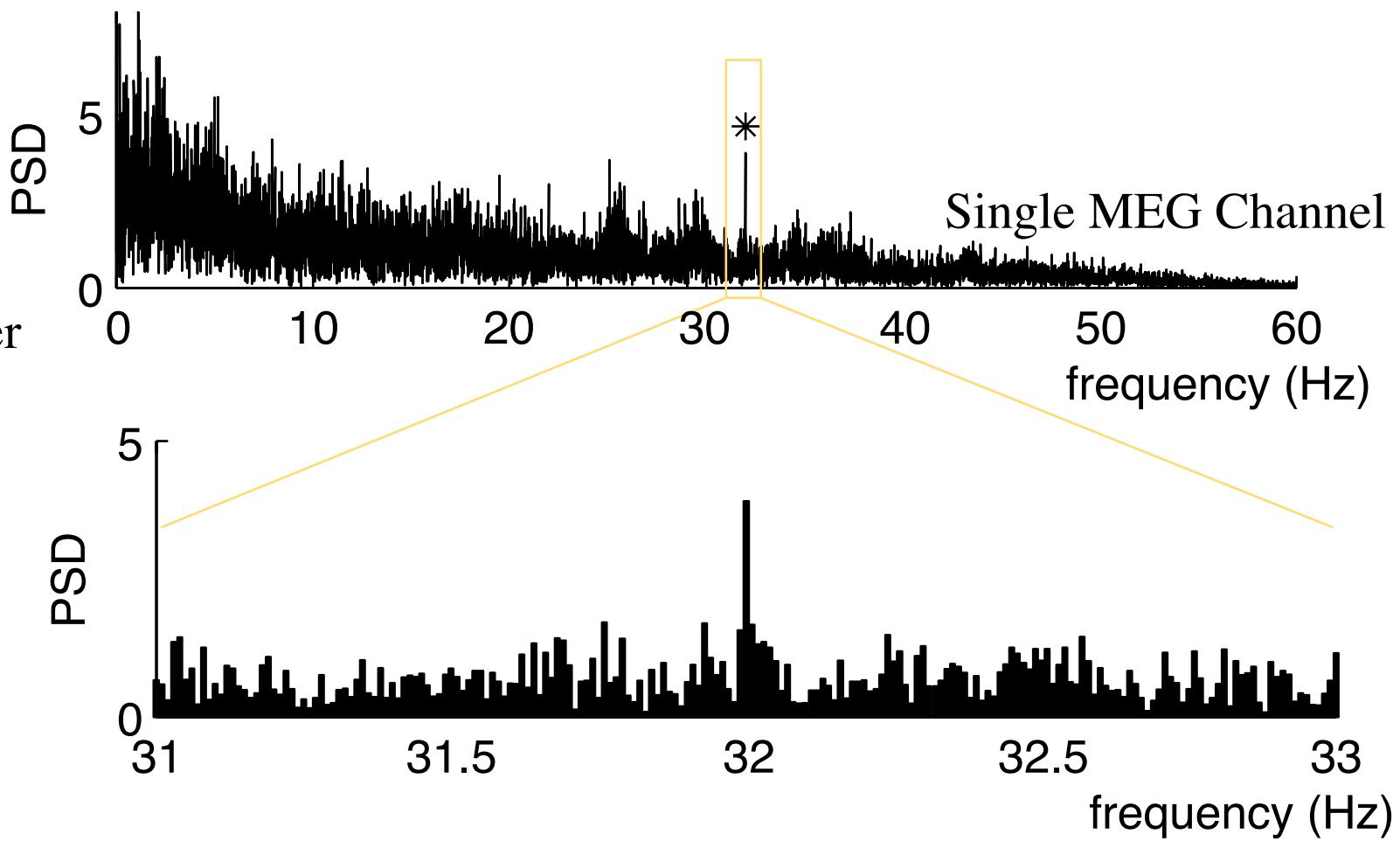
- Simple Modulations → Simple Cortical Encoding
 - Amplitude Modulation coding for slower modulations
 - Rate coding (invisible to MEG) for faster modulations
- Applies to general modulations: AM, FM, other
- Amplitude Modulation coding is easily detectable in Fourier/Spectral domain
 - Spectral Peak at Modulation Frequency



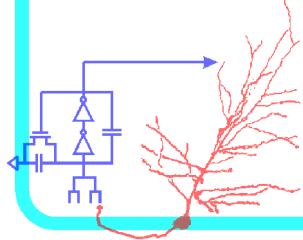
Frequency Response

Stimulus Modulated at Single Frequency \rightarrow *Steady State Response* (SSR)

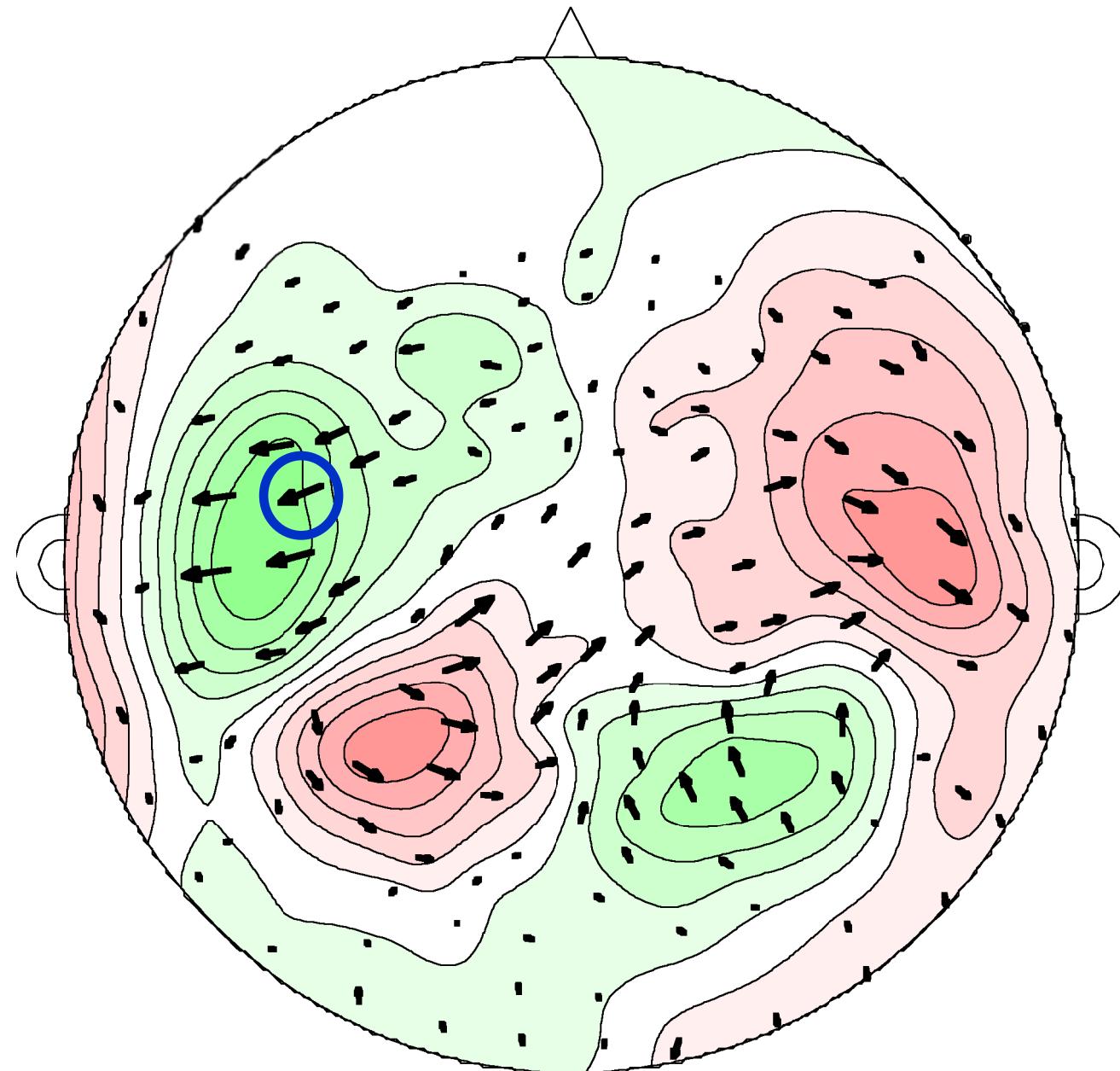
32 Hz Modulation
400 Hz tone carrier
100 trials @ 1 s
(concatenated)



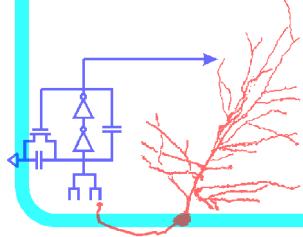
Extremely Precise Phase-Locking: 0.01 Hz
No trial-to-trial jitter



Whole-Head SSR

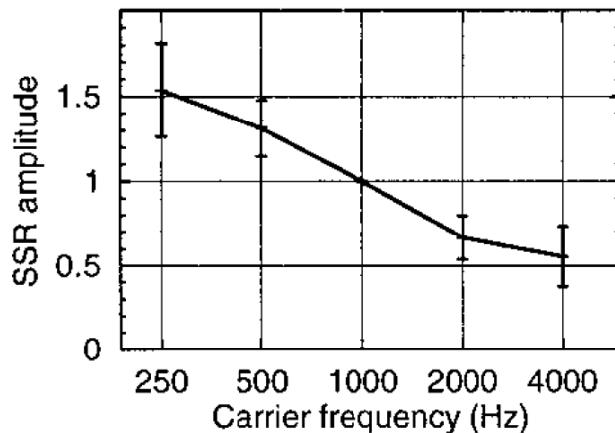


32 Hz

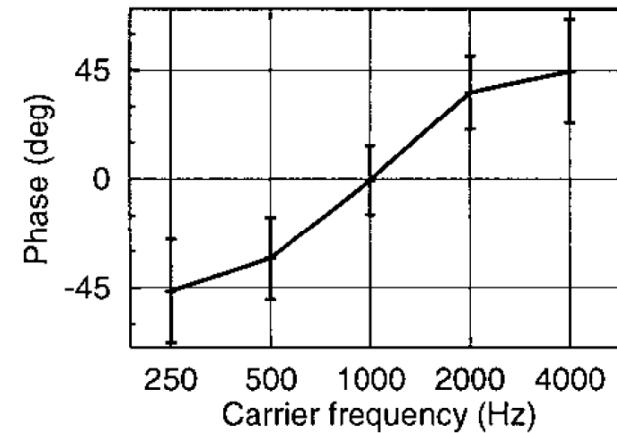


SSR Carrier Dependence

SSR Amplitude



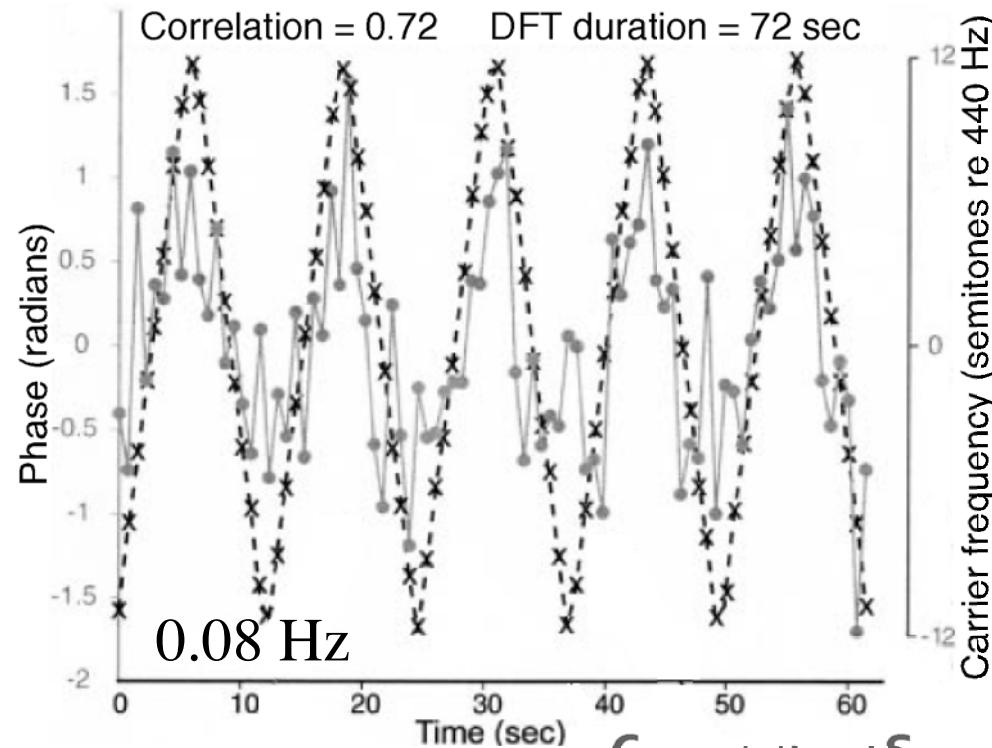
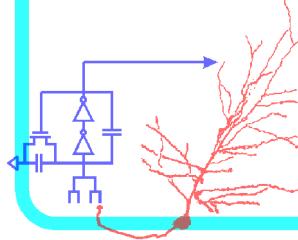
SSR Phase



*Ross et al.
(2000)*

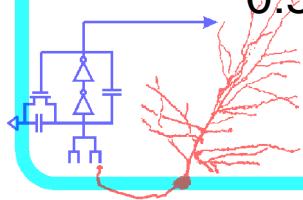
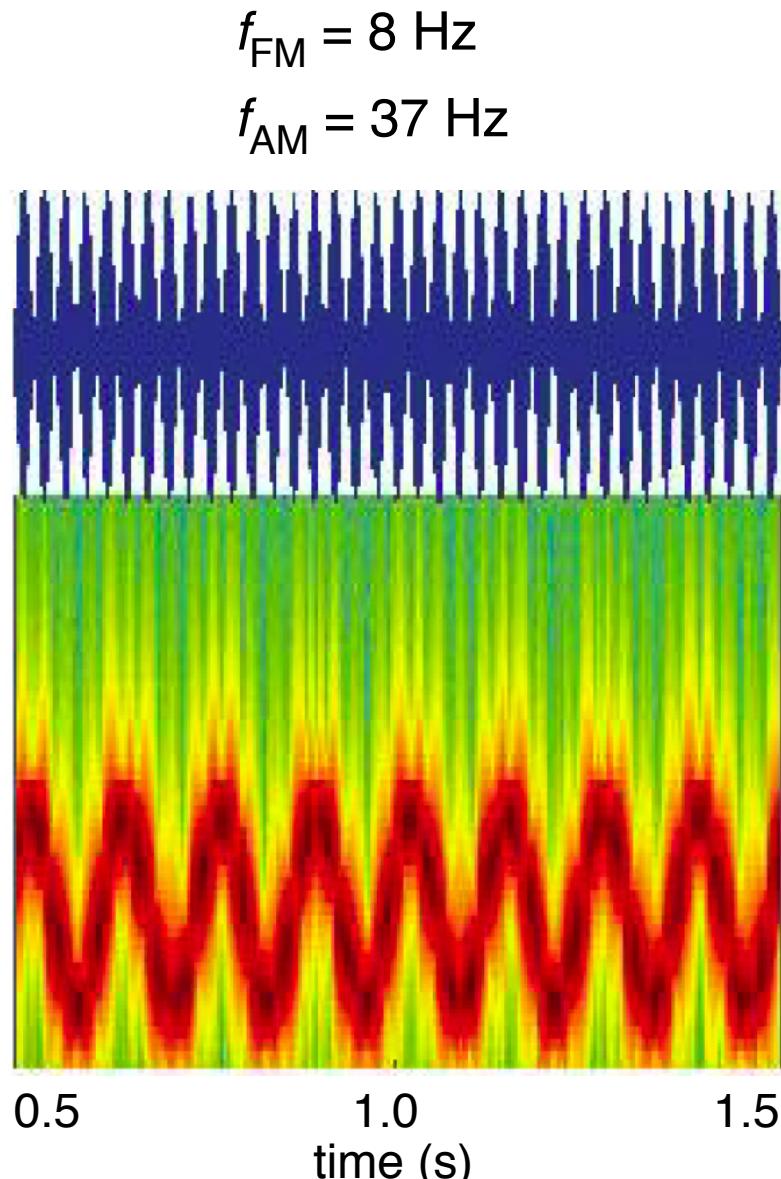
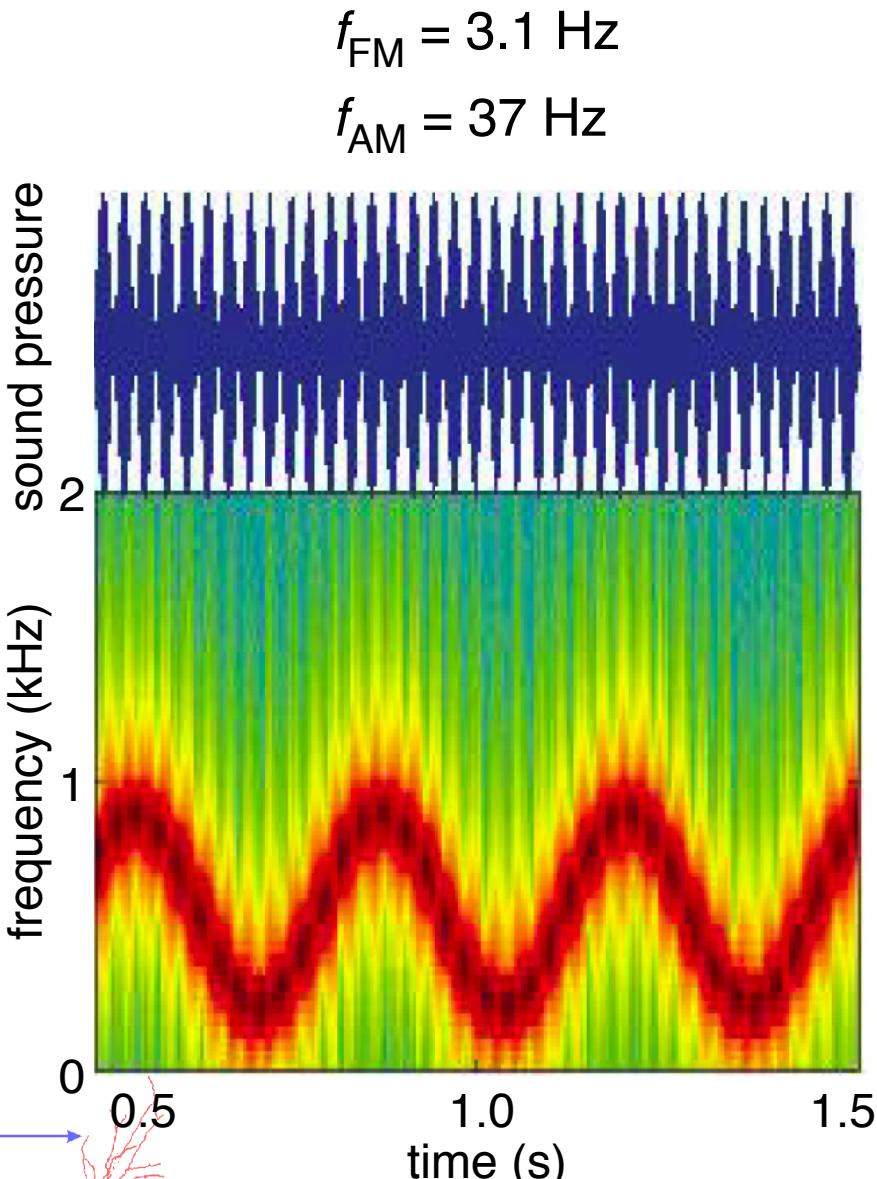
SSR Phase
Follows
Carrier

↓
Phase
Modulation
Encoding

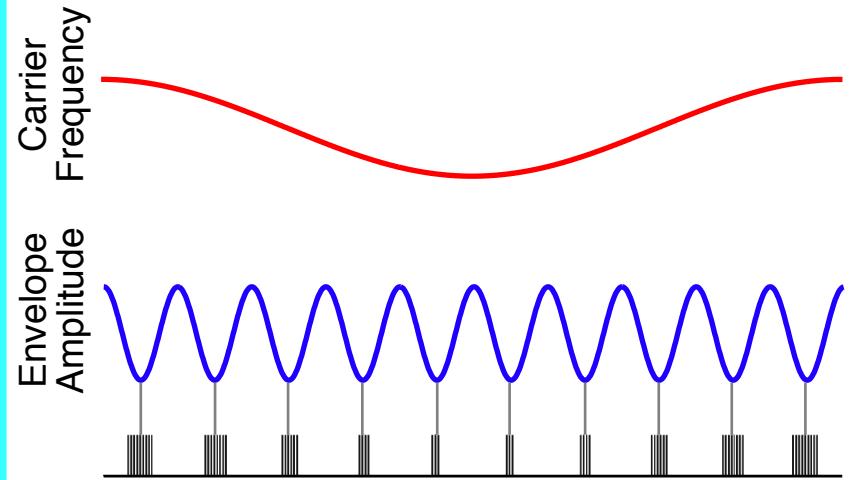


*Patel &
Balaban
(2004)*

Sample Dual Modulation Stimuli



Neural Modulation Models

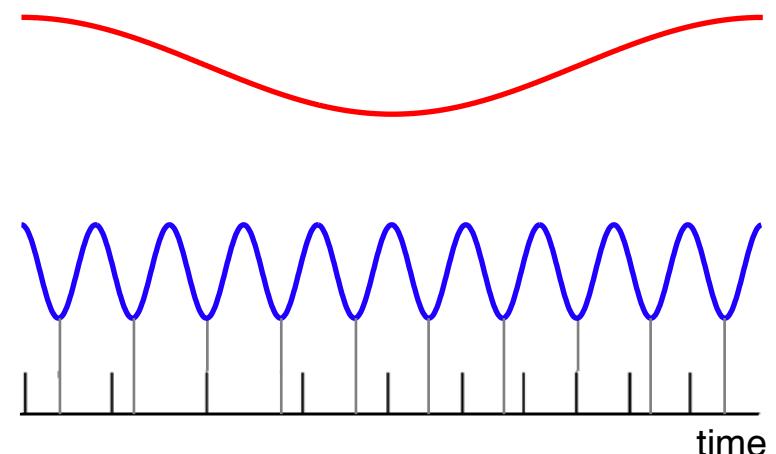


Amplitude Modulation (AM) Coding

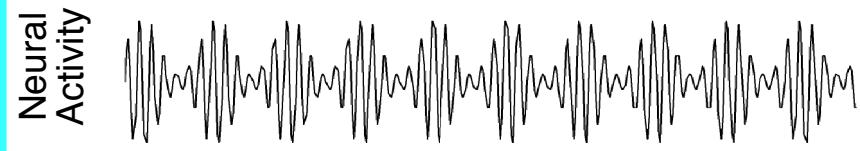
Stimulus Carrier Frequency (FM)

Stimulus Envelope Amplitude (AM)

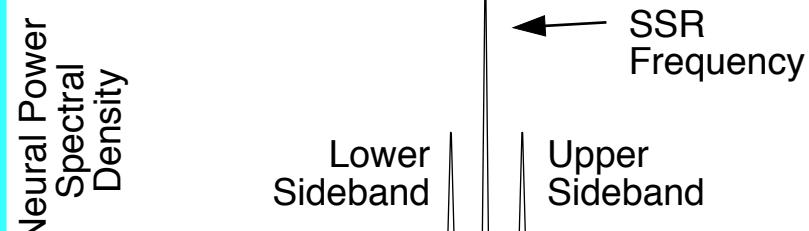
Neural Modulation Coding



Phase Modulation (PM) coding



Neural Averaged Response



Neural Response Spectrum

c.f.
Patel & Balaban (2004)

$\alpha_{AM} = 0 \text{ or } 2\pi$

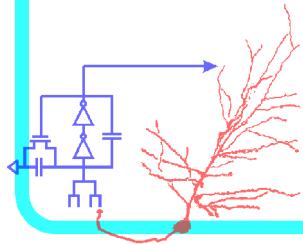
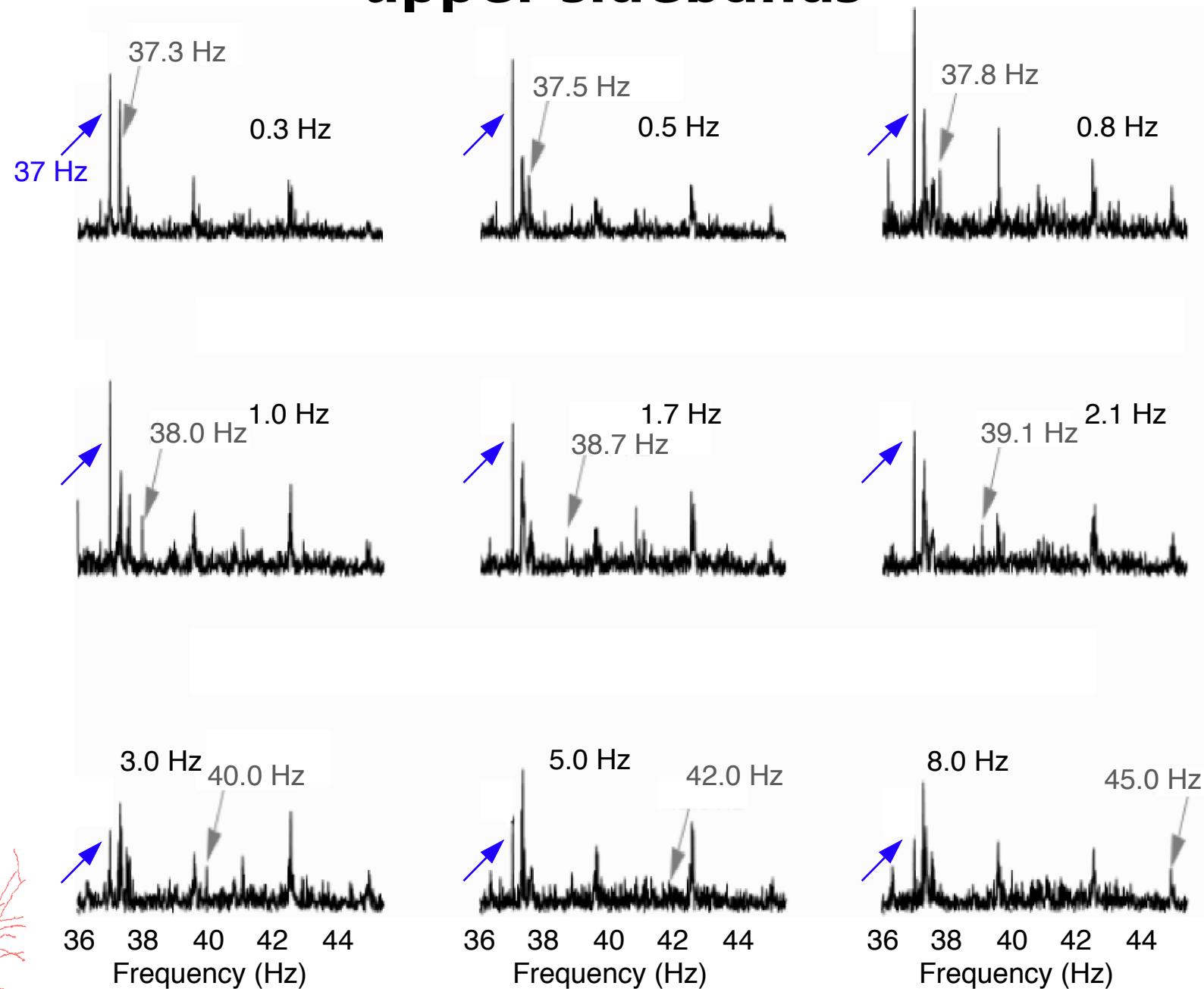
$$\alpha = (\varphi_{upper} - \varphi_{SSR}) - (\varphi_{SSR} - \varphi_{lower})$$

Neural Response Phase Encoding Parameter

$$\alpha_{PM} = \pi$$

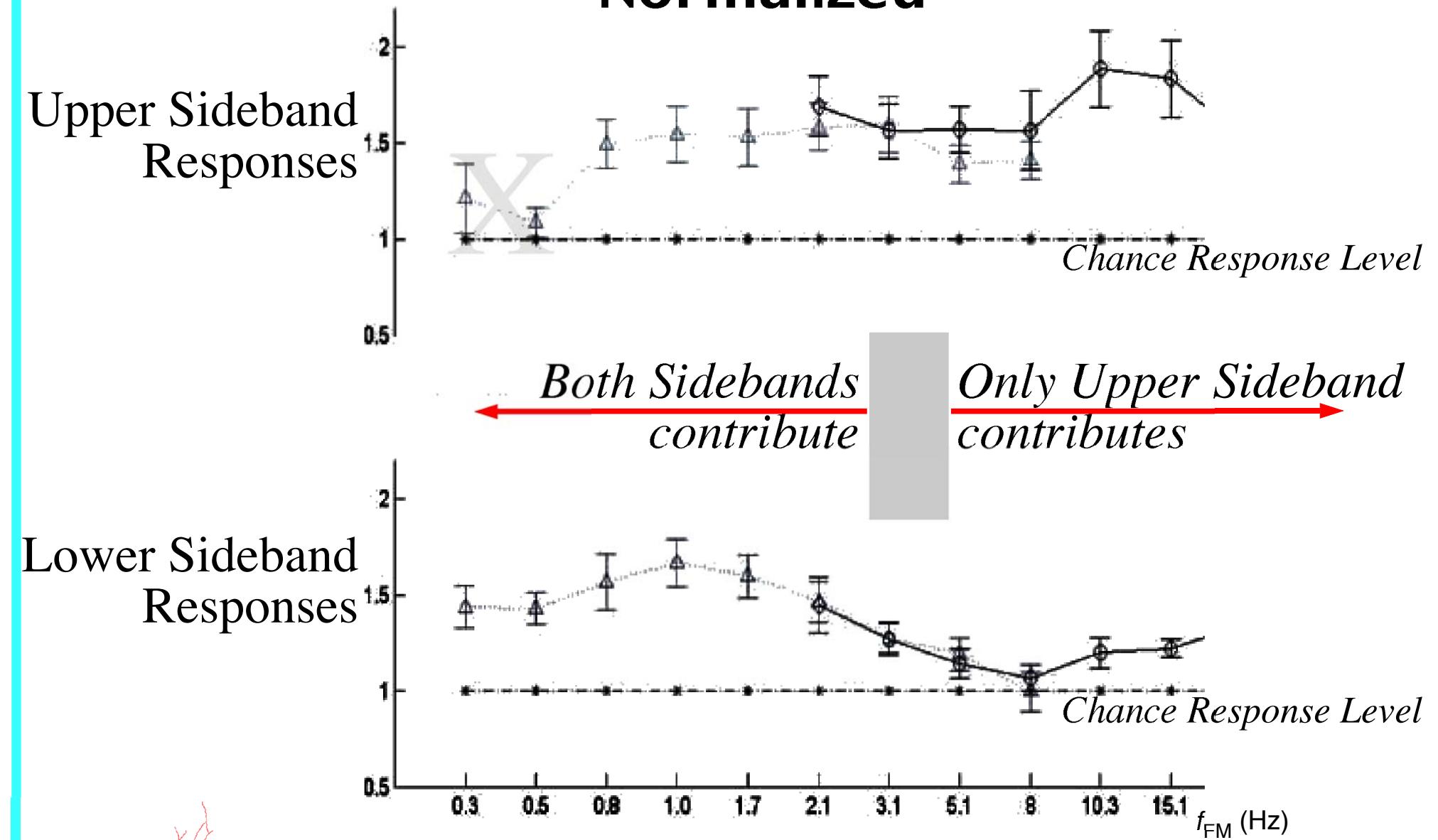
Spectral Sideband Responses

upper sidebands

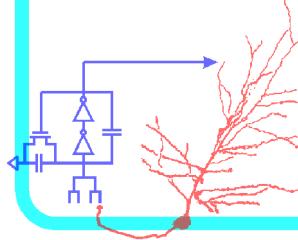


Sideband Responses

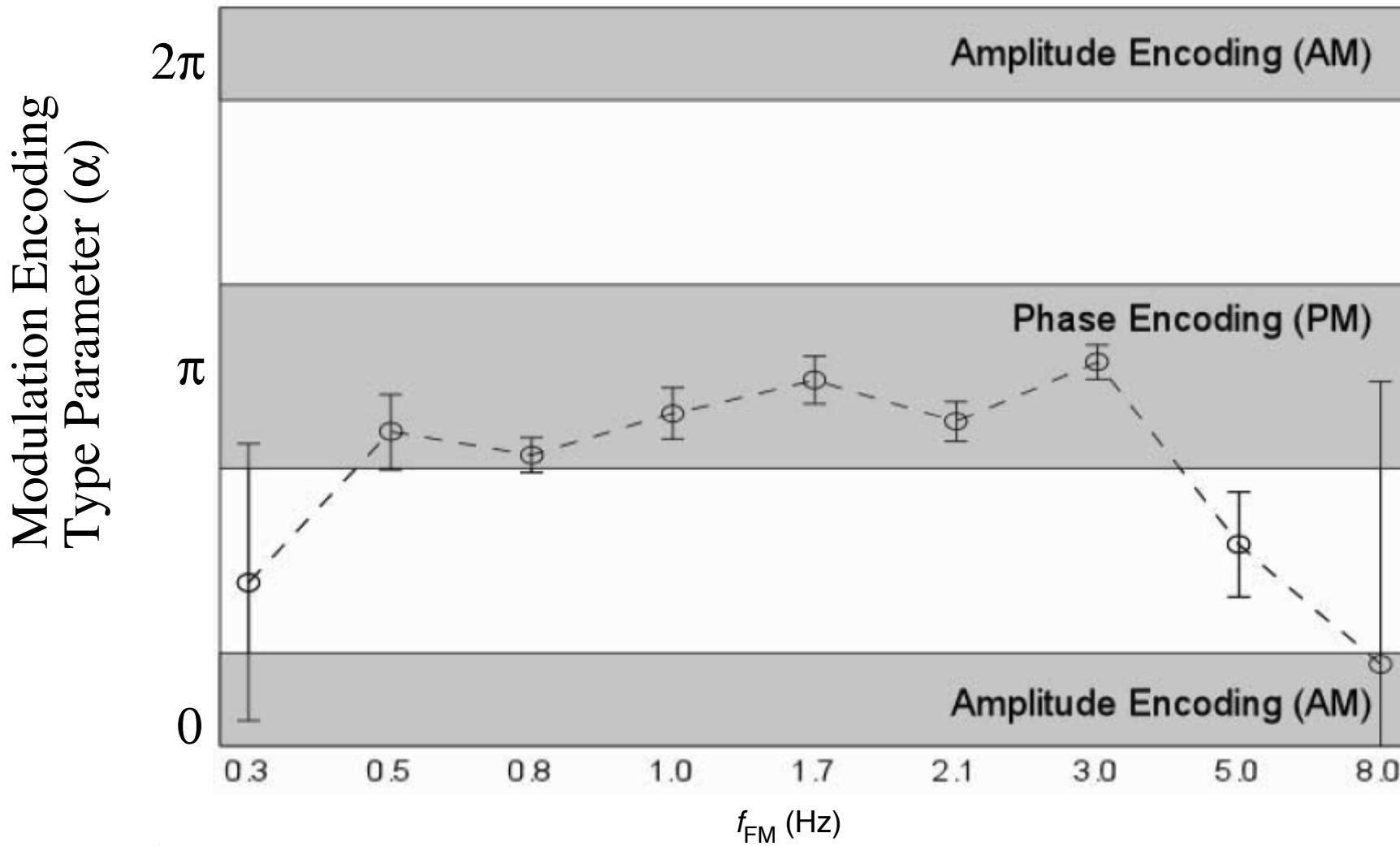
Normalized



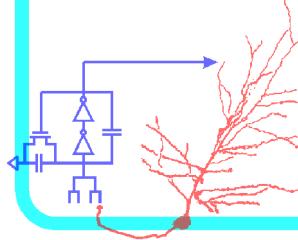
Modulation Encoding, with coding transition at $f_{FM} \sim 5$ Hz



Modulation Encoding Type



Phase Modulation Encoding below $f_{FM} \sim 5$ Hz



Conclusions

- MEG can address questions of Neural Coding
 - Coarseness of Localization not Intrinsic Obstacle
 - Modulation encoding gives family of response types
- Combined AM/FM modulations are encoded in Auditory Cortex
 - Phase Modulation seen at lowest FM rates
 - Modulation Encoding changes at higher rates
- Single Sideband Modulation unexpected
 - Speculate: Single Modulation Encoding type?
 - Or: Two populations of AM and PM encoding neurons whose phase happens to cancel in lower sideband?

